



南京理工大学

NANJING UNIVERSITY OF SCIENCE & TECHNOLOGY

计算光学成像与 光信息处理技术前沿

(第8讲)

左超

南京理工大学电光学院光电技术系

Jiangsu Key Laboratory of Spectral Imaging & Intelligent Sense (SIIS)

Nanjing University of Science and Technology,

Nanjing, Jiangsu Province 210094, China



电子工程与光电技术学院

School of Electronic and Optical Engineering



江苏省光谱成像与智能感知重点实验室

Jiangsu Key Laboratory of Spectral Imaging & Intelligent Sense



南京理工大学
NANJING UNIVERSITY OF SCIENCE & TECHNOLOGY

光学前沿
2020

光学成像与显示
2020年6月19-20日



光强传输方程

Transport of intensity equation

Chao Zuo (左超)

Smart Computational Imaging Laboratory (SCILab)

Jiangsu Key Laboratory of Spectral Imaging & Intelligent Sense (SIIS)

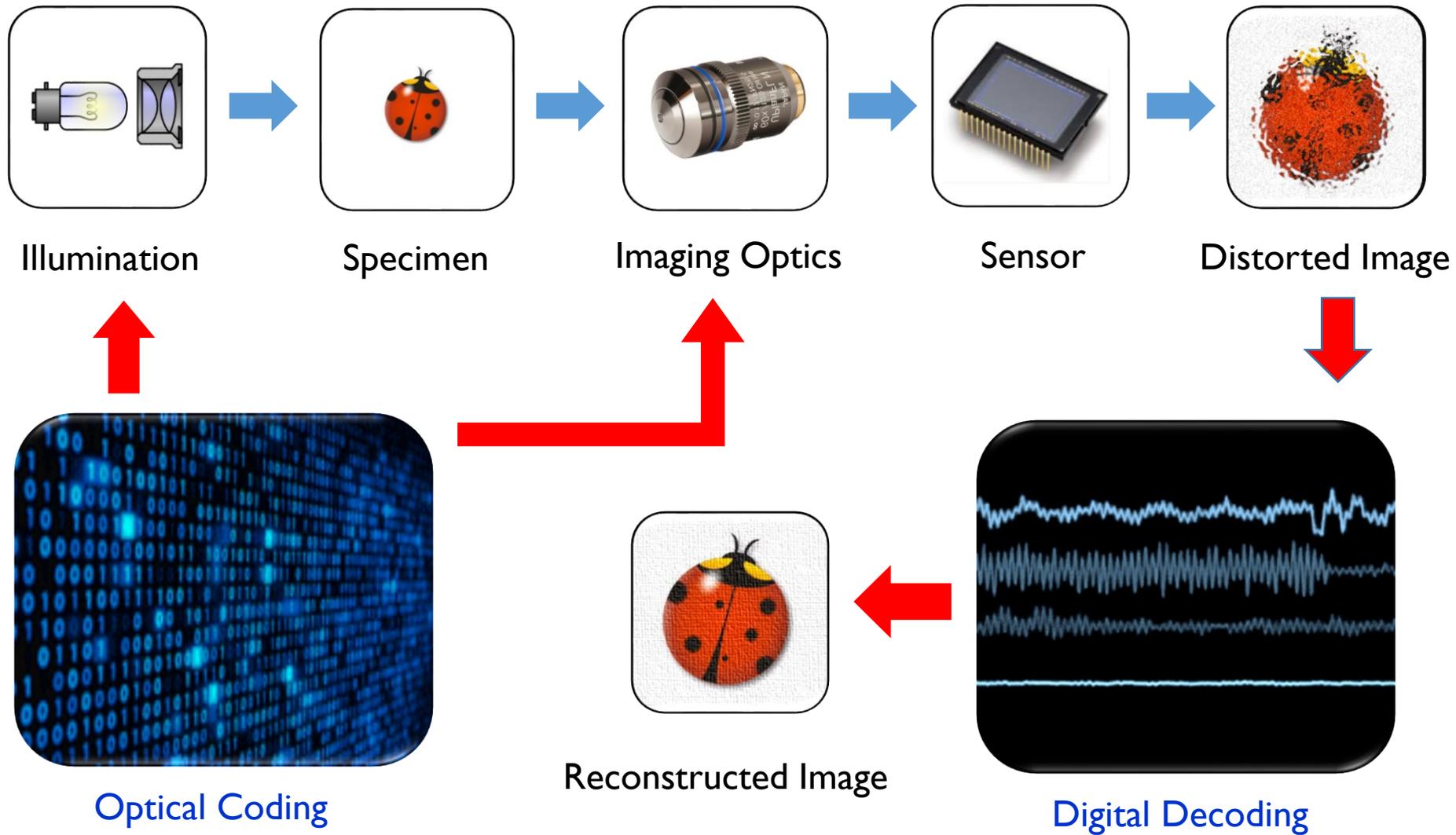
Nanjing University of Science and Technology,

Nanjing, Jiangsu Province 210094, China

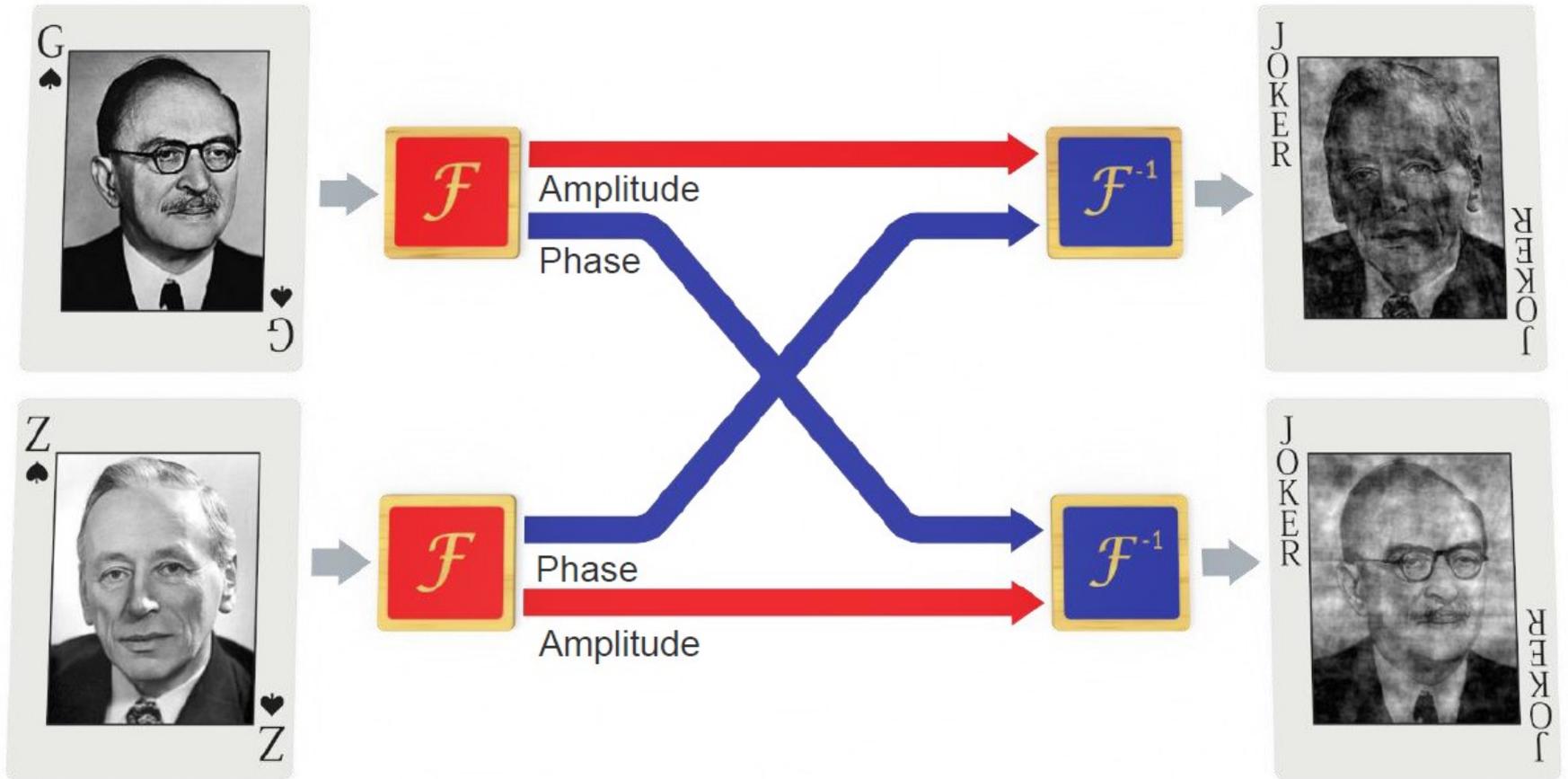


Smart Computational Imaging

Computational microscopy



Phase of a image

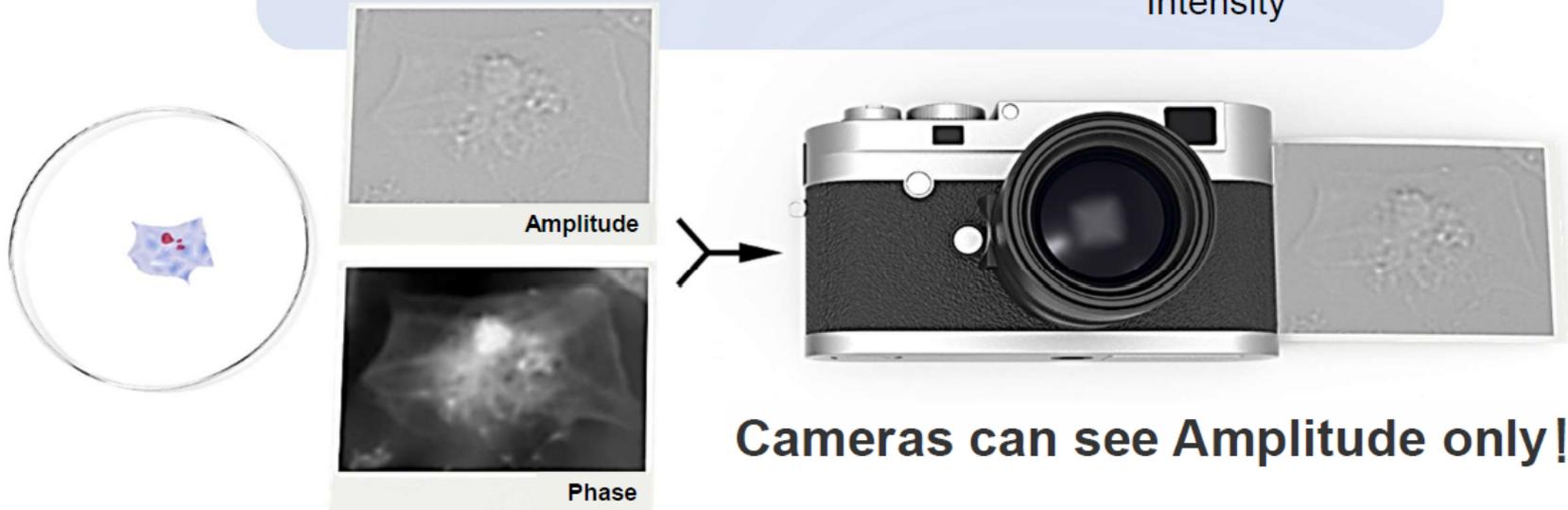


Phase of a object

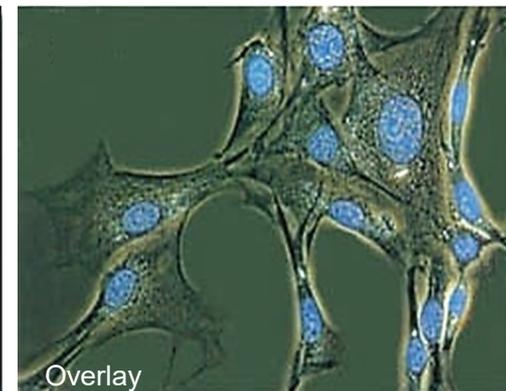
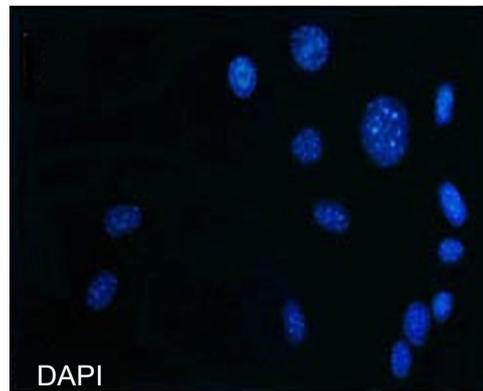
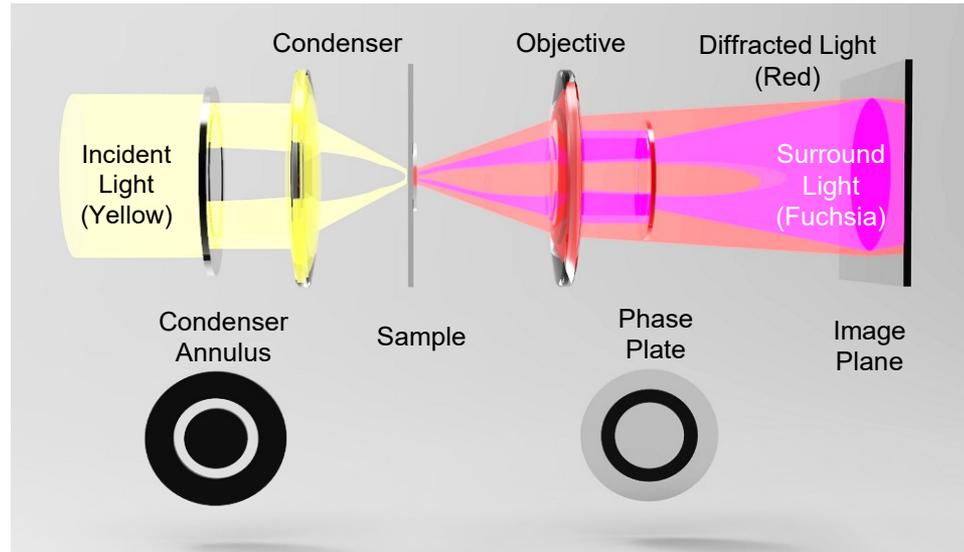
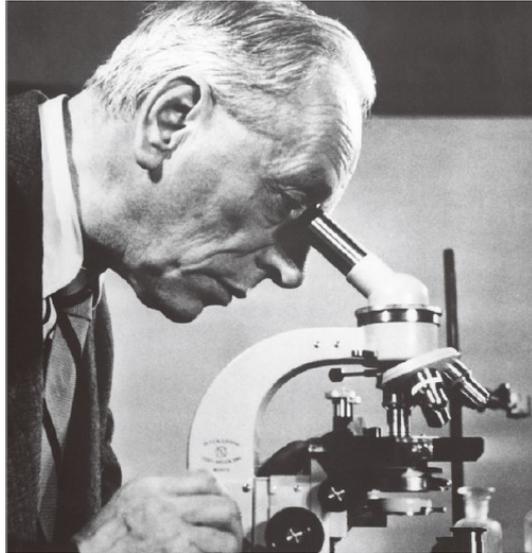
$$\underbrace{U(x, y)}_{\text{Complex Amplitude}} = \underbrace{A(x, y)}_{\text{Amplitude}} e^{j\phi(x, y)}$$

Phase

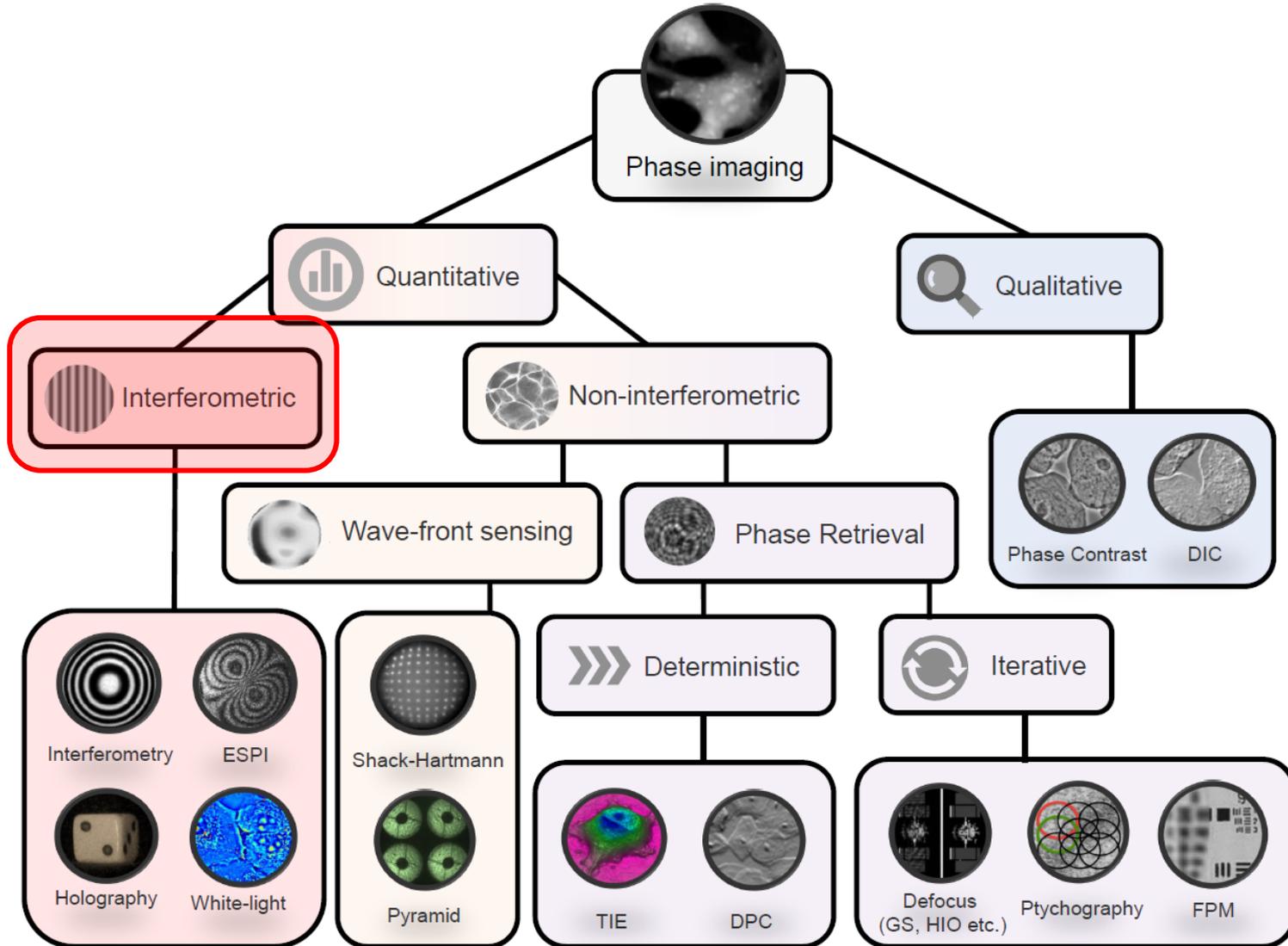
$$A(x, y) = \sqrt{\underbrace{I(x, y)}_{\text{Intensity}}}$$



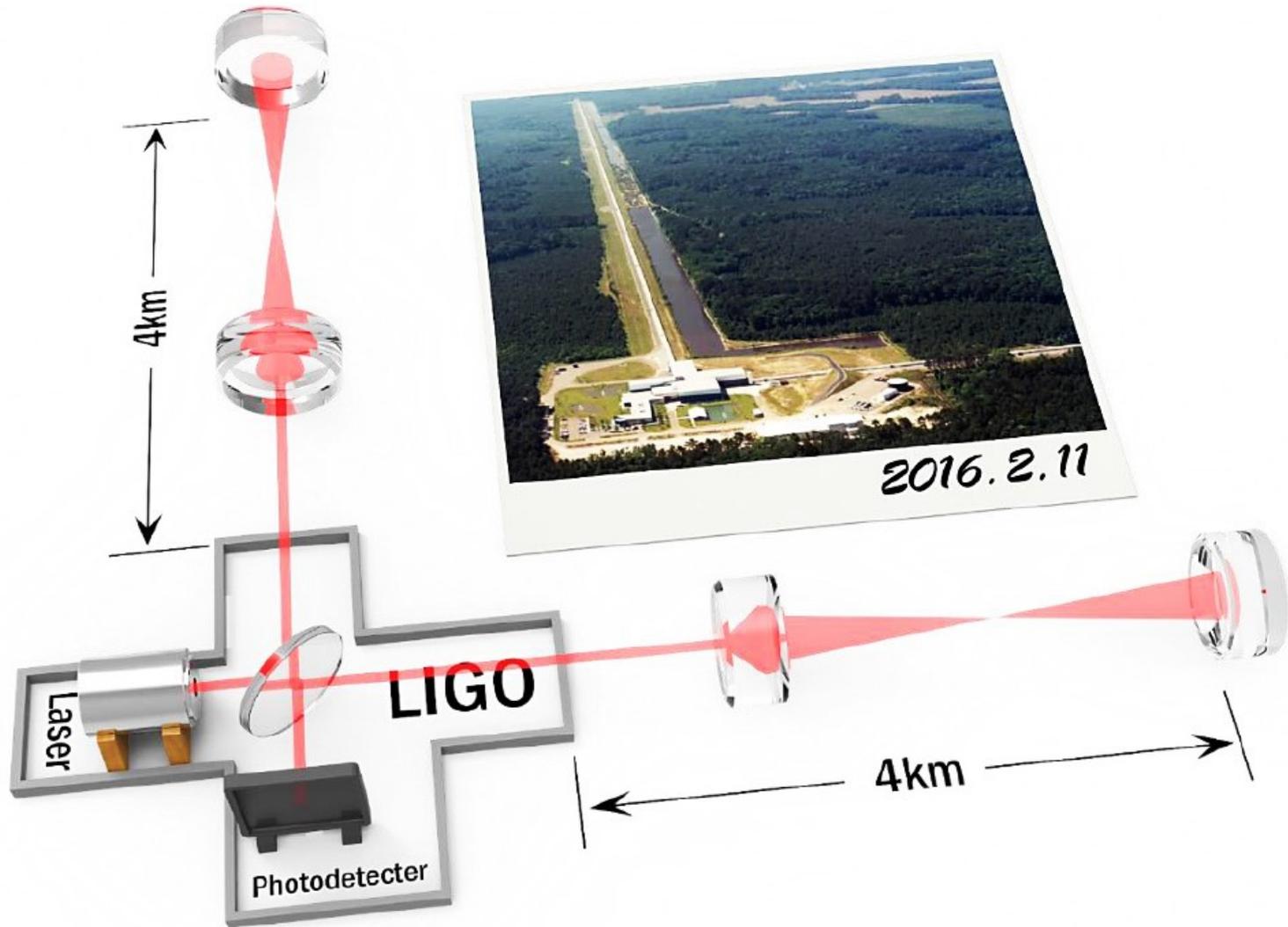
Phase contrast microscopy



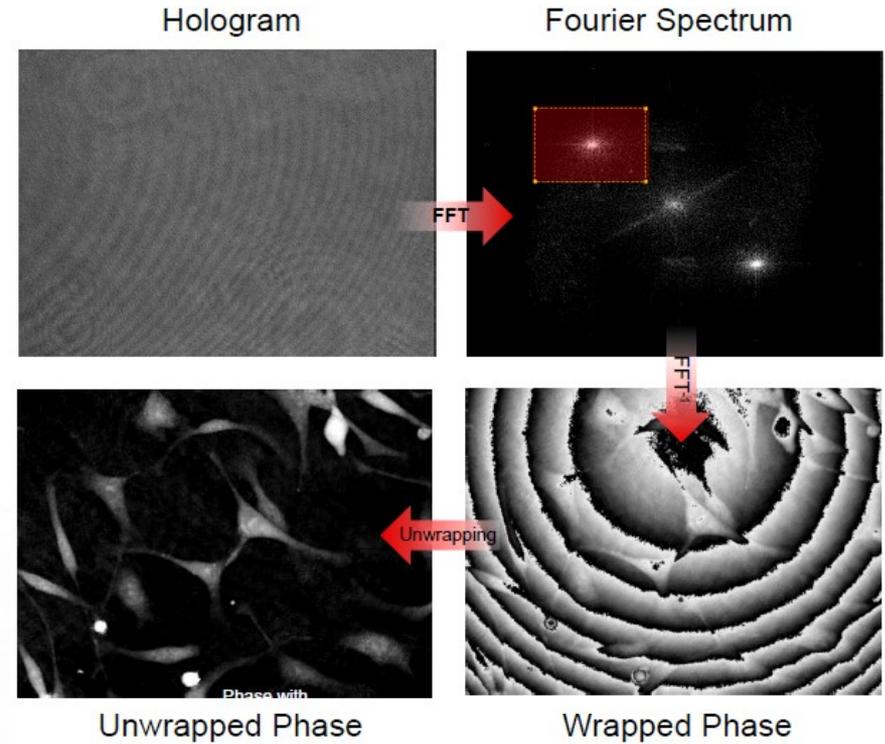
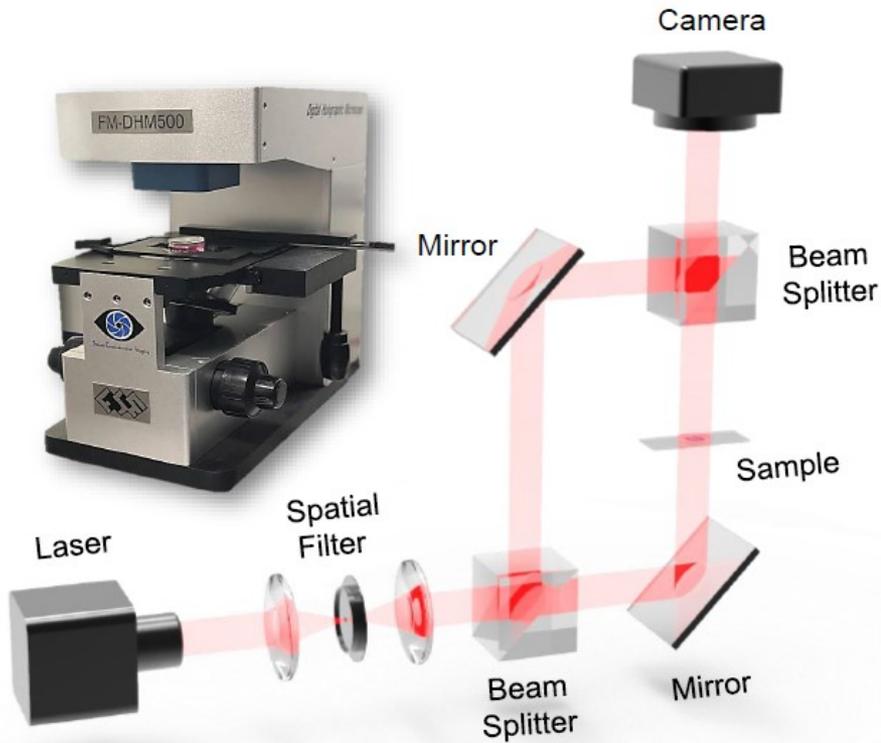
Phase imaging



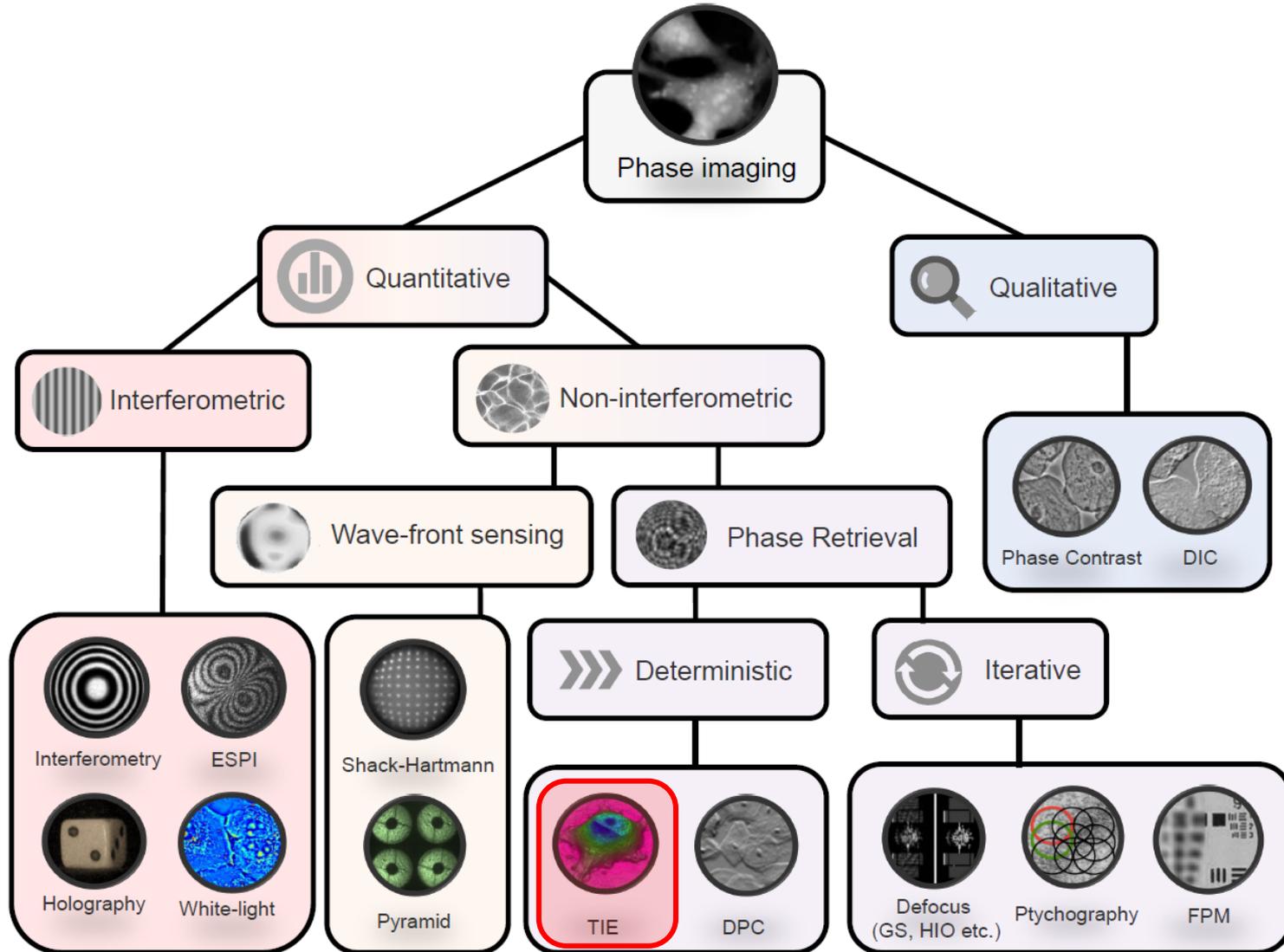
Interferometry



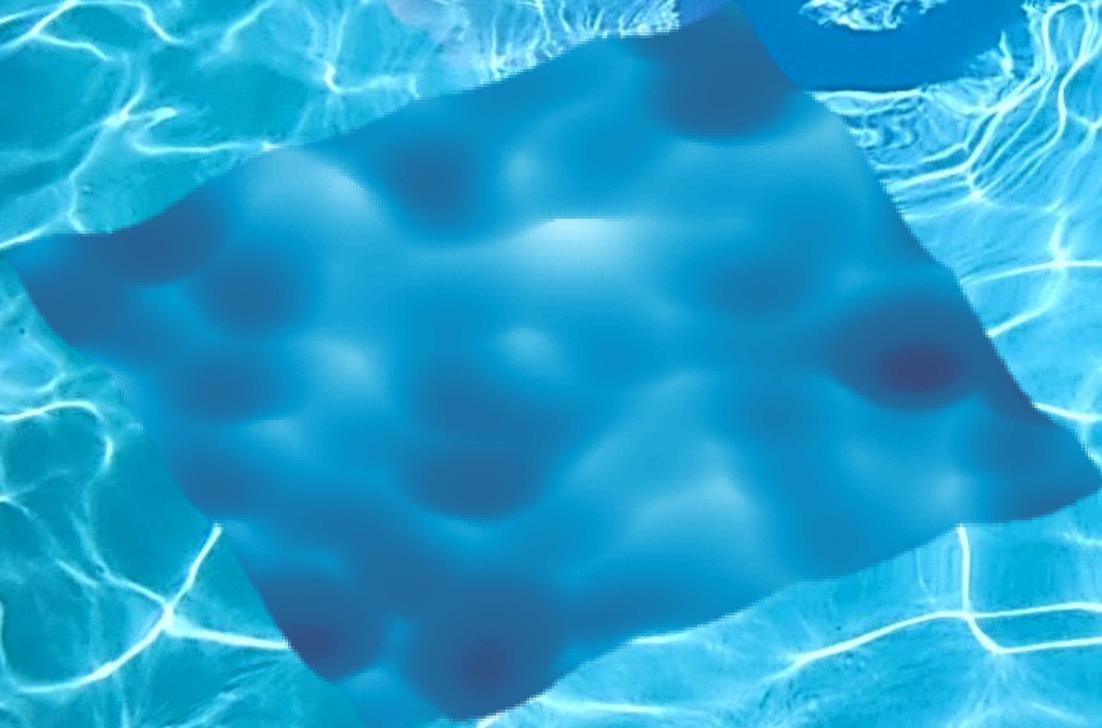
Digital Holography



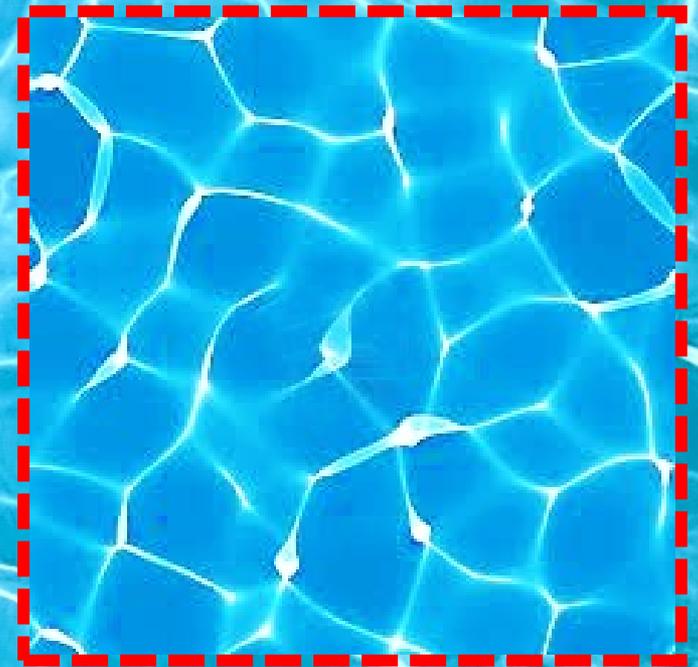
Phase imaging



See Phase w/o Interference



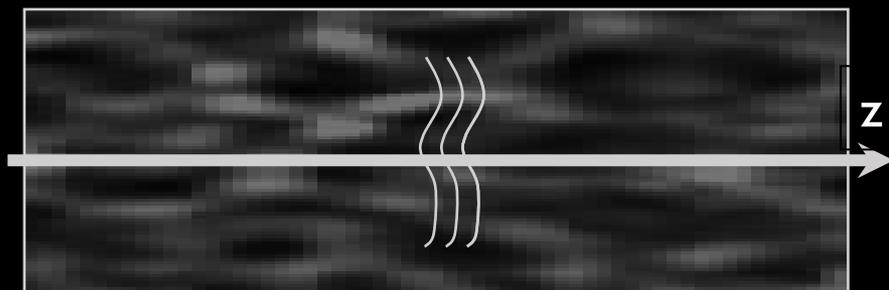
Intensity \rightarrow Phase



Phase \rightarrow intensity

How does wave propagate?

Non-planar phase changes the intensity during wave propagation

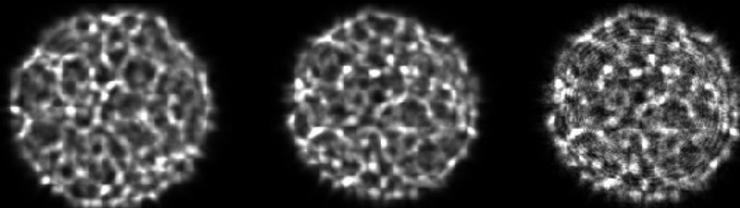


 Light spreads out – dimmer
 Light is concentrated – brighter

$z = -\Delta z$

$z = 0$

$z = +\Delta z$



$$U(x, y) = \sqrt{I(x, y)} e^{i\phi(x, y)}$$

$\phi(x, y) = \text{constant}$

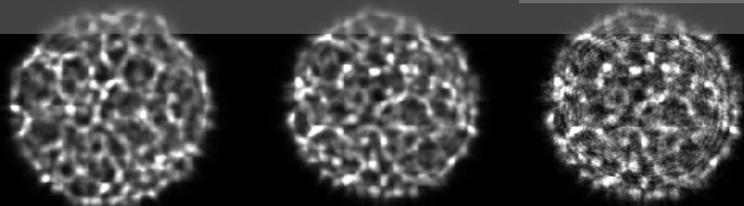
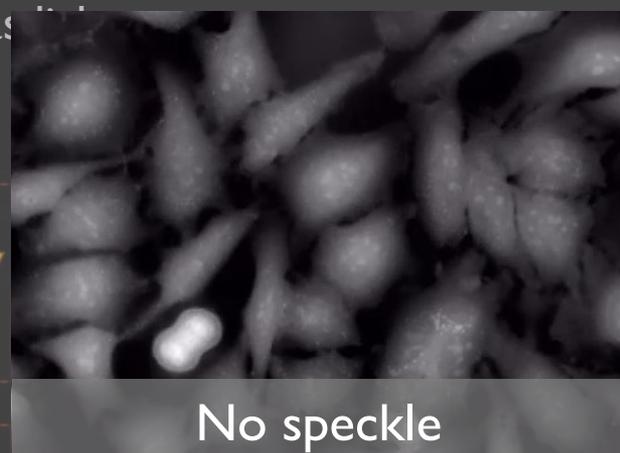
Paraxial Wave Equation

$$\nabla^2 U(x, y) + 2k \frac{\partial U(x, y)}{\partial z} = 0$$

Transport-of-intensity equation (TIE)¹

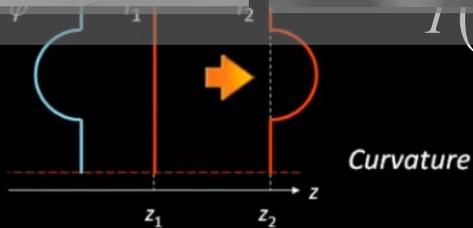
$$-k \frac{\partial I(x, y)}{\partial z} = \nabla \cdot [I(x, y) \nabla \phi(x, y)]$$

Transport-of-intensity equation (TIE)

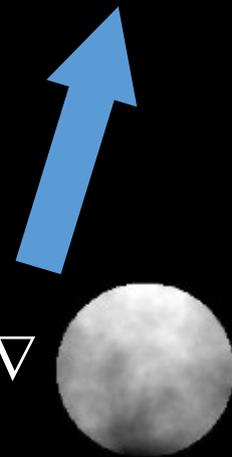


$$\approx \frac{I_{+\Delta z}(x, y) - I_{-\Delta z}(x, y)}{2\Delta z}$$

Transport-of-intensity equation (TIE)



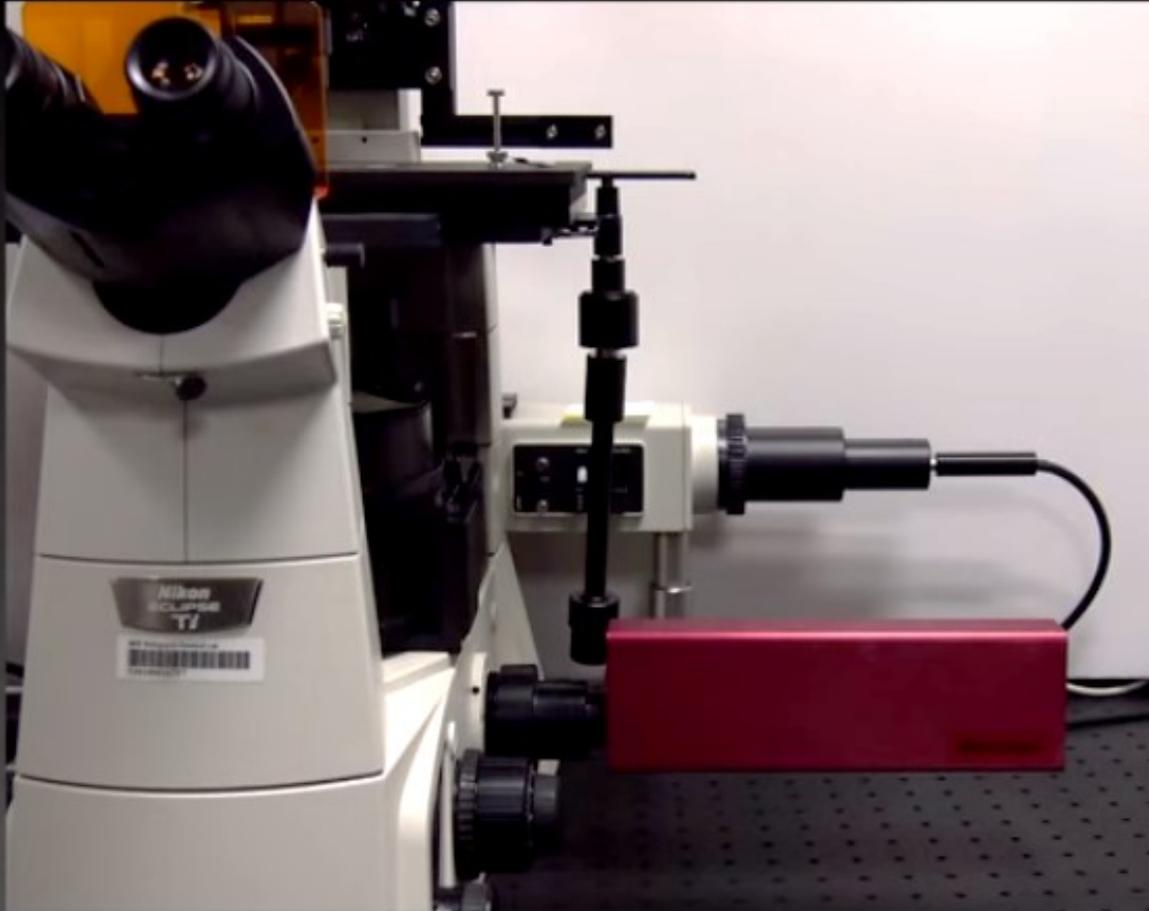
$$-k \frac{\partial I(x, y)}{\partial z} = \nabla \cdot \left[I(x, y) \nabla \right]$$



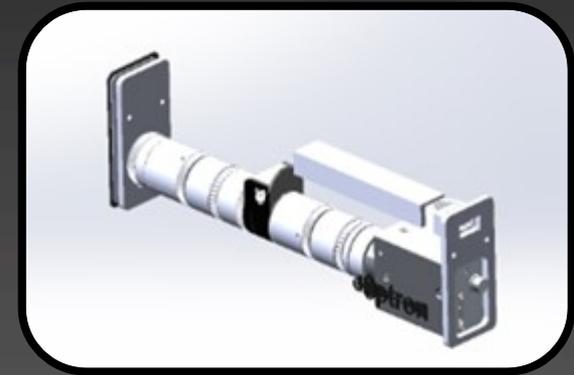
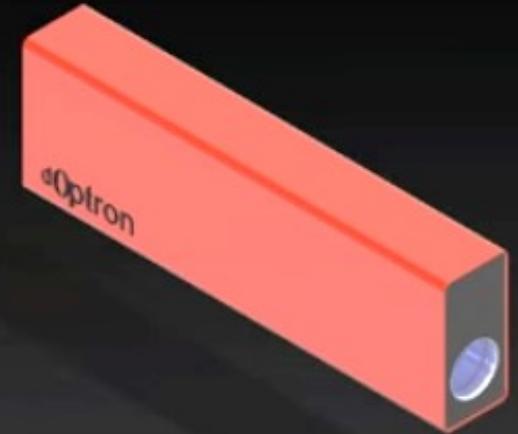
Code & dataset available @ www.scilaboratory.com

- [1] M. Reed Teague, J. Opt. Soc. Am. 73, 1434-1441 (1983).
- [2] C. Zuo, Q. Chen, Y. Yu, and A. Asundi, Optics Express 21, 5346-5362 (2013).
- [3] C. Zuo, Q. Chen, and A. Asundi, Optics Express 22, 9220-9244 (2014).
- [4] C. Zuo, Q. Chen, H. Li, W. Qu, and A. Asundi Optics Express 22, 18310-18324 (2014).

Dynamic TIE microscopy

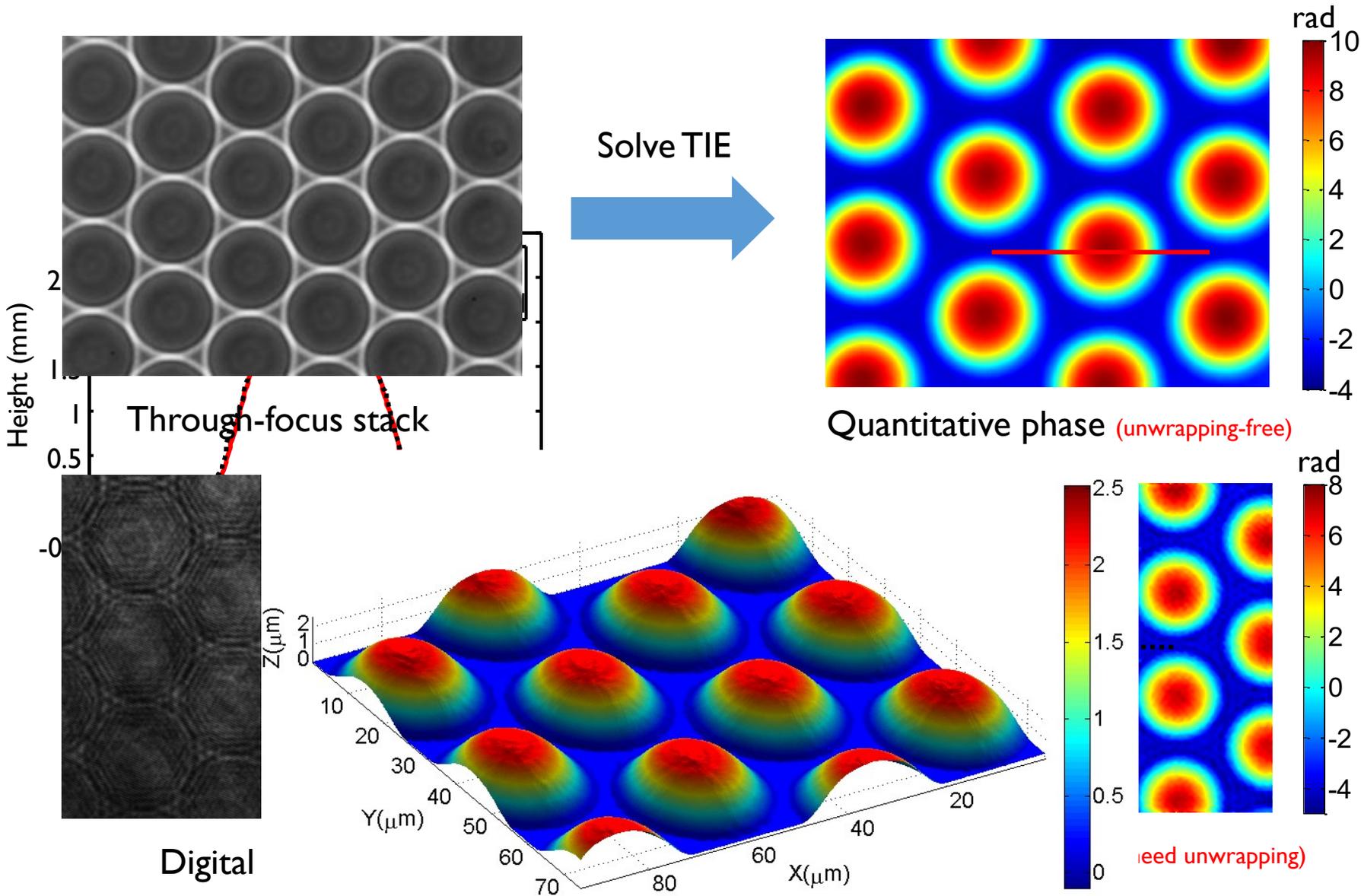


d'Optron
Dynamic vision of new Dimensions

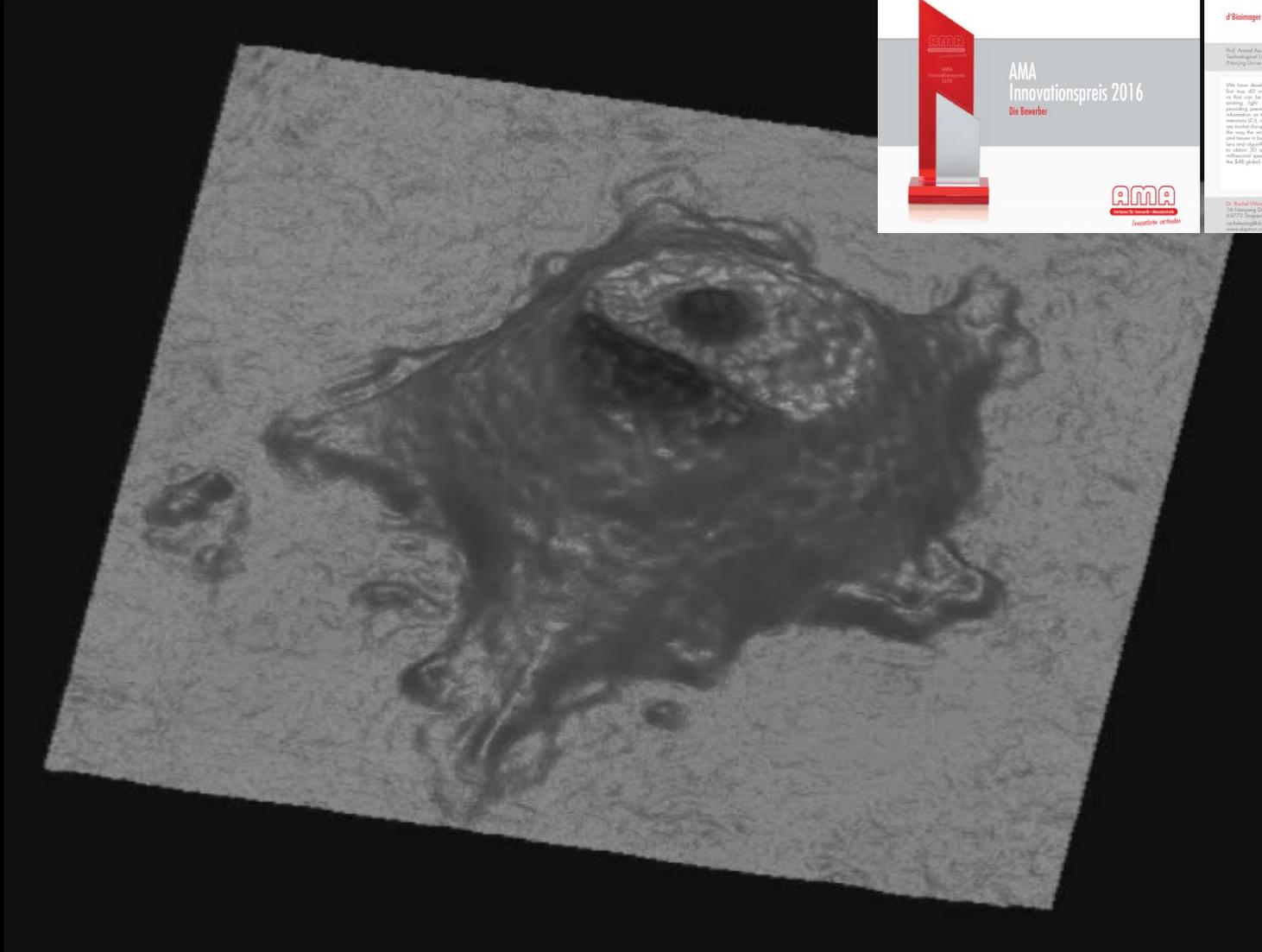


Use d'Biomager with any light microscope

Dynamic TIE microscopy



Dynamic TIE microscopy



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(10) International Publication Number
WO 2015/002614 A1

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Innovationspreis
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Who have developed the world's first true 2D microscopy camera that can be attached to any existing light microscope. By providing previously unavailable information on how individual cells respond to light, our camera permits us to watch the action by changing the way the world looks at cells and tissues in 3D. By combining the power of advanced sensors and algorithms based on terahertz electron optics, we are able to obtain 2D quantitative phase information of transparently thin, sub-micron sized cells. With our new camera system, we can generate the 2D global microscopy image.

Dr. Ruchal Wang Qu, Dr. Ruchal Wang Qu, Thomas Bismayer, Philipp Technolab, University of Applied Sciences, Paderborn, Dr. Zuo Chen, Peking University of Science and Technology.

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2016
Die Bewerber

AMA
Innovationspreis
2016
Die Bewerber

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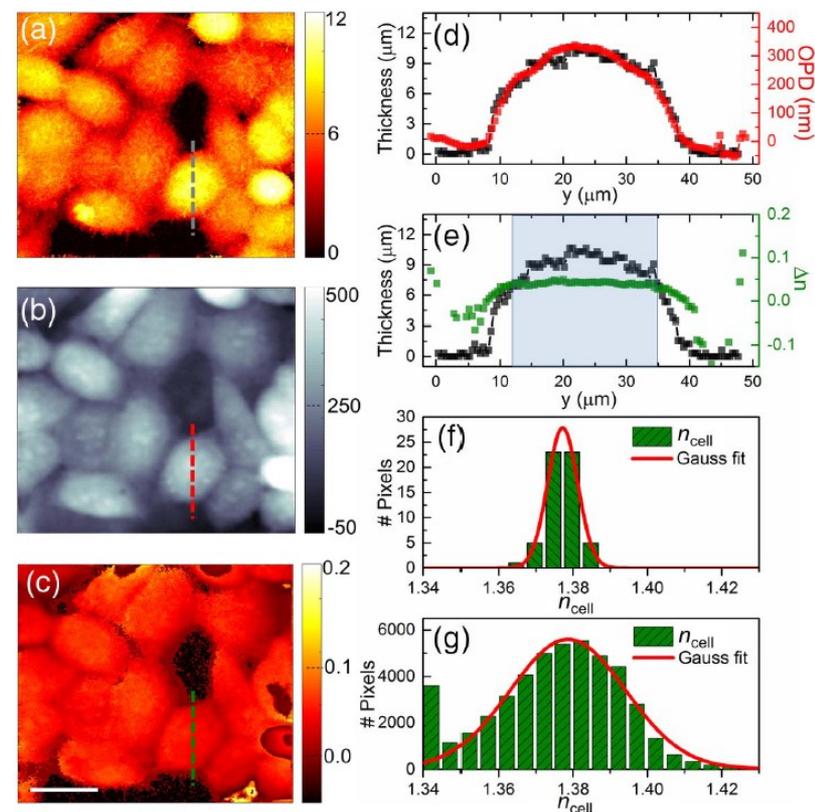
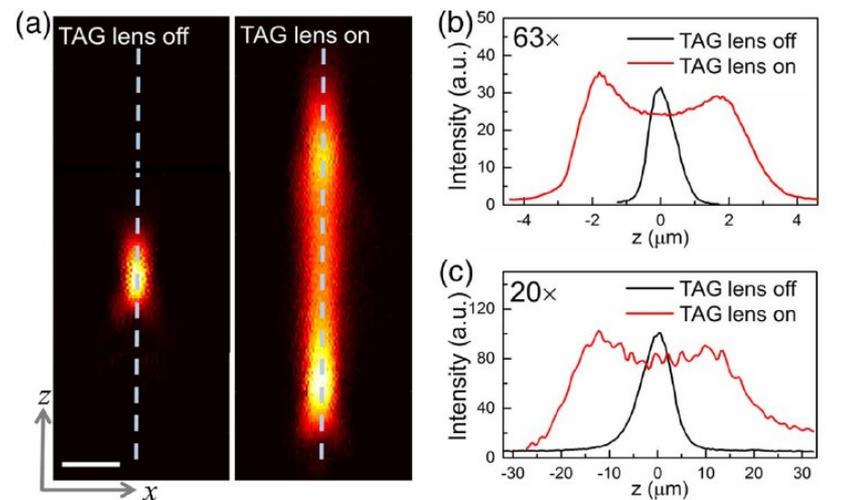
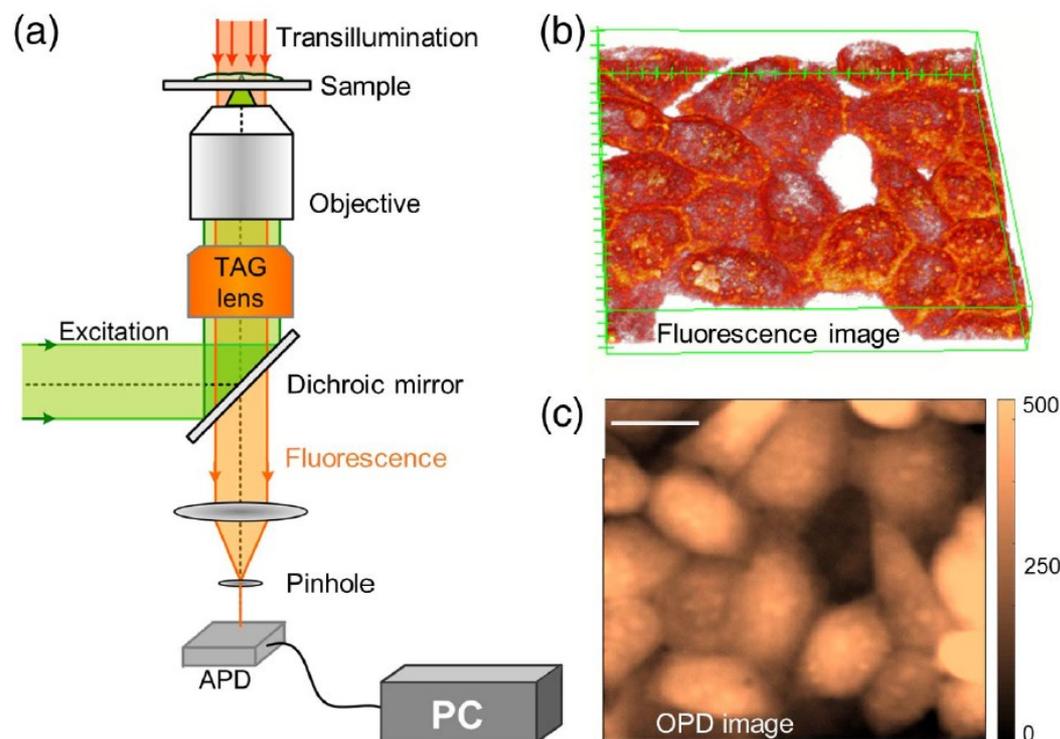
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Fax: +65 64602284

Dual-mode phase and fluorescence imaging with a confocal laser scanning microscope

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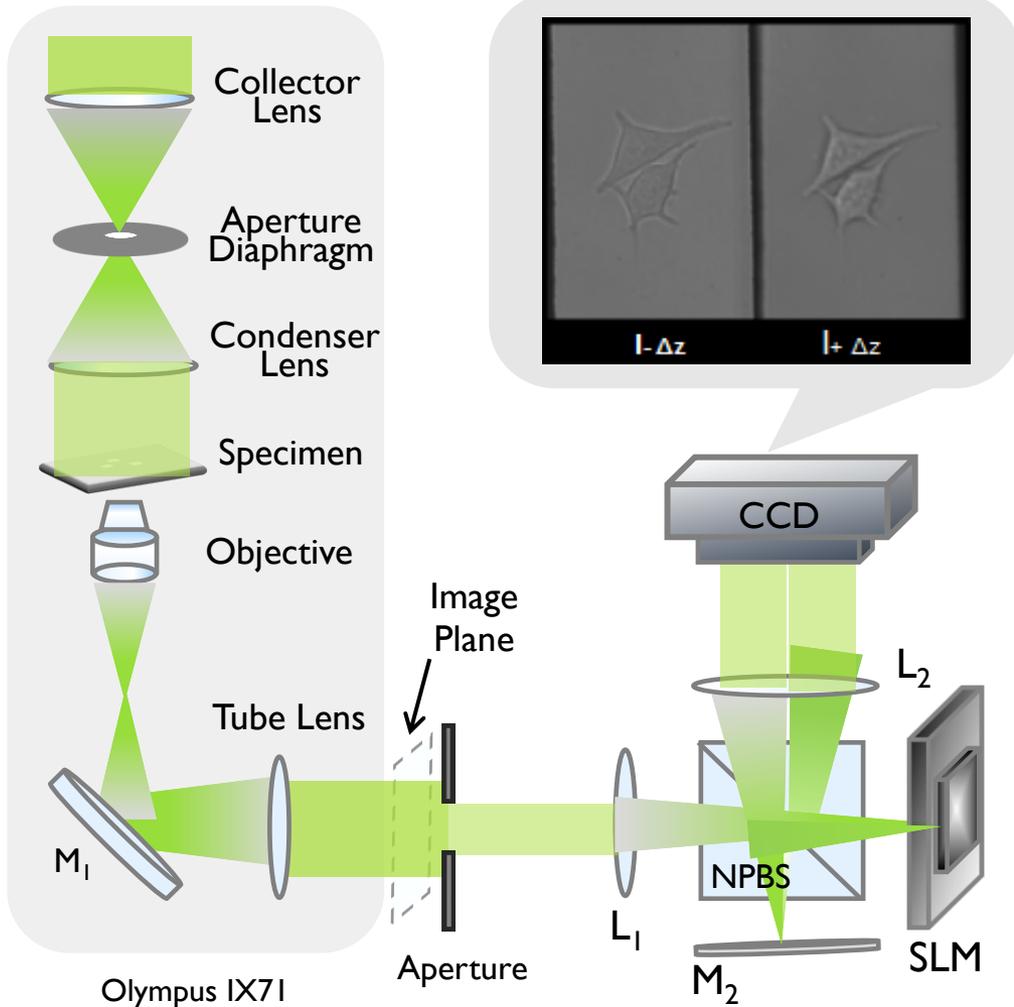
*Corresponding author: uli@uiuc.edu

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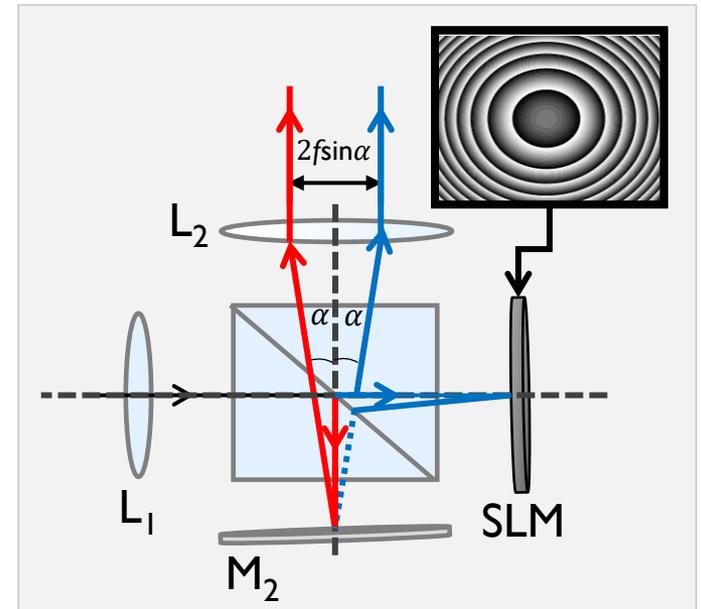
Dynamic TIE microscopy

Single-shot quantitative phase microscopy (SQPM)



Free space
Propagation kernel

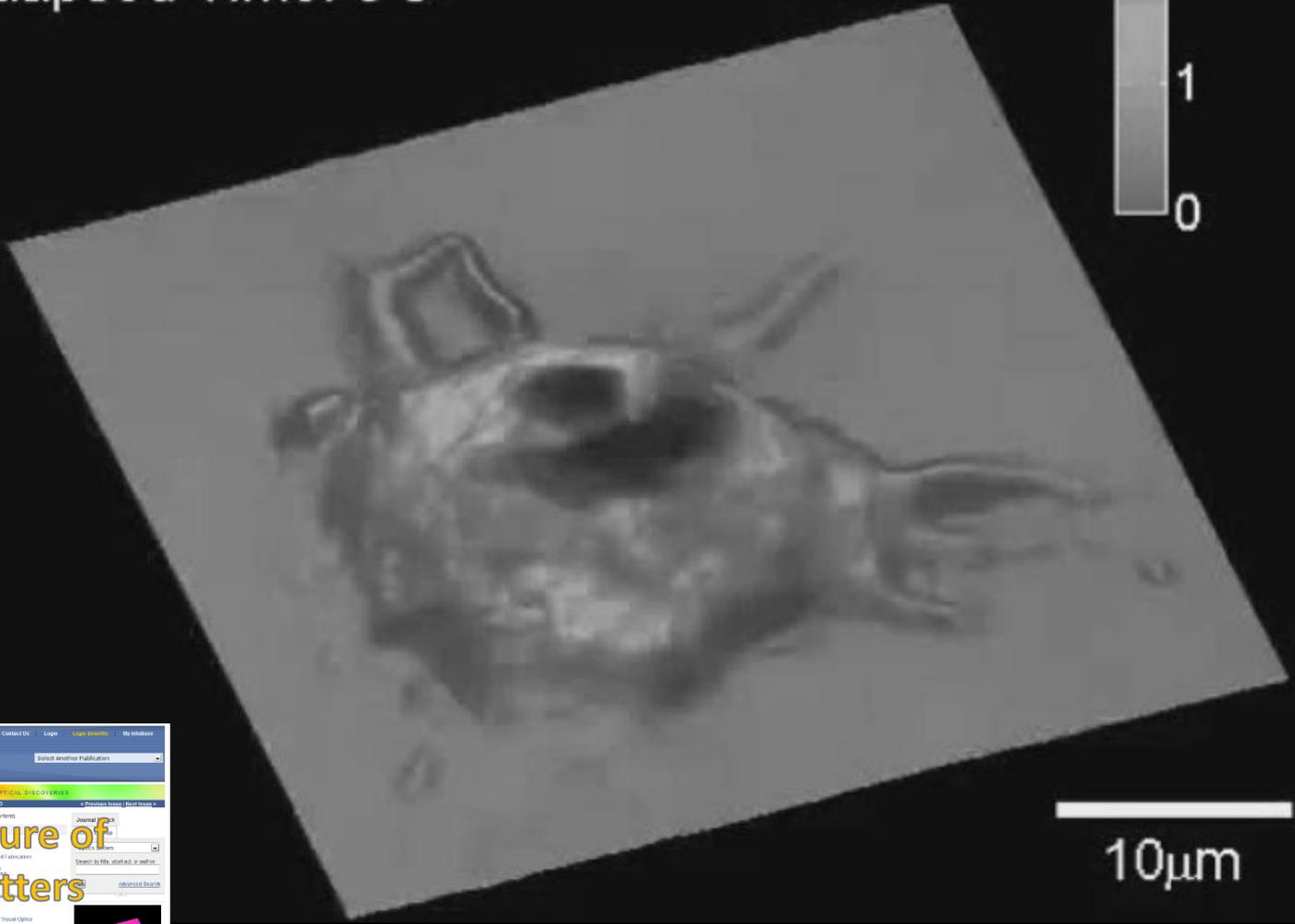
$$\exp\left(-i2\pi\Delta z\sqrt{1 - (\lambda\xi)^2 - (\lambda\eta)^2} / \lambda\right)$$



Dynamic TIE microscopy

Elapsed Time: 0 s

Phase [rad]



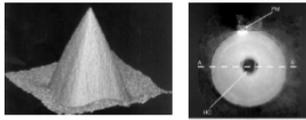
10 μ m

A screenshot of the OpticsInfoBase website. The page features a navigation menu on the left with categories like Home, Current Issue, Past Issues, and About. The main content area displays a table of contents for 'Optics Letters' with various article titles and authors. A small thumbnail image of a fly is visible in the bottom right corner of the screenshot. The text 'Cover feature of Optics Letters' is overlaid on the screenshot in a large, bold, yellow font.

Transport of intensity equation

2000-2008

Applications to TEM and neutron, and atom imaging [163-173]



2010-2015

High-order finite difference and OSF for Multi-plane TIE [188, 194-199, 204, 205, 273-275, 366, 367]

2014-2015

DCT-based solutions under inhomogeneous boundary conditions [200-202]

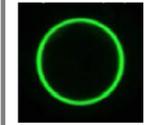
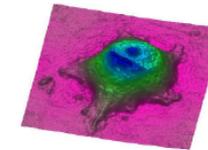
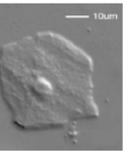
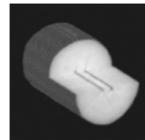
2014-2015

Generalized TIE in phase space [206, 207]

$$\frac{\partial I(\mathbf{x})}{\partial z} = -\nabla_{\mathbf{x}} \cdot \iint \lambda \mathbf{u} W_{\omega}(\mathbf{x}, \mathbf{u}) d\mathbf{u} d\omega$$

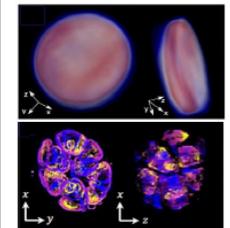
1999-2000

Frist demonstration of Quantitative phase tomography [162, 175]



2017-2019

Resolution enhancement by illumination engineering [208-210, 355, 369-371]

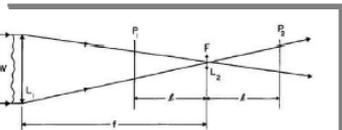


2015-2019

Transport of intensity diffraction tomography [211-213, 389, 395, 395, 407]

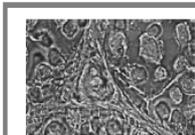
1988-1990

Frist application to adaptive optics (curvature sensing) [144-146]



1984

Frist exploration of partially coherence and optical microscopy [142]



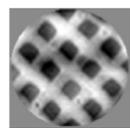
1982-1983

TIE derived [140, 141]

$$-k \frac{\partial I(\mathbf{x}, z)}{\partial z} = \nabla \cdot [I(\mathbf{x}, z) \nabla \phi(\mathbf{x})]$$

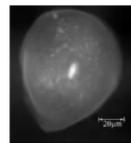
1995-1996

Frist applications to X-ray imaging [159, 160]



1998

Poynting vector Interpretation [158]

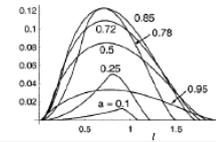


1998

Frist demonstration of quantitative optical phase microscopy [174]

2010

Compatibility to DIC microscope [187]

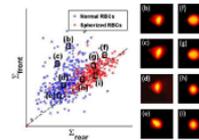


2002

Transfer function analysis [176, 178]

2012-2013

Dynamic TIE phase microscopy for live cells [193, 215, 216]



Transport of intensity equation

$$-k \frac{\partial I(\mathbf{x}, z)}{\partial z} = \nabla \cdot [I(\mathbf{x}, z) \nabla \phi(\mathbf{x})]$$

Solution

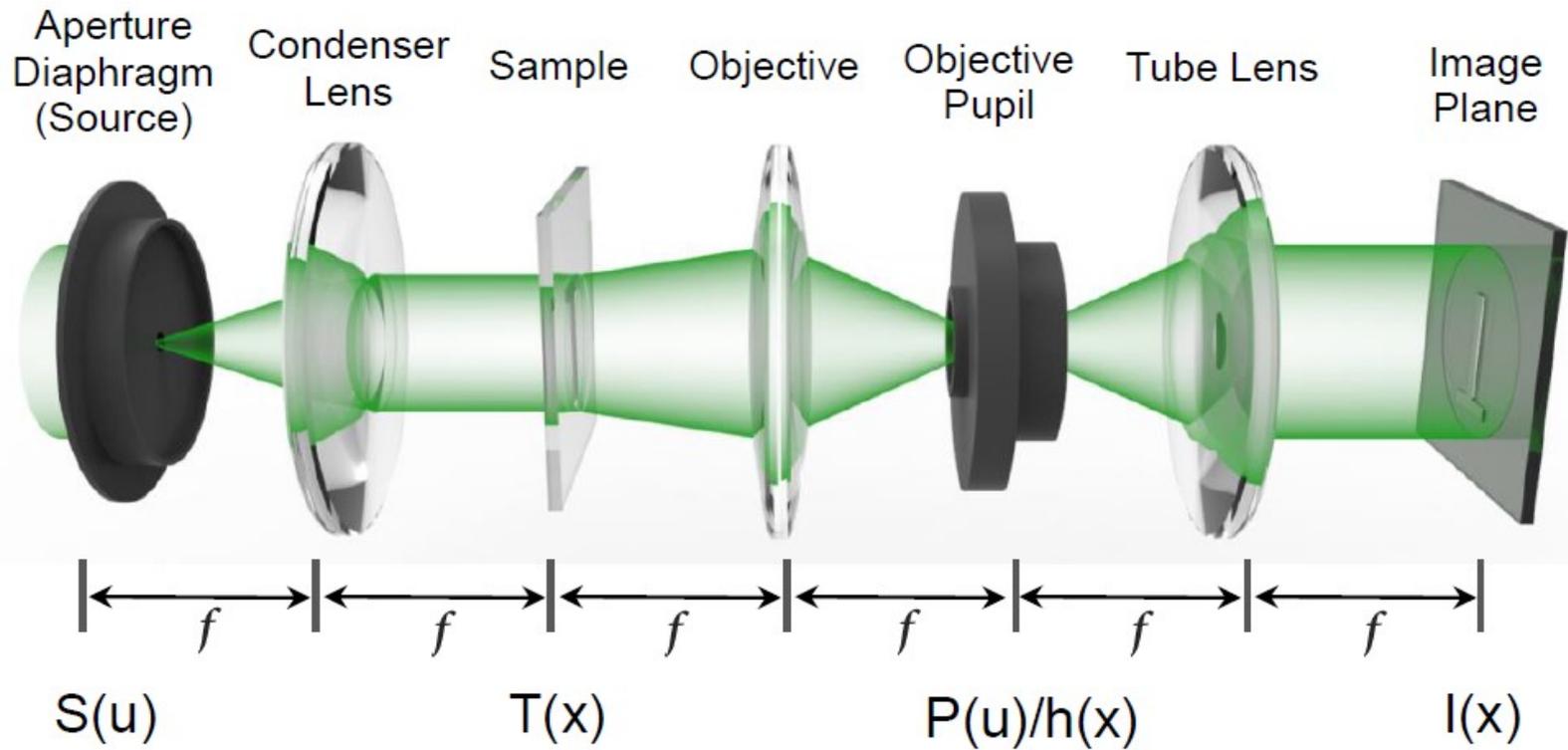
$$\phi(\mathbf{x}) = -k \nabla^{-2} \nabla \cdot \left[I^{-1}(\mathbf{x}) \nabla \nabla^{-2} \frac{\partial I(\mathbf{x})}{\partial z} \right]$$

Coherent TIE

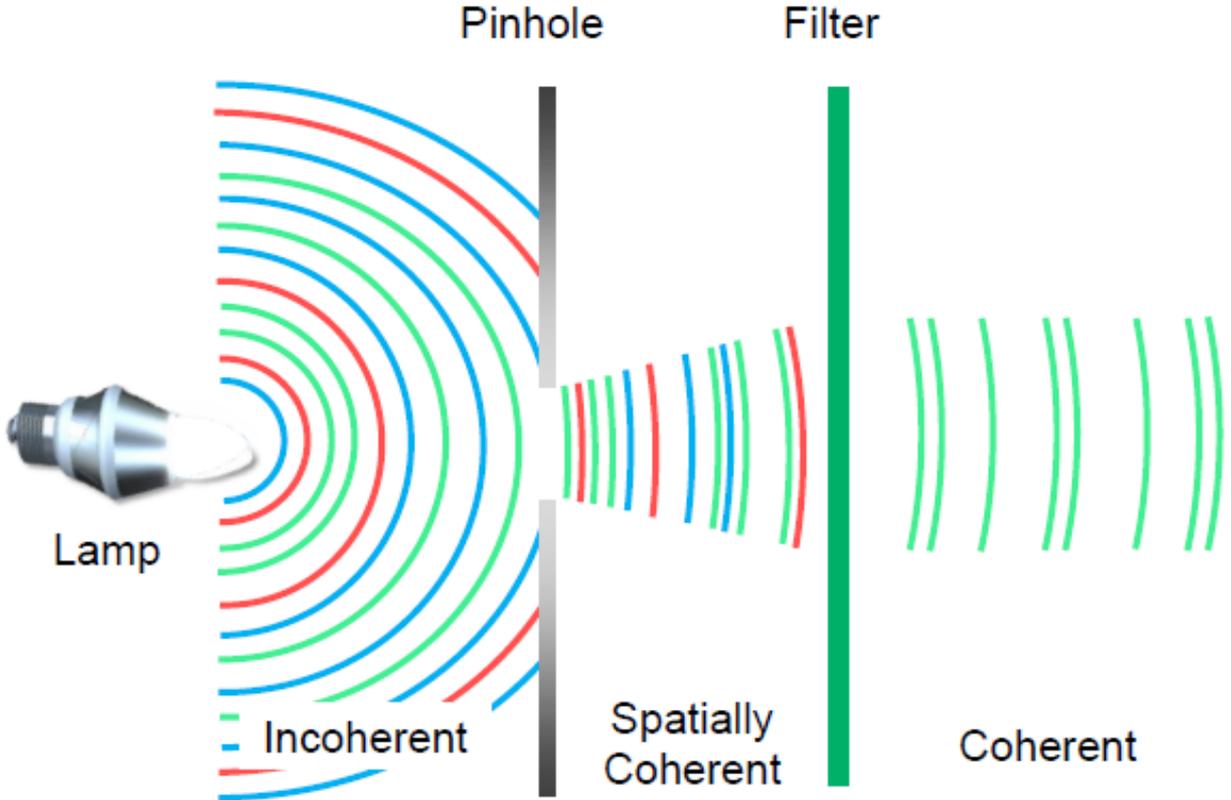
Methods	Approximation conditions	Phase reconstruction algorithms
TIE	Paraxial approximation $\lambda^2 \mathbf{u} ^2 \ll 1$	$-k \frac{\partial I(\mathbf{x})}{\partial z} = \nabla \cdot [I(\mathbf{x}) \nabla \phi(\mathbf{x})]$ Fourier solution:
	Weak defocusing approximation $\Delta z \rightarrow 0$	$\phi(\mathbf{x}) = -k \mathcal{F}^{-1} \left\{ \frac{j2\pi \mathbf{u}}{4\pi^2 \mathbf{u} ^2 + \varepsilon} \mathcal{F} \left[\frac{1}{I(\mathbf{x})} \mathcal{F}^{-1} \left\{ \frac{j2\pi \mathbf{u}}{4\pi^2 \mathbf{u} ^2 + \varepsilon} \mathcal{F} \left[\frac{\partial I(\mathbf{x})}{\partial z} \right] \right\} \right] \right\}$ $\varepsilon > 0$ is a small constant.

Coherent illumination, ideal imaging?

Imaging System



Illumination



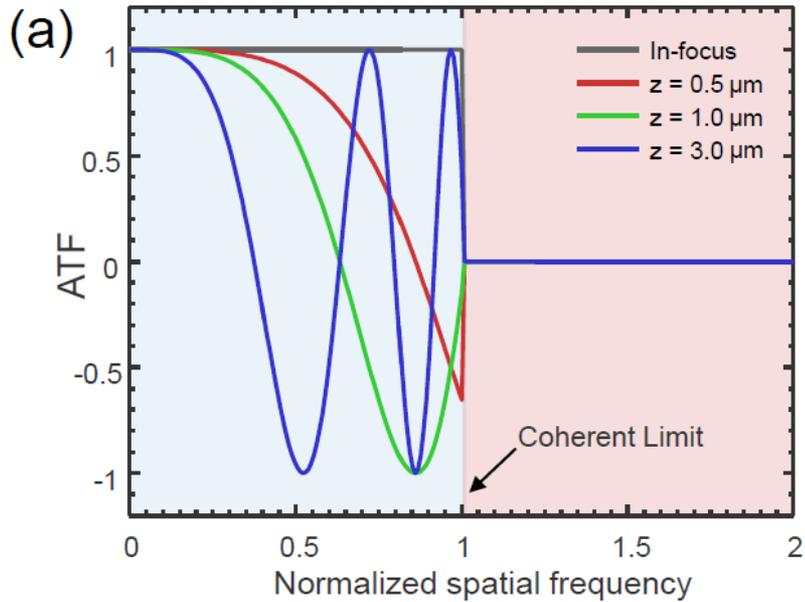
Coherent Imaging System

$$H(\mathbf{u}) = P(\mathbf{u}) H_{\Delta z}(\mathbf{u}) = P(\mathbf{u}) e^{jk\Delta z \sqrt{1-\lambda^2|\mathbf{u}|^2}},$$

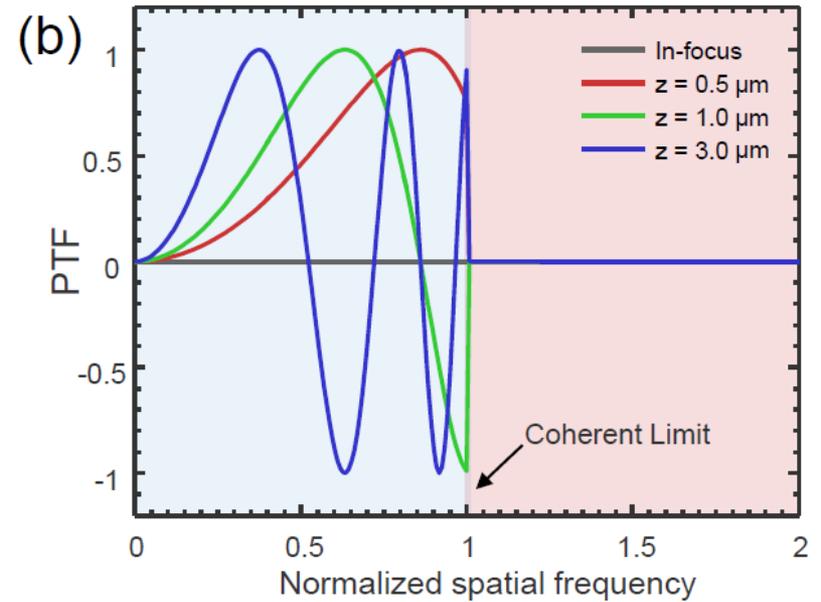
$$P(\mathbf{u}) = \text{circ}\left(\frac{\mathbf{u}}{NA/\lambda}\right) = \begin{cases} 1 & |\mathbf{u}| \leq \frac{NA}{\lambda} \\ 0 & \text{else} \end{cases}$$

$$\begin{aligned} h(r) &= \int_{\rho} \text{circ}\left(\frac{\rho}{NA/\lambda}\right) J_0(2\pi r \rho) 2\pi \rho d\rho \\ &= \frac{NA}{\mu\lambda} J_1\left(2\pi r \frac{NA}{\lambda}\right) \\ &= \pi \left(\frac{NA}{\lambda}\right)^2 \left[\frac{2J_1(\bar{r})}{\bar{r}}\right] \end{aligned}$$

Coherent Limit

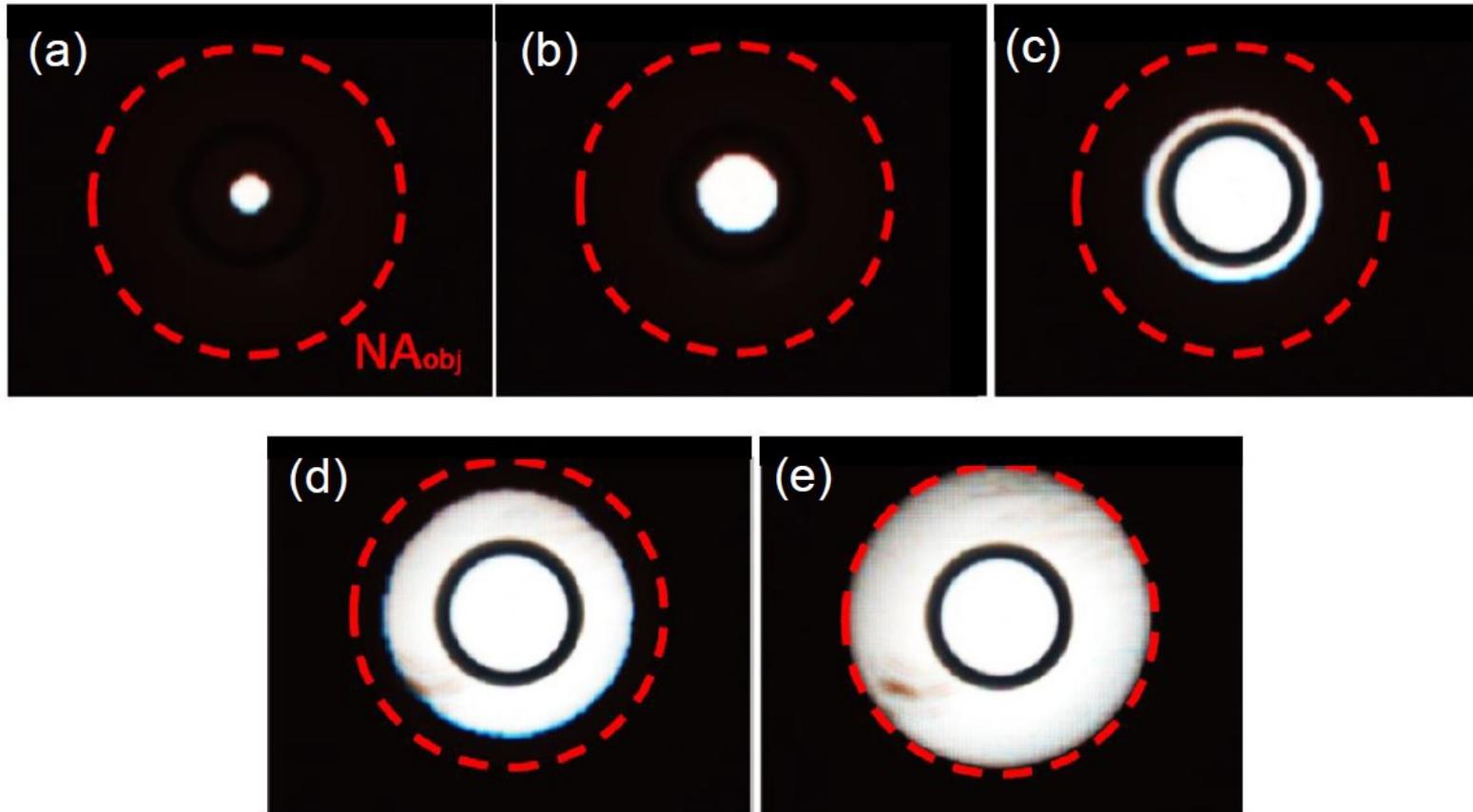


Amplitude



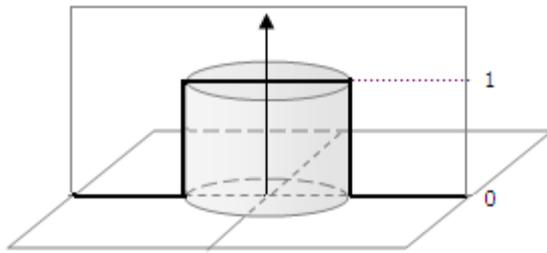
Phase

Coherence in a microscope

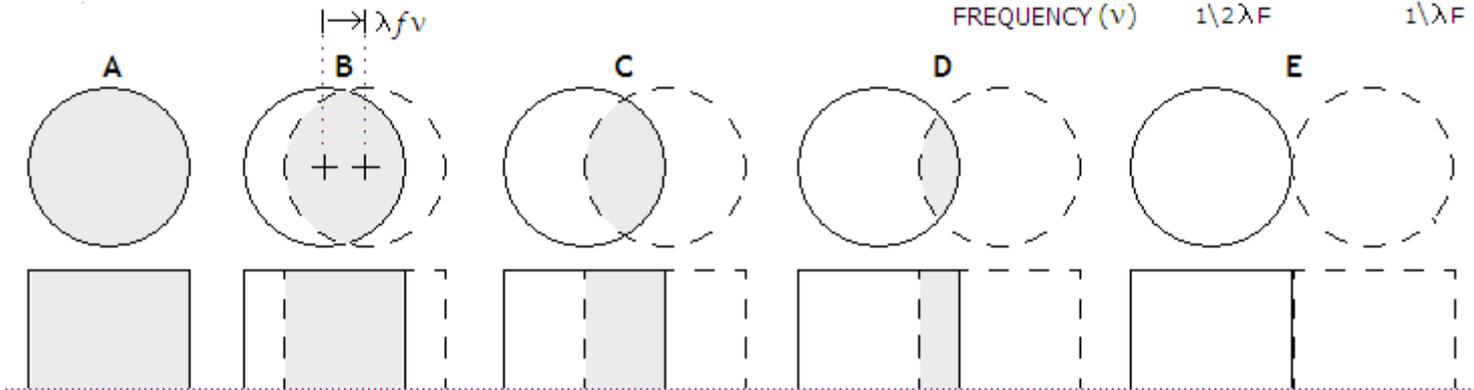
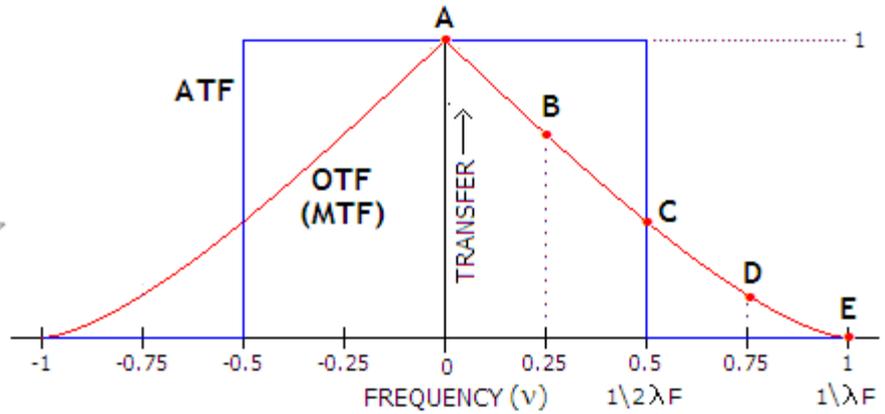


Coherent Limit

PUPIL FUNCTION
(ABERRATION-FREE CIRCULAR)



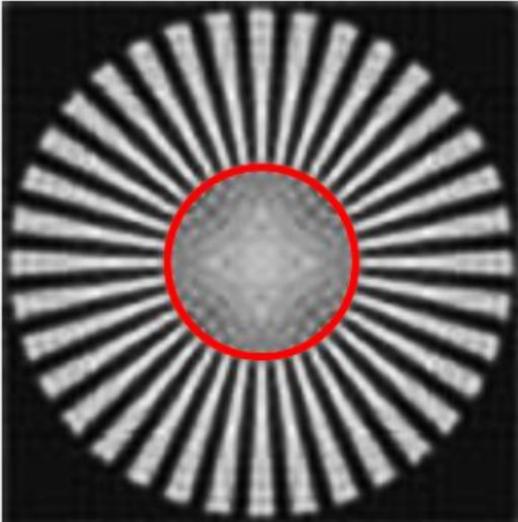
TRANSFER FUNCTION



PUPIL FUNCTION AUTOCORRELATION

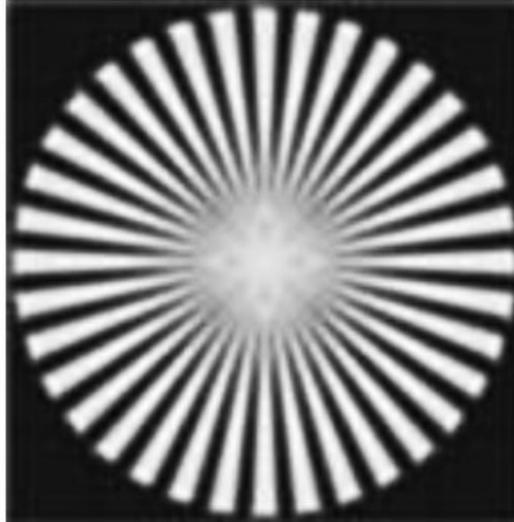
Coherent Limit

coherent

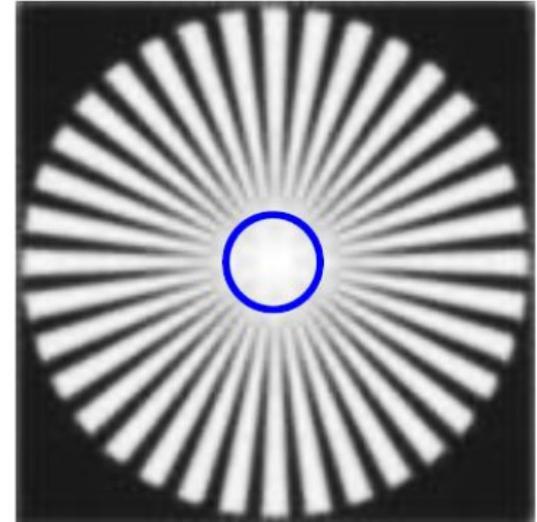


frequency
 $\nu_o = \sin u / \lambda$

partial coherent



incoherent



frequency
 $\nu_o = 2 \sin u / \lambda$

Resolution improvement in DHM

1328 OPTICS LETTERS / Vol. 38, No. 8 / April 15, 2013

Superresolution digital holographic microscopy for three-dimensional samples

Vicente Micó^{1*}, Zeev Zalevsky², Carlos Ferreira¹, and Javier García¹

¹Departamento de Óptica, Universitat de Valencia, C/Dr. Moliner, 50, 46100 Burjassot, Spain

²School of Engineering, Bar-Ilan University, Ramat-Gan, 52900 Israel

*Corresponding author: vicente.mico@uv.es

Resolution improvement in digital holography by angular and polarization multiplexing

Caojin Yuan,^{1,2*} Guohai Situ,² Giancarlo Pedrini,² Jun Ma,² and Wolfgang Osten²

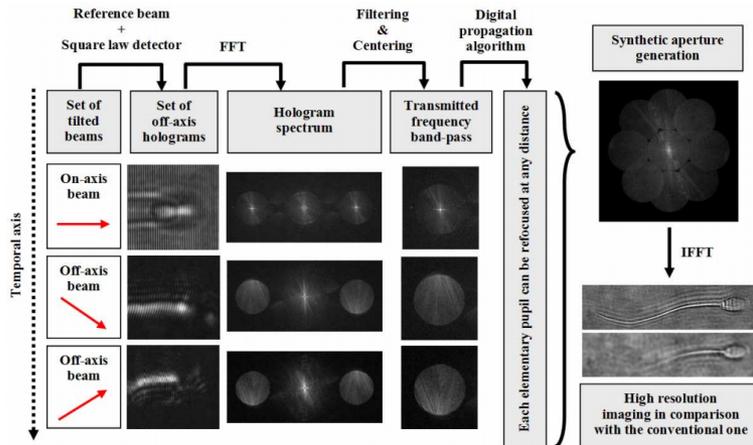


Fig. 3. Schematic chart of the used methodology used where the images depicted in the chart correspond with experimental results obtained with the proposed approach.

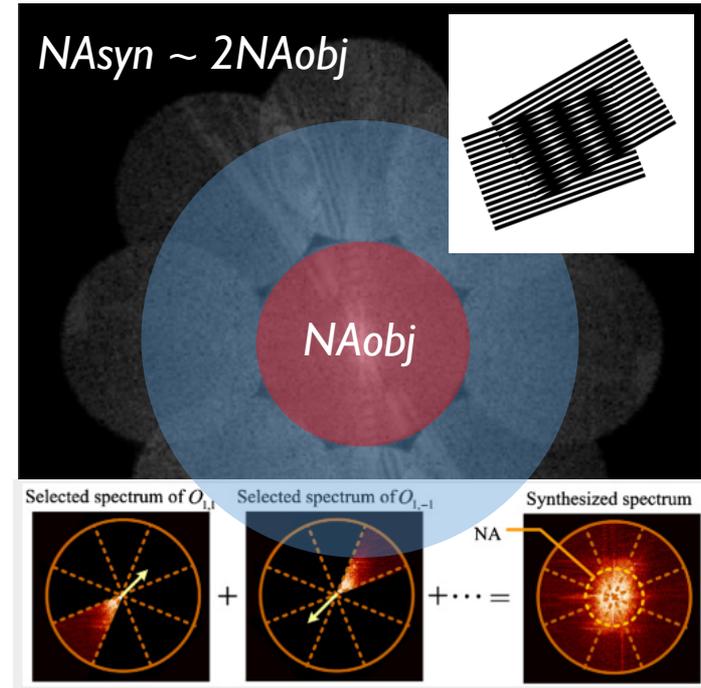
Structured illumination for resolution enhancement and autofocusing in digital holographic microscopy

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²State Key Laboratory of Transient Optics and Photonics, Xi'an Institute of Optics and Precision Mechanics, Chinese Academy of Sciences, Xi'an 710119, China

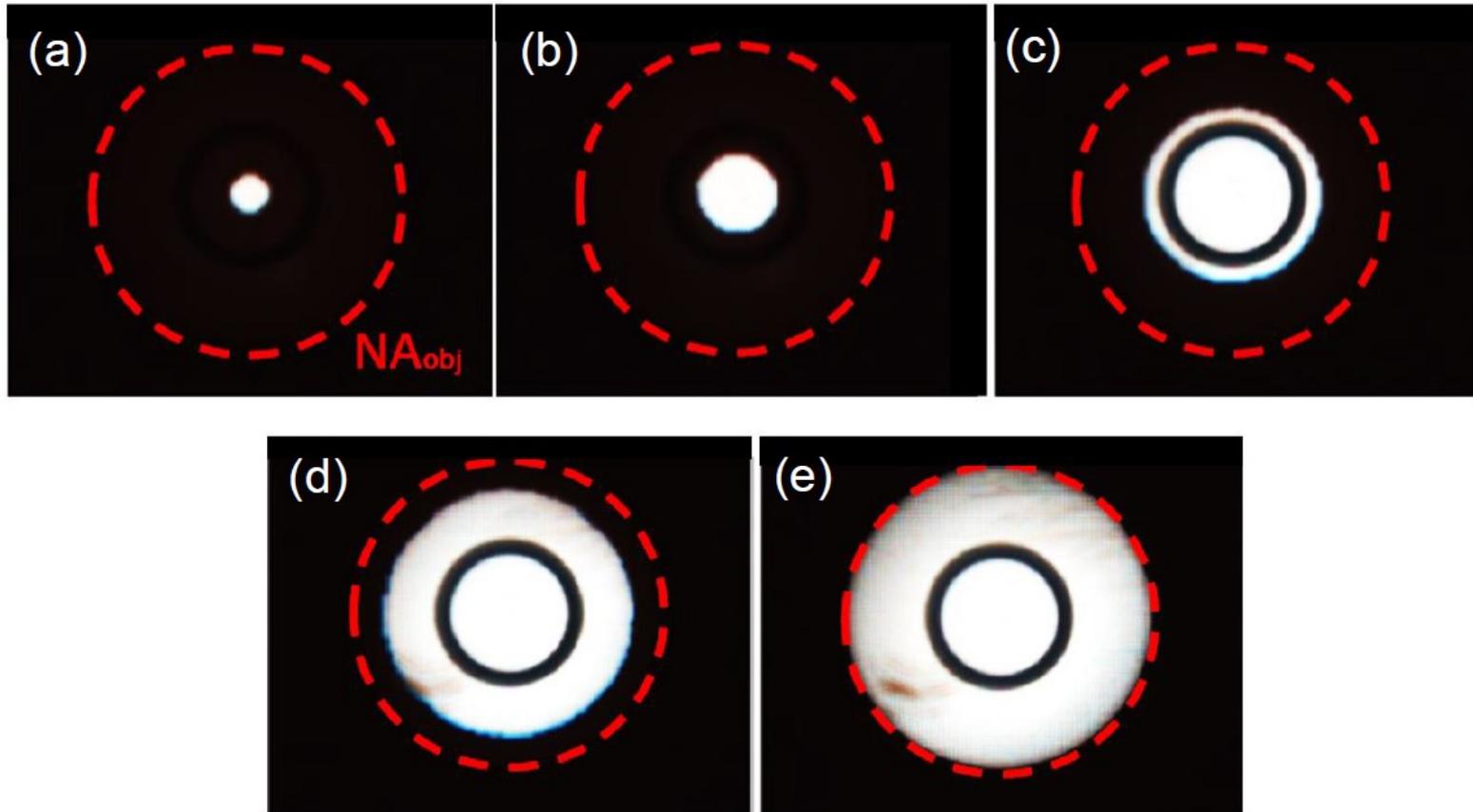
*Corresponding author: peng.gao@ito.uni-stuttgart.de



Synthetic Aperture (Beam scanning or Structured illumination)

Multi-angle measurement to achieve $\sim 2NA_{obj}$

Coherence in a microscope



No interference

Incoherent light:

Different wavelengths
Different phases



Monochromatic,
incoherent light

Same wavelength
Different phases



Coherent light:

Same wavelength
Same phase



Transport of intensity equation ?

$$-k \frac{\partial I(\mathbf{x}, z)}{\partial z} = \nabla \cdot [I(\mathbf{x}, z) \nabla \phi(\mathbf{x})]$$

Effect of partially coherent illumination



$$I(x, y) = \langle U(x, y) U^*(x, y) \rangle = |U(x, y)|^2$$

Purely coherent field



$$W(\mathbf{x}, \mathbf{u}) = \langle U(\mathbf{x}_1, \mathbf{y}_1) U^*(\mathbf{x}_2, \mathbf{y}_2) \exp(-i2\pi \mathbf{u} \cdot \mathbf{x}') \rangle$$

Partially coherent field

Transport of intensity equation ?

$$-k \frac{\partial I(\mathbf{x}, z)}{\partial z} = \nabla \cdot [I(\mathbf{x}, z) \nabla \phi(\mathbf{x})]$$

Generalized transport of intensity equation

$$\frac{\partial I(\mathbf{x})}{\partial z} = -\nabla_{\mathbf{x}} \cdot \iint \lambda \mathbf{u} W_{\omega}(\mathbf{x}, \mathbf{u}) d\mathbf{u} d\omega$$

OPTICS LETTERS / Vol. 39, No. 3 / February 1, 2014

Light field moment imaging: comment

Chao Zuo,^{1,2,3} Qian Chen,^{1,*} and Anand Asundi²

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Optics and Lasers in Engineering 71 (2015) 20–32

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Transport of intensity phase retrieval and computational imaging for partially coherent fields: The phase space perspective

Chao Zuo^{a,b,*}, Qian Chen^a, Lei Tian^c, Laura Waller^c, Anand Asundi^b

^aJiangsu Key Laboratory of Spectral Imaging & Intelligence Sense, Nanjing University of Science and Technology, Nanjing, Jiangsu Province 210094, China

^bCentre for Optical and Laser Engineering, School of Mechanical and Aerospace Engineering, Nanyang Technological University, 639798 Singapore

^cDepartment of Electrical Engineering and Computer Sciences, University of California, Berkeley, CA 94720, USA



Generalized transport of intensity equation

$$\frac{\partial I(\mathbf{x})}{\partial z} = -\lambda \nabla_{\mathbf{x}} \cdot \int \mathbf{u} W(\mathbf{x}, \mathbf{u}) d\mathbf{u}.$$

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^cDepartment of Electrical Engineering and Computer Sciences, University of California, Berkeley, CA 94720, USA



Transport of intensity equation

$$-k \frac{\partial I(\mathbf{x}, z)}{\partial z} = \nabla \cdot [I(\mathbf{x}, z) \nabla \phi(\mathbf{x})]$$

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^cDepartment of Electrical Engineering and Computer Sciences, University of California, Berkeley, CA 94720, USA



Generalized Phase

$$\frac{\int \mathbf{u} W(\mathbf{x}, \mathbf{u}) d\mathbf{u}}{\int W(\mathbf{x}, \mathbf{u}) d\mathbf{u}} = \frac{1}{2\pi} \nabla_{\mathbf{x}} \hat{\phi}(\mathbf{x})$$

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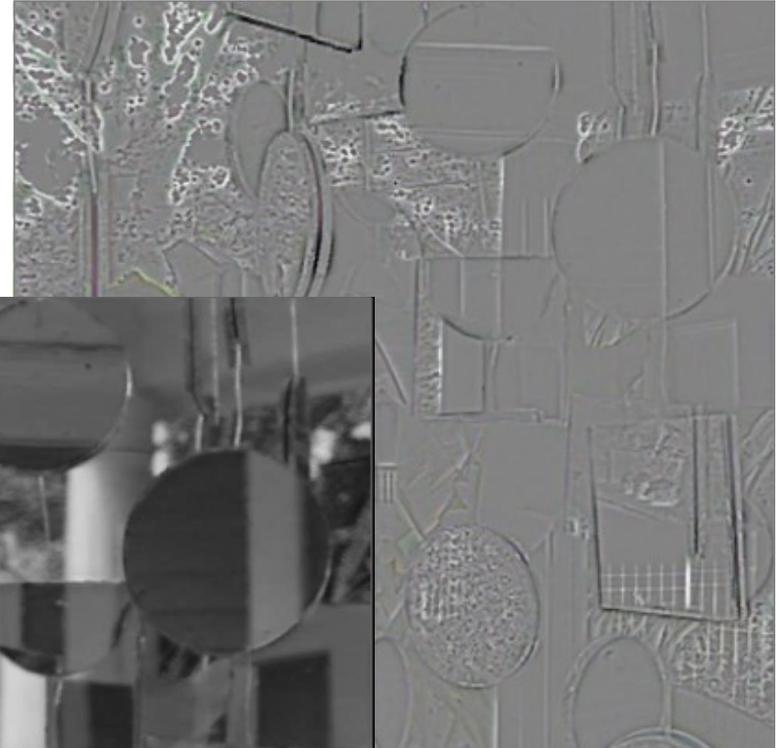
^cDepartment of Electrical Engineering and Computer Sciences, University of California, Berkeley, CA 94720, USA



Light field \sim Wigner distribution

$$L(\mathbf{x}, \theta) \approx W(\mathbf{x}, \lambda \mathbf{u})$$

Computational light field imaging



Two images with slight
 $I(x, y)$

ive $\frac{\partial I(x, y)}{\partial z}$

OPTICS LETTERS / Vol. 38, No. 15 / August 1, 2013

Light field moment

imaging: comment

Antony Orth^{1,2} and Kenneth J. Crozier³

and Anand Asundi²

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²Jiangsu Key Laboratory of Spectral Imaging & Intelligence Sense, Nanjing University of Science and Technology, Nanjing, Jiangsu Province 210094, China

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³e-mail: kcrozier@seas.harvard.edu

Computational light field imaging



OPTICS LETTERS / Vol. 38, No. 15 / August 1, 2013

Light field m

aging: comment

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Generalized Phase

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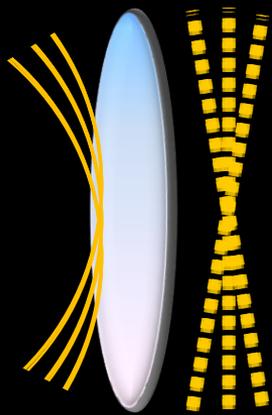
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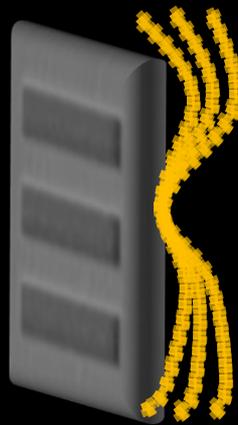
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Phase of the object



$$W_{in} \mathbf{x}, \mathbf{u}$$



$$W_T \mathbf{x}, \mathbf{u}$$

$$W_{out} \mathbf{x}, \mathbf{u} = W_{in} \mathbf{x}, \mathbf{u} \otimes_{\mathbf{u}} W_T \mathbf{x}, \mathbf{u}$$

Generalized Phase

$$\frac{\int \mathbf{u} W_{out}(\mathbf{x}, \mathbf{u}) d\mathbf{u}}{\int W_{out}(\mathbf{x}, \mathbf{u}) d\mathbf{u}} = \frac{\int \mathbf{u} W_T(\mathbf{x}, \mathbf{u}) d\mathbf{u}}{\int W_T(\mathbf{x}, \mathbf{u}) d\mathbf{u}} + \frac{\int \mathbf{u} W_{in}(\mathbf{x}, \mathbf{u}) d\mathbf{u}}{\int W_{in}(\mathbf{x}, \mathbf{u}) d\mathbf{u}}$$

OPTICS LETTERS / Vol. 39, No. 3 / February 1, 2014

Light field moment imaging: comment

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^cDepartment of Electrical Engineering and Computer Sciences, University of California, Berkeley, CA 94720, USA



Generalized Phase

$$\nabla_{\mathbf{x}} \hat{\phi}_{out}(\mathbf{x}) = \nabla_{\mathbf{x}} \left[\hat{\phi}_{in}(\mathbf{x}) + \phi(\mathbf{x}) \right]$$

OPTICS LETTERS / Vol. 39, No. 3 / February 1, 2014

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“Zero-moment” condition

$$\int \mathbf{u} W_{in}(\mathbf{x}, \mathbf{u}) d\mathbf{u} = 0$$

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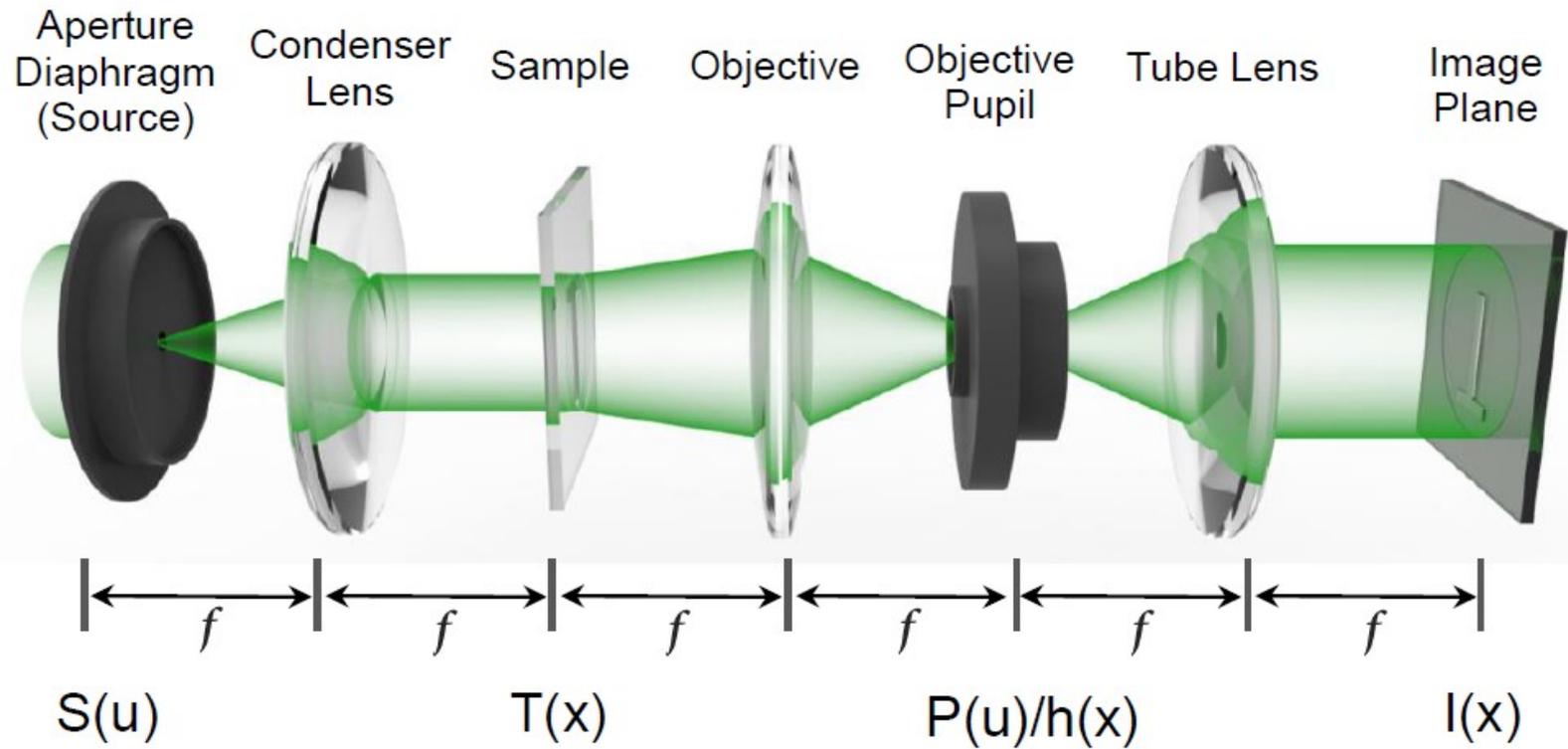
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^cDepartment of Electrical Engineering and Computer Sciences, University of California, Berkeley, CA 94720, USA



Imaging System



Imaging System

$$\begin{aligned} W_{image}(\mathbf{x}, \mathbf{u}) &= \int \Gamma_{image} \left(\mathbf{x} + \frac{\mathbf{x}'}{2}, \mathbf{x} - \frac{\mathbf{x}'}{2} \right) \exp(-j2\pi \mathbf{u} \mathbf{x}') d\mathbf{x}' \\ &= W_{out}(\mathbf{x}, \mathbf{u}) \underset{\mathbf{x}}{\otimes} W_{psf}(\mathbf{x}, \mathbf{u}) \\ &= W_T(\mathbf{x}, \mathbf{u}) \underset{\mathbf{u}}{\otimes} W_{in}(\mathbf{x}, \mathbf{u}) \underset{\mathbf{x}}{\otimes} W_{psf}(\mathbf{x}, \mathbf{u}) \end{aligned}$$

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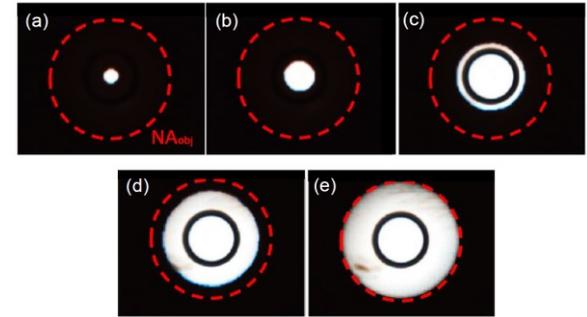
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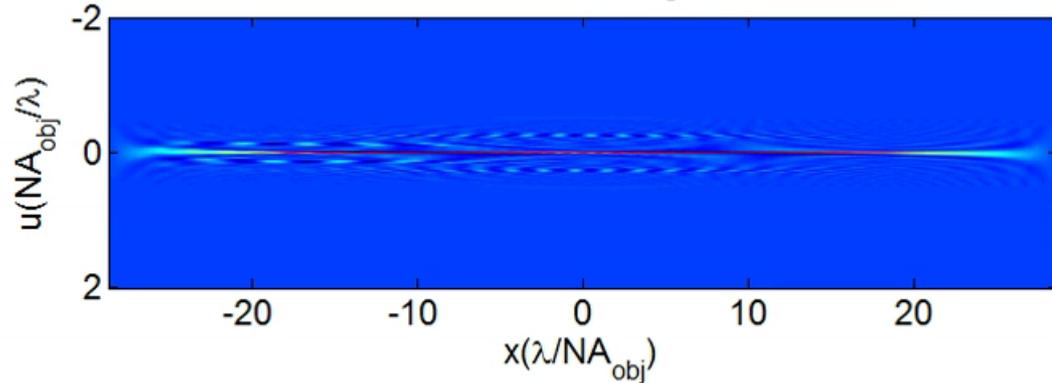


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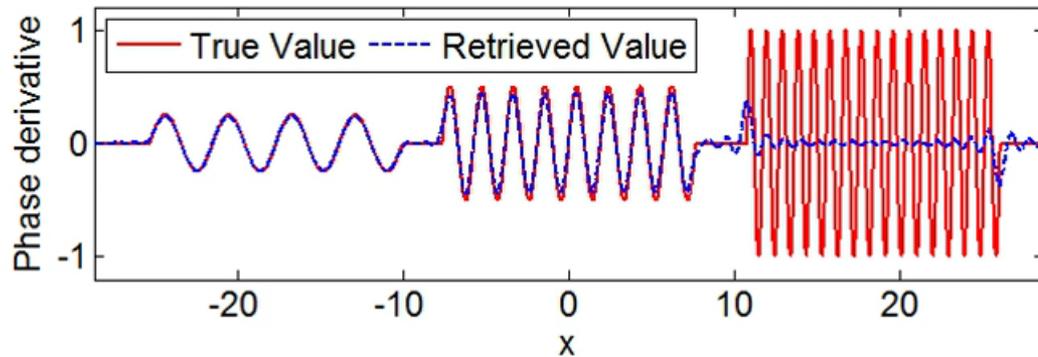
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^bCentre for Optical and Laser Engineering, School of Mechanical and Aerospace Engineering, Nanyang Technological University, 639798 Singapore
^cDepartment of Electrical Engineering and Computer Sciences, University of California, Berkeley, CA 94720, USA

Imaging System

WDF at image plane $W_{\text{image}}(x,u)$, $S = 0.01$



Retrieved phase derivative (first conditional frequency moment)





Invited Paper

Proc. of SPIE Vol. 9718 97180A-1

Phase microscope imaging in phase space

Colin J. R. Sheppard^{*a}, Shalin B. Mehta^b

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^bEugene Bell Center for Regenerative Biology & Tissue Engineering, Marine Biological Laboratory, Woods Hole, MA 02543, USA.

6. THE IMAGE IN PHASE SPACE

This approach can be extended to consider the partial coherence of the image itself. In particular, we can consider the mutual intensity, WDF or ambiguity function of the image. It is important to note that Ψ is not a WDF, and *not* the WDF of the image. The phase space representations of the image have relevance to phase reconstruction methods such as phase space tomography, or the transport of intensity equation approach, and to the 3D image properties.

In phase space tomography, knowledge of the mutual intensity of a wave field in 3D can be used to reconstruct the wave field, including its phase and the correlation coefficient [33-38].

It is interesting to note that Hopkins calculated the image intensity in a partially coherent microscope by propagating the mutual intensity through the system, but did not give an expression for the mutual intensity of the image [23]. The mutual intensity of the image is [39]

$$J(\mathbf{x}_1, \mathbf{x}_2) = \iiint P(\mathbf{m}_1 + \xi) P^*(\mathbf{m}_2 + \xi) S(\xi) T(\mathbf{m}_1) T^*(\mathbf{m}_2) \exp\{i2\pi[(\mathbf{m}_1 + \xi) \cdot \mathbf{x}_1 - (\mathbf{m}_2 + \xi) \cdot \mathbf{x}_2]\} d\mathbf{m}_1 d\mathbf{m}_2 d\xi.$$

[39] Zuo, C., Chen, Q., Tian, L., Waller, L. and Asundi, A. "Transport of intensity phase retrieval and computational imaging for partially coherent fields: The phase space perspective," Optics and Lasers in Engineering 71, 20-32 (2015).

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Phase microscope imaging in phase space

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Colin J. R. Sheppard, Shalin B. Mehta, "Phase microscope imaging in phase space," Proc. SPIE 9718, Quantum Micro Imaging II, 97180A-1 (2015), doi:10.1117/1.2551802

SPIE, Denver, SPIE/BOS, 2015, San Francisco, California, United States

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Proc. of SPIE Vol. 9718 97180A-1



1272 Vol. 35, No. 8 / August 2018 / Journal of the Optical Society of America A **Research**

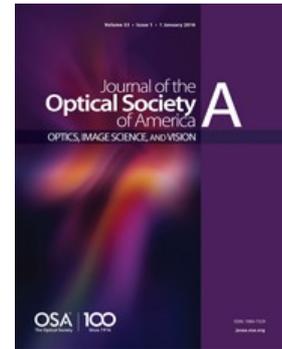
Journal of the
Optical Society A
of America
OPTICS, IMAGE SCIENCE, AND VISION

Partially coherent microscope in phase space

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²Nanophysics, Istituto Italiano di Tecnologia, via Morego 30, 16163 Genova, Italy
³School of Chemistry, University of Wollongong, Northfields Avenue, Wollongong, NSW 2522, Australia
*Corresponding author: colinjrsheppard@gmail.com

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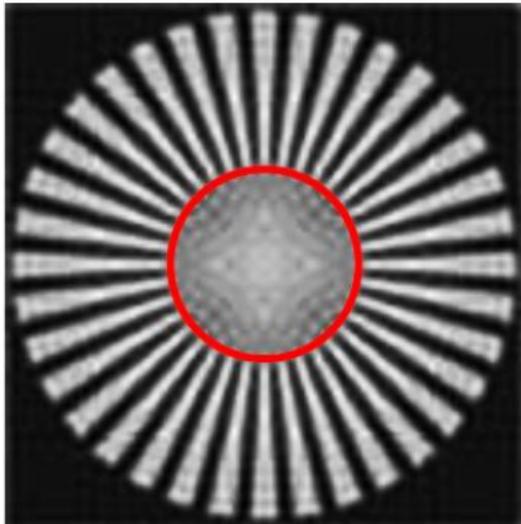
JOSA A 35, 8 (2018)

taken into account [12–14]. Significant advances have been made in describing partially coherent fields with phase space distributions [15]. However, only a few papers have addressed the question of what forward model to use for elegantly capturing the properties of partially coherent imaging [16–18]. Even

16. S. B. Mehta and C. J. R. Sheppard, “Phase-space representation of partially-coherent imaging systems using the Cohen class distribution,” *Opt. Lett.* **35**, 348–350 (2010).
17. S. B. Mehta and C. J. R. Sheppard, “Using the phase-space imager to analyze partially coherent imaging systems: bright-field, phase contrast, differential interference contrast, differential phase contrast, and spiral phase contrast,” *J. Mod. Opt.* **57**, 718–739 (2010).
18. C. Zuo, Q. Chen, L. Tian, L. Waller, and A. Asundi, “Transport of intensity phase retrieval and computational imaging for partially coherent fields: the phase space perspective,” *Opt. Lasers Eng.* **71**, 20–32 (2015).

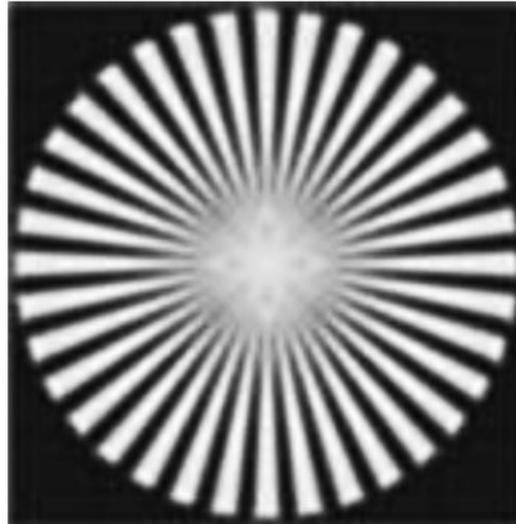
Coherent Limit

coherent

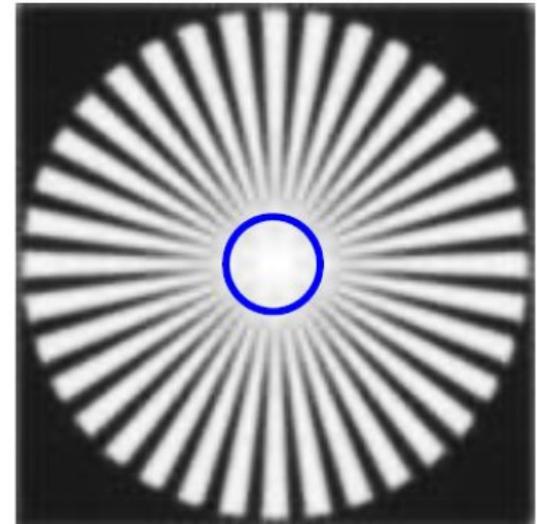


frequency
 $\nu_o = \sin u / \lambda$

partial coherent

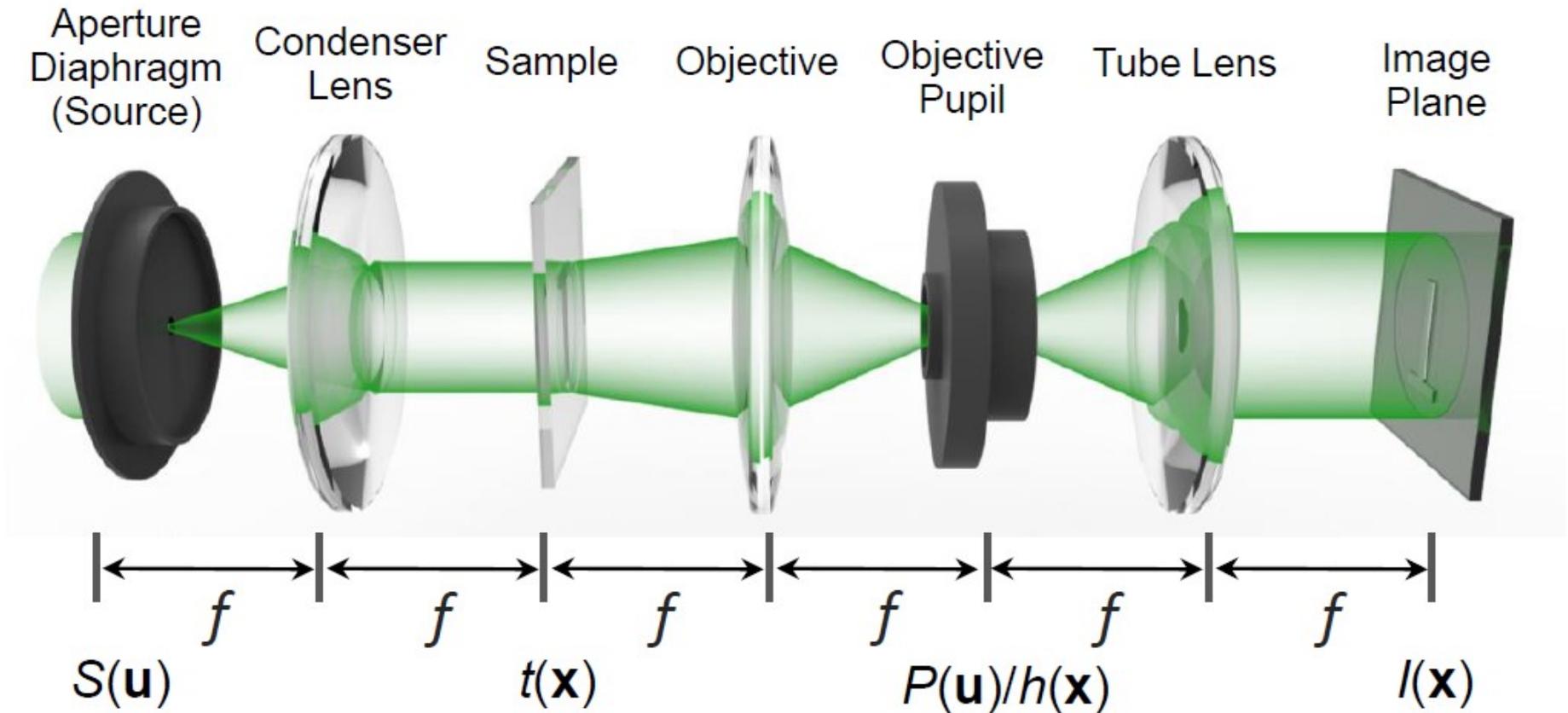


incoherent



frequency
 $\nu_o = 2 \sin u / \lambda$

Tradeoff between resolution and contrast



Microscope based on Köhler Illumination: 6f system

Partially coherent
diffraction limit

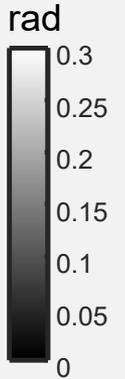
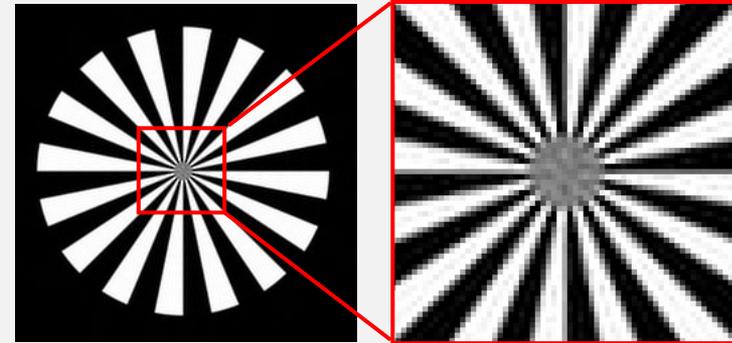
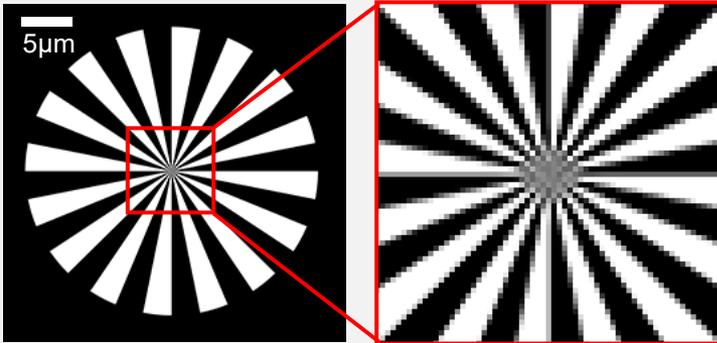
$$NA_{eff} = NA_{obj} + NA_{ill} \leq 2NA_{obj} \quad \text{Incoherent limit}$$

Tradeoff between resolution and contrast

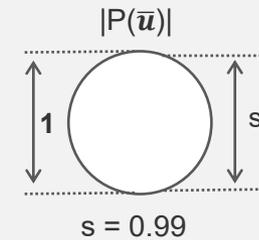
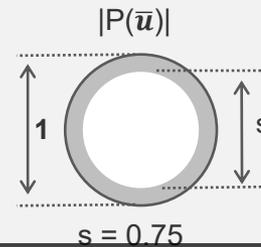
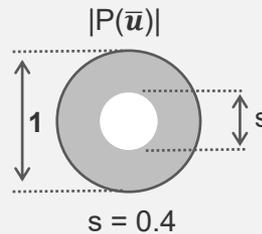
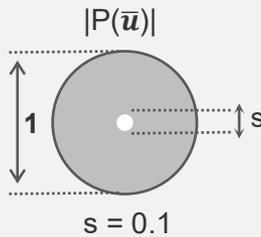
Raw phase image

Diffraction limited ($2NA_{obj}$)

Test Object



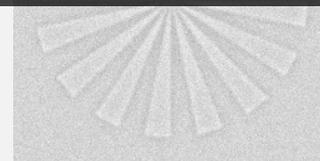
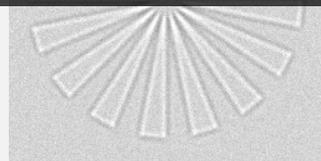
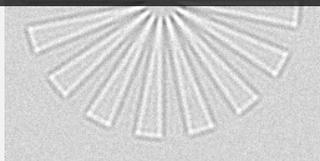
Condenser aperture

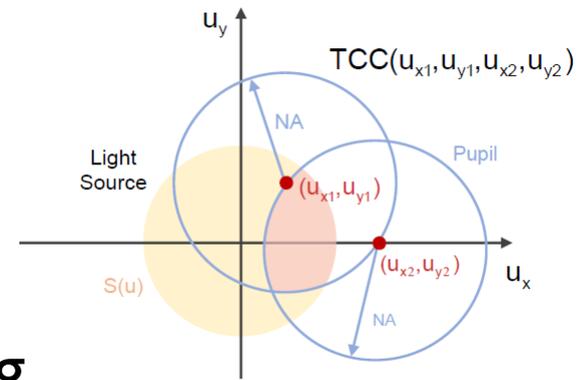


Phase effect gradually vanishes with the increase of $NA_{||}$

Tradeoff between resolution and phase contrast in brightfield microscopy

Defocused Image





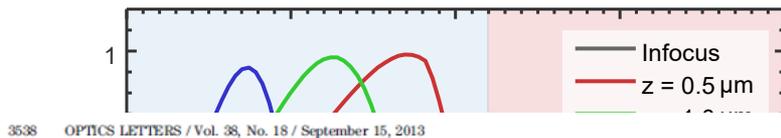
Partially coherent imaging

$$WOTF(\mathbf{u}) \equiv TCC(\mathbf{u}, 0) =$$

$$\iint S(\mathbf{u}') P(\mathbf{u}') P(\mathbf{u}' + \mathbf{u})$$

$$e^{jk\Delta z \left(-\sqrt{1 - \lambda^2 |\mathbf{u}'|^2} + \sqrt{1 - \lambda^2 |\mathbf{u} + \mathbf{u}'|^2} \right)} d\mathbf{u}'$$

Tradeoff between resolution and contrast



3538 OPTICS LETTERS / Vol. 38, No. 18 / September 15, 2013

Noninterferometric single-shot quantitative phase microscopy

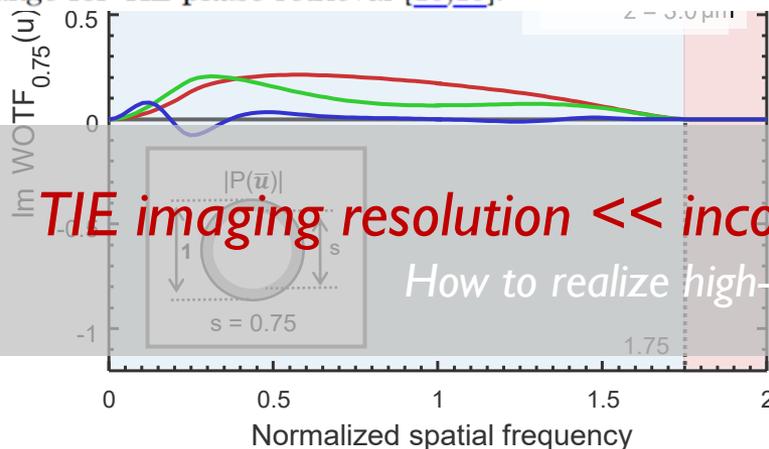
Chao Zuo,^{1,2*} Qian Chen,³ Weijuan Qu,³ and Anand Asundi²

¹Jiangsu Key Laboratory of Spectral Imaging & Intelligence Sense, Nanjing University of Science and Technology, Nanjing, Jiangsu Province 210094, China

²Centre for Optical and Laser Engineering, School of Mechanical and Aerospace Engineering, Nanyang Technological University, Singapore 639798

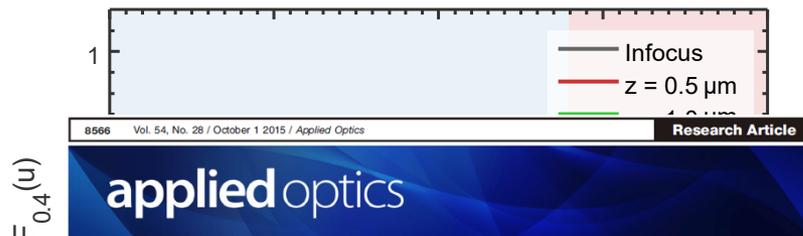
³Centre for Applied Photonics and Laser Technology, Ngee Ann Polytechnic, 535 Clementi Road, Singapore 599489
*Corresponding author: surpasszuo@163.com

($S = NA_{\text{cond}}/NA_{\text{obj}}$). Conventionally, high-resolution optical microscopy depends on the numerical aperture of the condenser being comparable to that of the objective ($S = 0.7 \sim 0.8$). For TIE phase measurements, the results are largely independent of the condenser setting (especially for the low spatial frequency components) [15]. However, in the SQPM, we prefer to narrow down the condenser aperture a bit ($S = 0.3 \sim 0.4$) to ensure a certain level of spatial coherence. This allows a larger depth of field, higher phase contrast on defocus, and, more importantly, a wider linear spatial frequency response range for TIE phase retrieval [15,16].



TIE imaging resolution << incoherent diffraction limit ($2NA_{\text{obj}}$)

How to realize high-resolution TIE imaging?



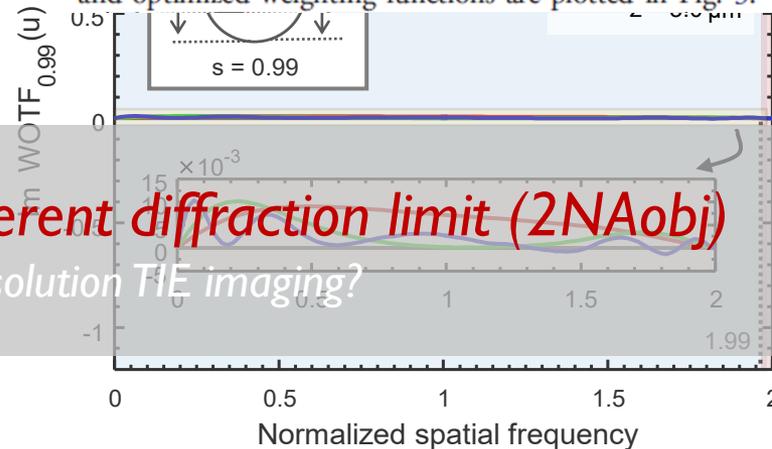
Quantitative phase microscopy via optimized inversion of the phase optical transfer function

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for equally spaced planes whereas a recent study has shown exponentially spaced planes to be a more efficient sampling scheme [69]. In any case, partially coherent TIE methods result in high spatial frequency attenuation as the condenser numerical aperture (NA) is increased [70]. This results in blurry phase reconstructions with lower spatial resolution.

FWHM). The level of partial spatial coherence is determined by $NA_c = 0.375$, which has been set using a condenser (Olympus U-POC-2) aperture diaphragm. Because we have not encountered any need for regularization, α is set to zero and the resulting radially varying partially coherent POTFs and optimized weighting functions are plotted in Fig. 3.

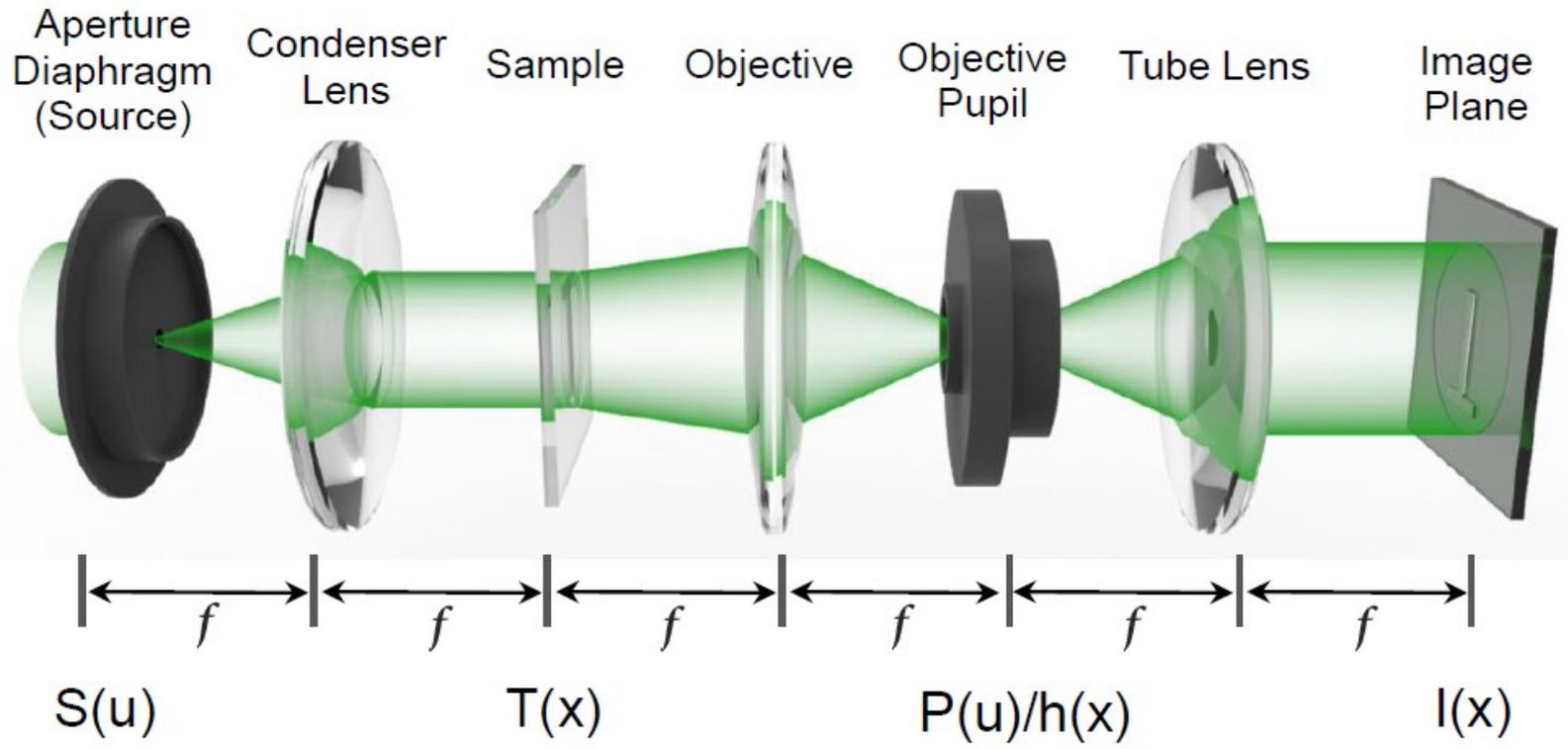


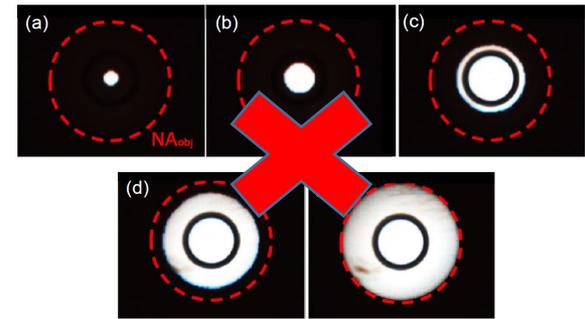
TIE imaging resolution << incoherent diffraction limit ($2NA_{\text{obj}}$)

Transport of intensity equation ?

$$-k \frac{\partial I(\mathbf{x}, z)}{\partial z} = \nabla \cdot [I(\mathbf{x}, z) \nabla \phi(\mathbf{x})]$$

Imaging System !





Illumination Engineering

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SCIENTIFIC REPORTS

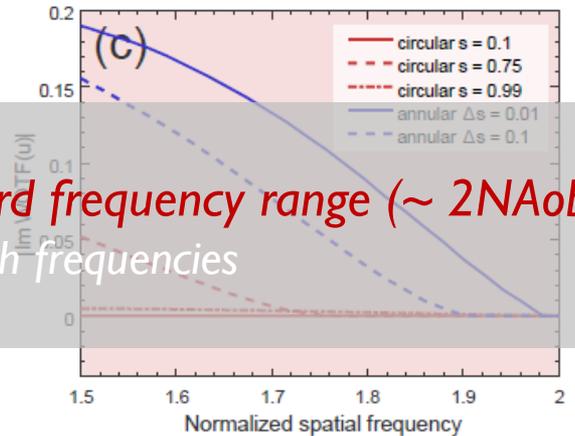
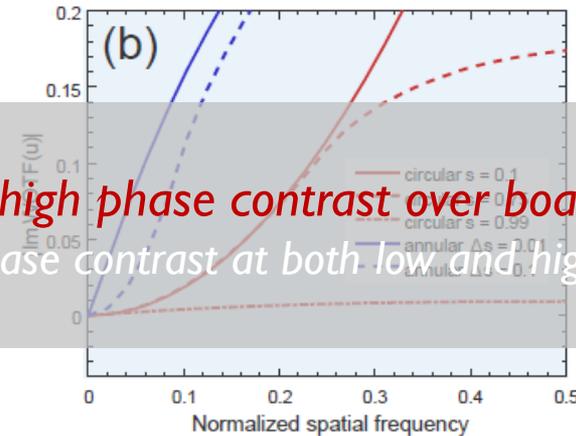
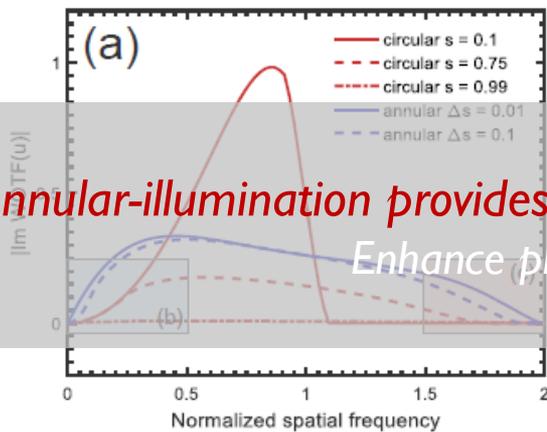
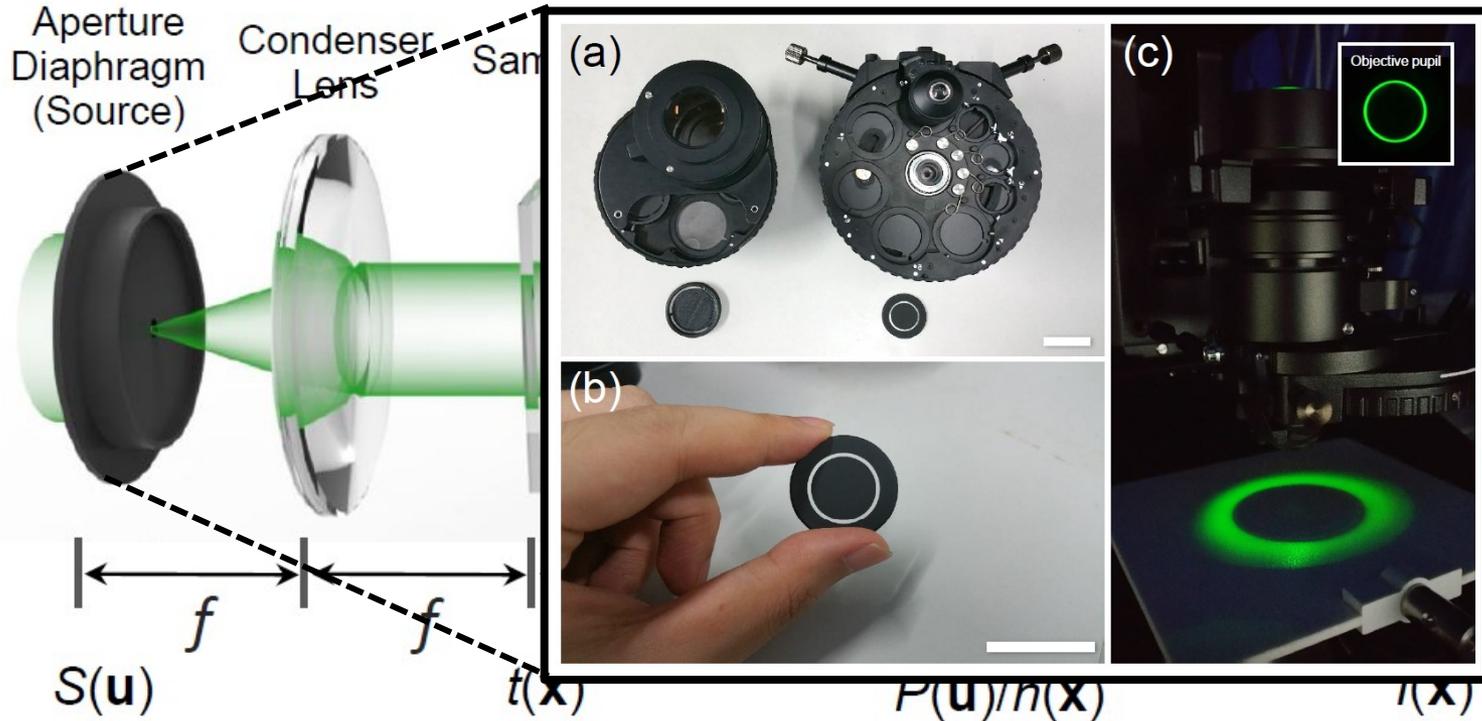
OPEN High-resolution transport-of-intensity quantitative phase microscopy with annular illumination

Received: 1 March 2017
Accepted: 7 June 2017
Published online: 09 August 2017

Chao Zuo^{1,2}, Jiasong Sun^{1,2}, Jiaji Li^{1,2}, Jialin Zhang^{1,2}, Anand Asund³ & Qian Chen²

For quantitative phase imaging (QPI) based on transport-of-intensity equation (TIE), partially coherent illumination provides speckle-free imaging, compatibility with brightfield microscopy, and transverse resolution beyond coherent diffraction limit. Unfortunately, in a conventional microscope with circular illumination aperture, partial coherence tends to diminish the phase contrast, exacerbating the inherent noise-to-resolution tradeoff in TIE imaging, resulting in strong low-frequency artifacts and compromised imaging resolution. Here, we demonstrate how these issues can be effectively addressed by replacing the conventional circular illumination aperture with an annular one. The matched annular illumination not only strongly boosts the phase contrast for low spatial frequencies, but significantly improves the practical imaging resolution to near the incoherent diffraction limit. By incorporating high-numerical aperture (NA) illumination as well as high-NA objective, it is shown, for the first time, that TIE phase imaging can achieve a transverse resolution up to 208 nm, corresponding to an effective NA of 2.66. Time-lapse imaging of *in vitro* HeLa cells revealing cellular morphology and subcellular dynamics during cells mitosis and apoptosis is exemplified. Given its capability for high-resolution QPI as well as the compatibility with widely available brightfield microscopy hardware, the proposed approach is expected to be adopted by the wider biology and medicine community.

Annular-illumination TIE

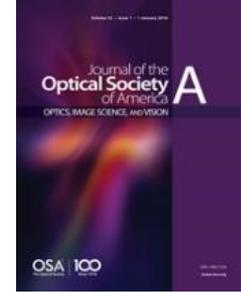


*Annular-illumination provides high phase contrast over board frequency range ($\sim 2NA_{obj}$)
Enhance phase contrast at both low and high frequencies*



Partially coherent microscope imaging system in phase space: effect of defocus and phase reconstruction

COLIN J. R. SHEPPARD^{1,2}



JOSAA
35, 11 (2018)

circular source for $S = 0.613$. In each case the maximum values have been normalized to unity. It is seen that the annular source has a broader spatial frequency response. An interesting and important feature is that the parabolic region for low spatial frequencies for the circular case vanishes for the annular case, so that low spatial frequencies are imaged more efficiently. The imaginary part of the WOTF for different values of defocus has been presented by Zuo *et al.* [40].

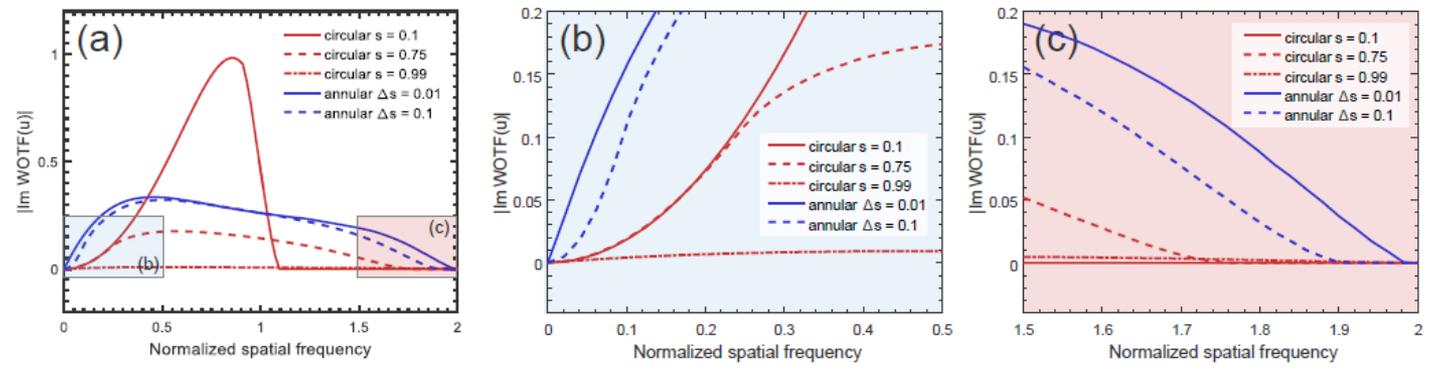
Interestingly, for $S = 1$, $C_{CG}(l)$ is very close to linear over its whole non-zero domain, so this is a good arrangement for performing TIE, but the scaling of the phase would need to be calibrated. We find that

$$C_{CG}(l) = -\frac{2}{\pi} + \left(\frac{\pi^2 - 2}{\pi^2}\right)l + \left(\frac{\pi^2 - 8}{4\pi^3}\right)l^2 + \left(\frac{\pi^2 - 12}{6\pi^4}\right)l^3 + \dots$$

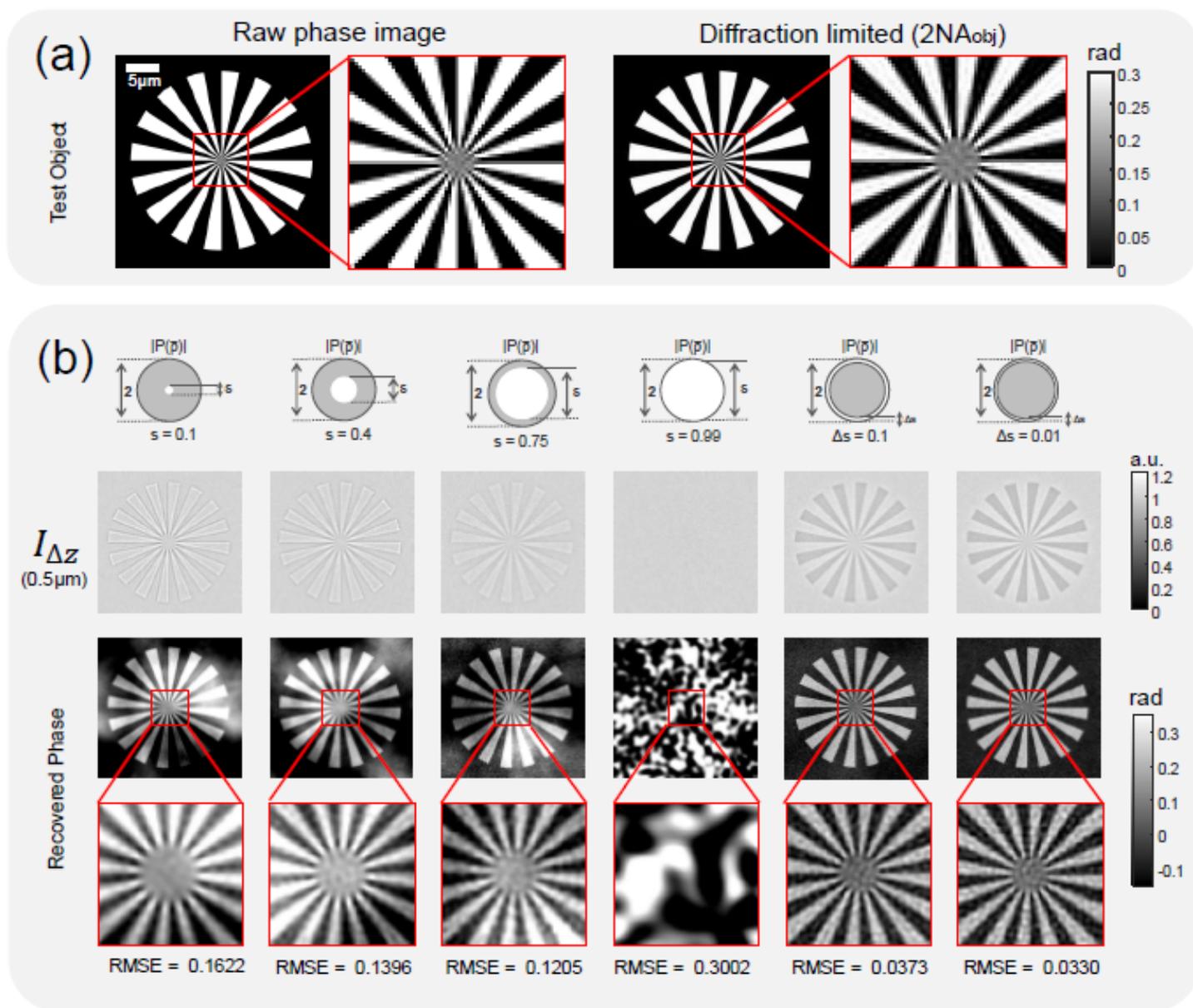
$$= -0.637 + 0.797l + 0.015l^2 - 0.0036l^3 + \dots \quad (53)$$

In fact, using an annular source for the TIE has been proposed by Zuo *et al.* [40].

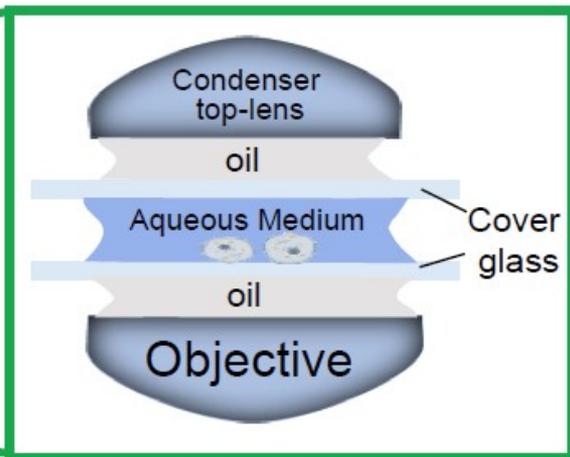
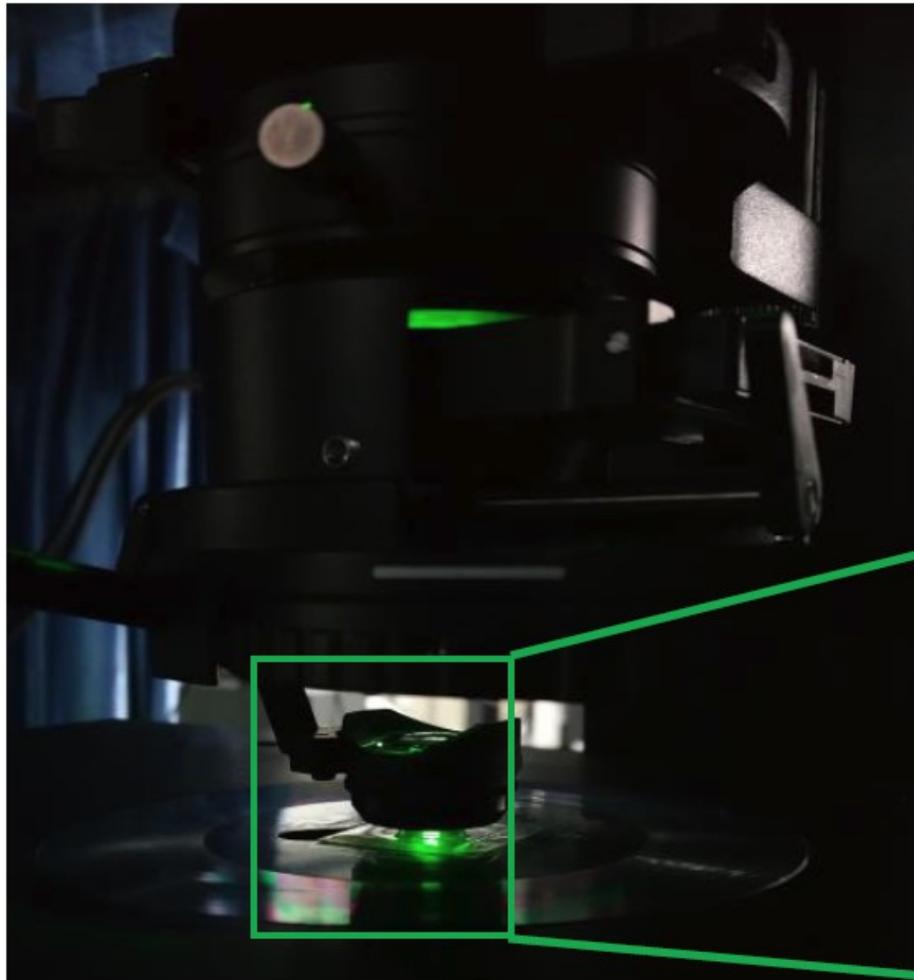
40. C. Zuo, J. Sun, J. Li, J. Zhang, A. Asundi, and Q. Chen, "High-resolution transport-of-intensity quantitative phase microscopy with annular illumination," *Sci. Rep.* **7**, 7654 (2017).



Annular-illumination TIE



Annular-illumination TIE

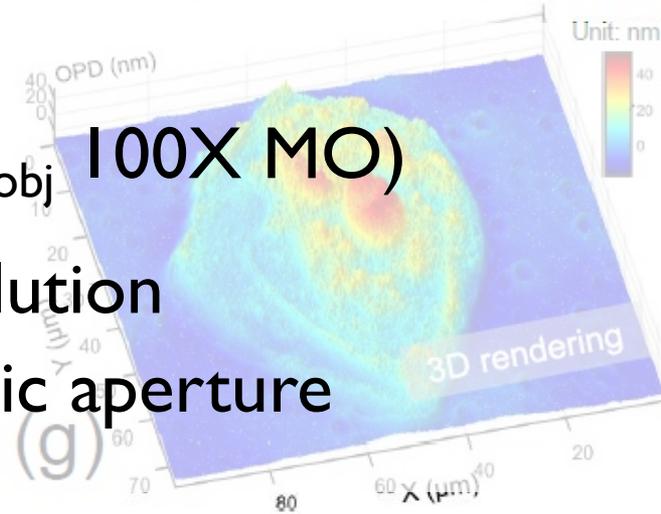
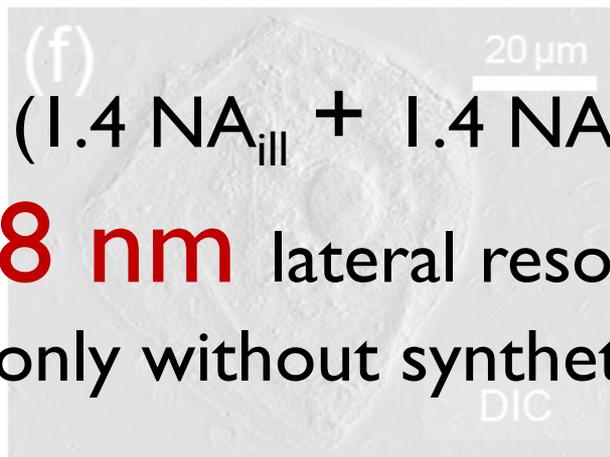
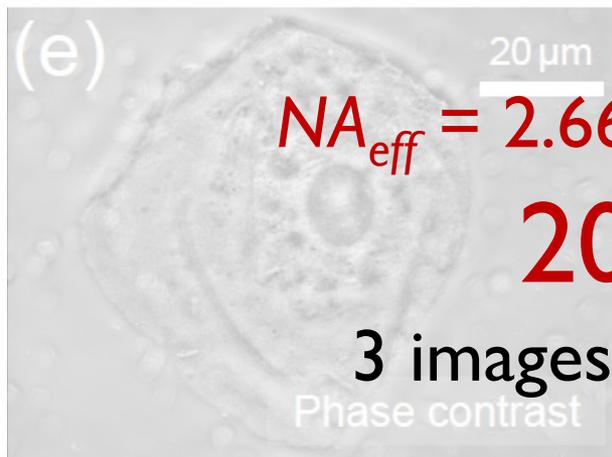
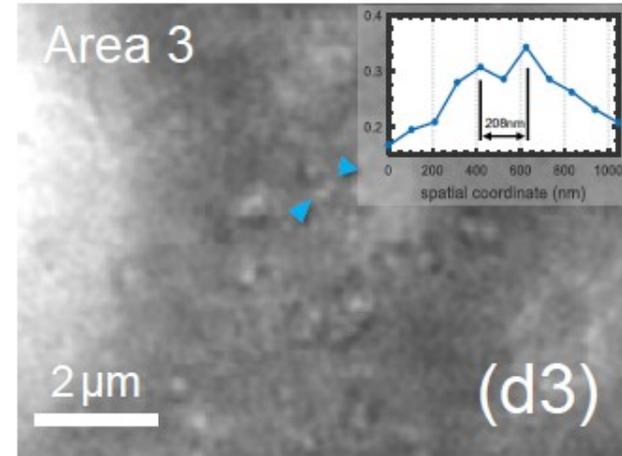
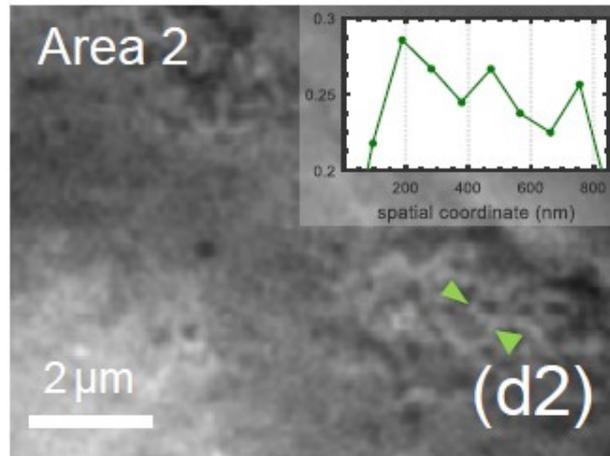
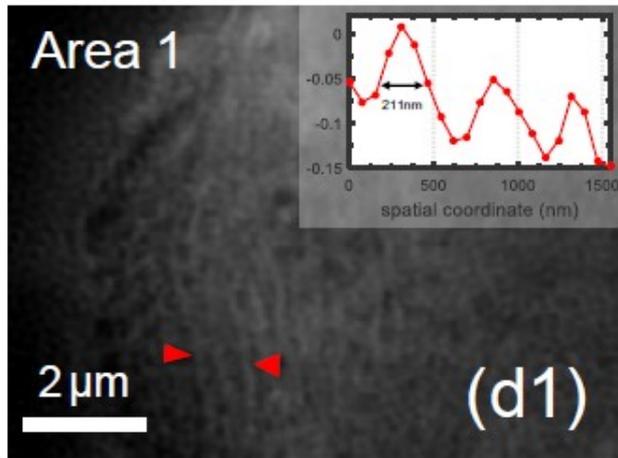


Experimental setup: $1.4 \text{ NA}_{\text{ill}} + 1.4 \text{ NA}_{\text{obj}}$ 100X MO

Annular-illumination TIE

rad
0.5

Area 2



$$NA_{eff} = 2.66 \quad (1.4 NA_{ill} + 1.4 NA_{obj} \text{ 100X MO})$$

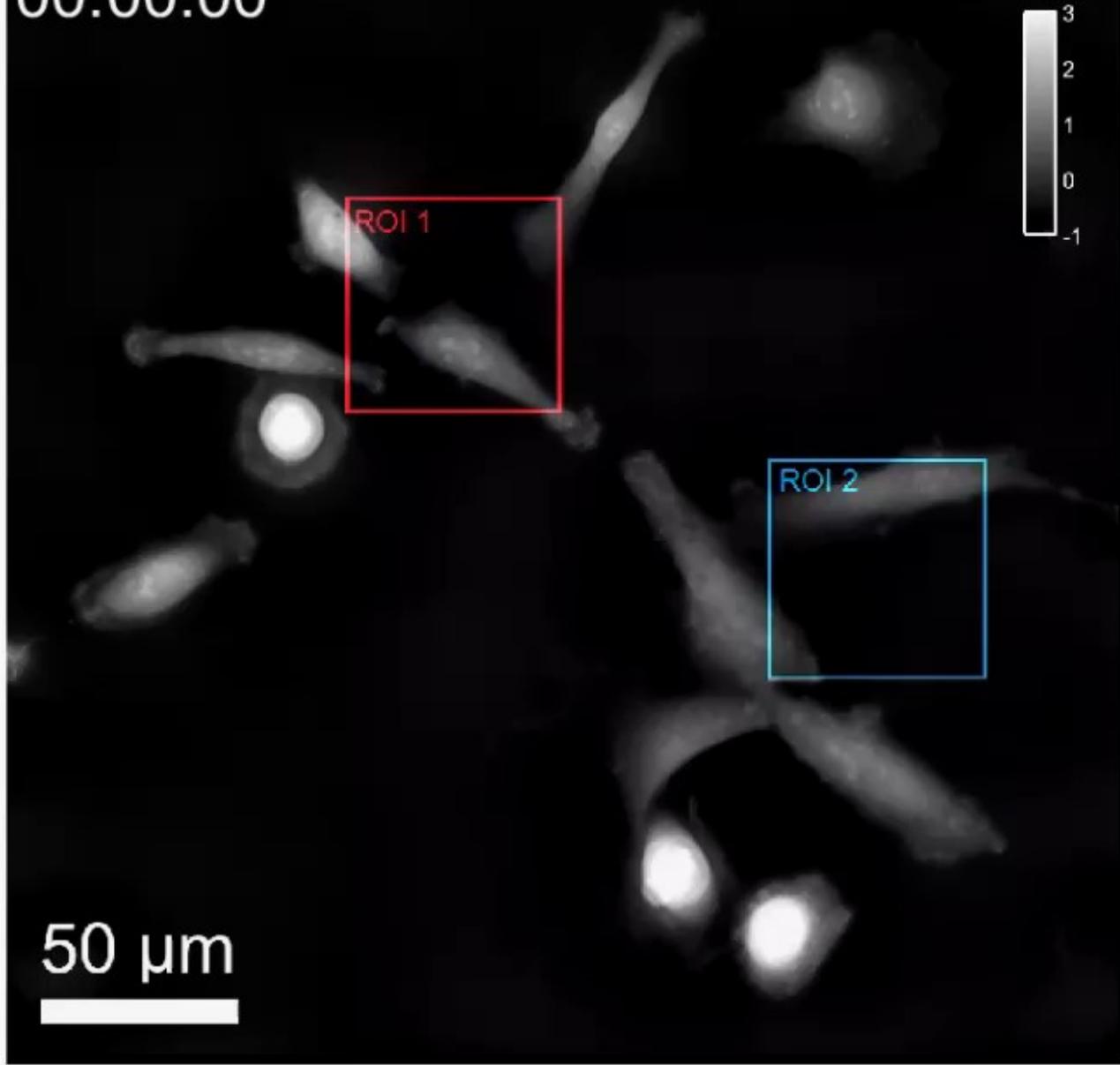
208 nm lateral resolution

3 images only without synthetic aperture

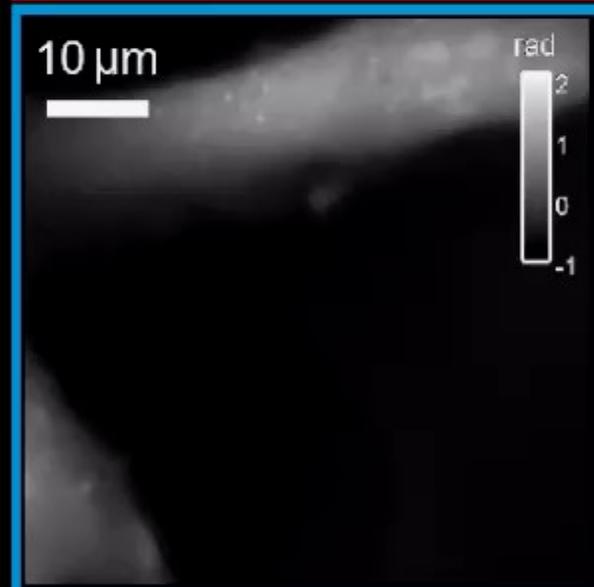
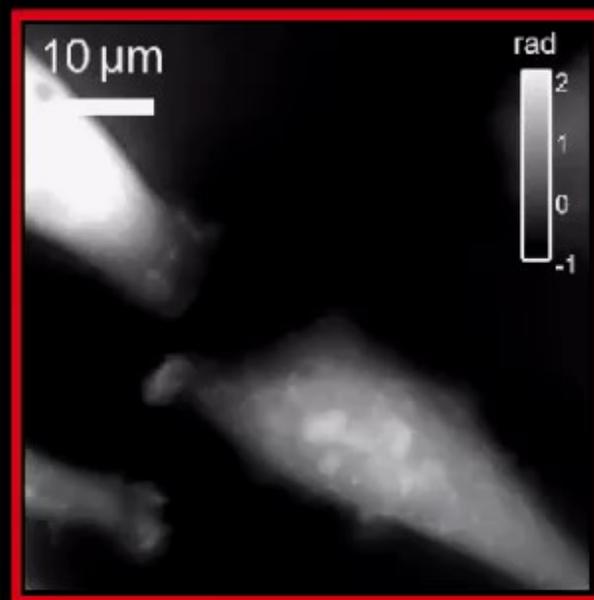
20 μm

Long-term time-lapse imaging of HeLa cell dividing in culture (60 h)

00:00:00



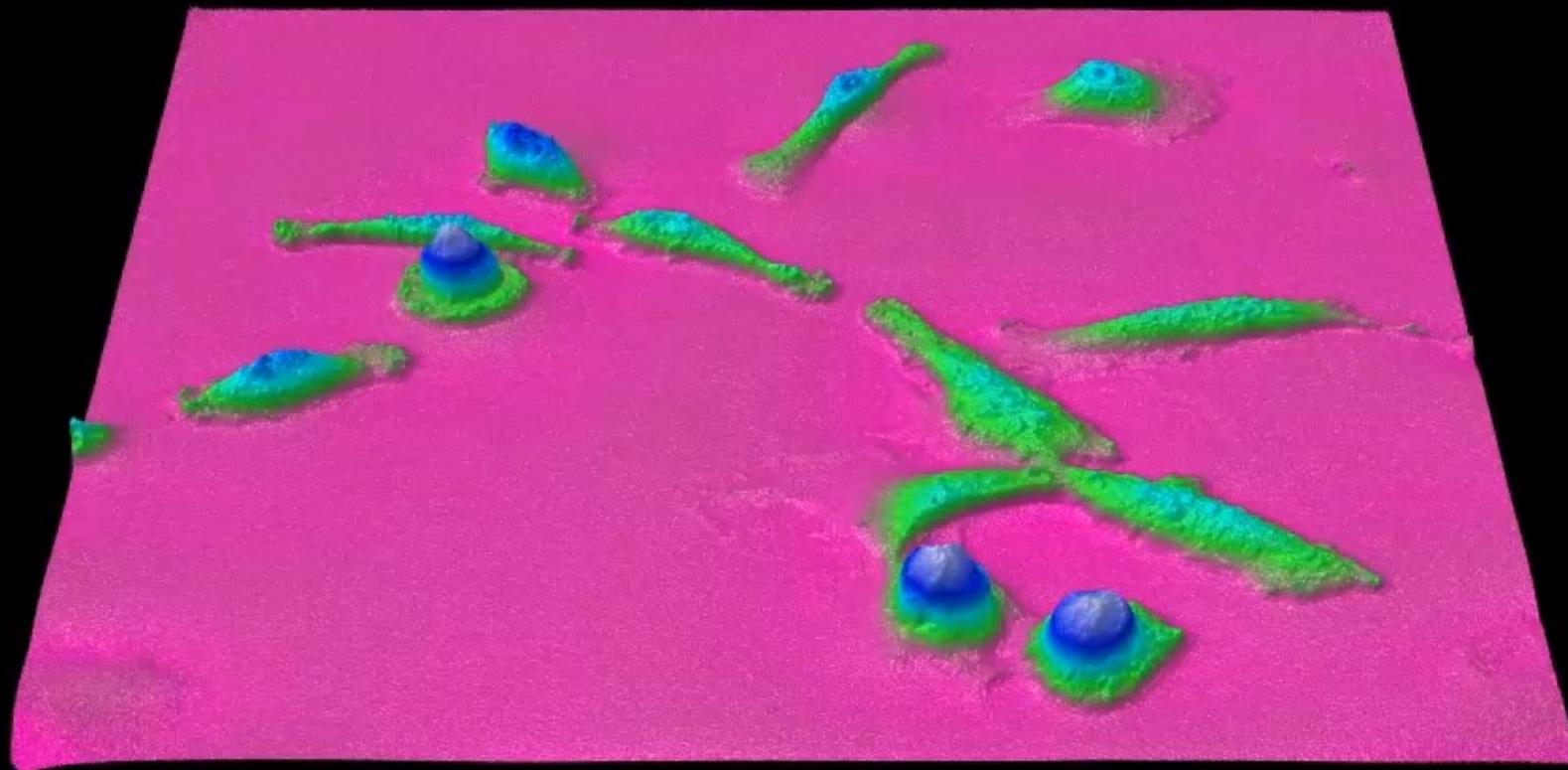
Cell No.:13 Confluence:13.6%



Long-term time-lapse imaging of HeLa cell dividing in culture (60 h)

Time: 00:00:00

Phase -1 0 1 2 3 4 5 (rad)
OPD -87.6 87.6 263.7 437.9(nm)

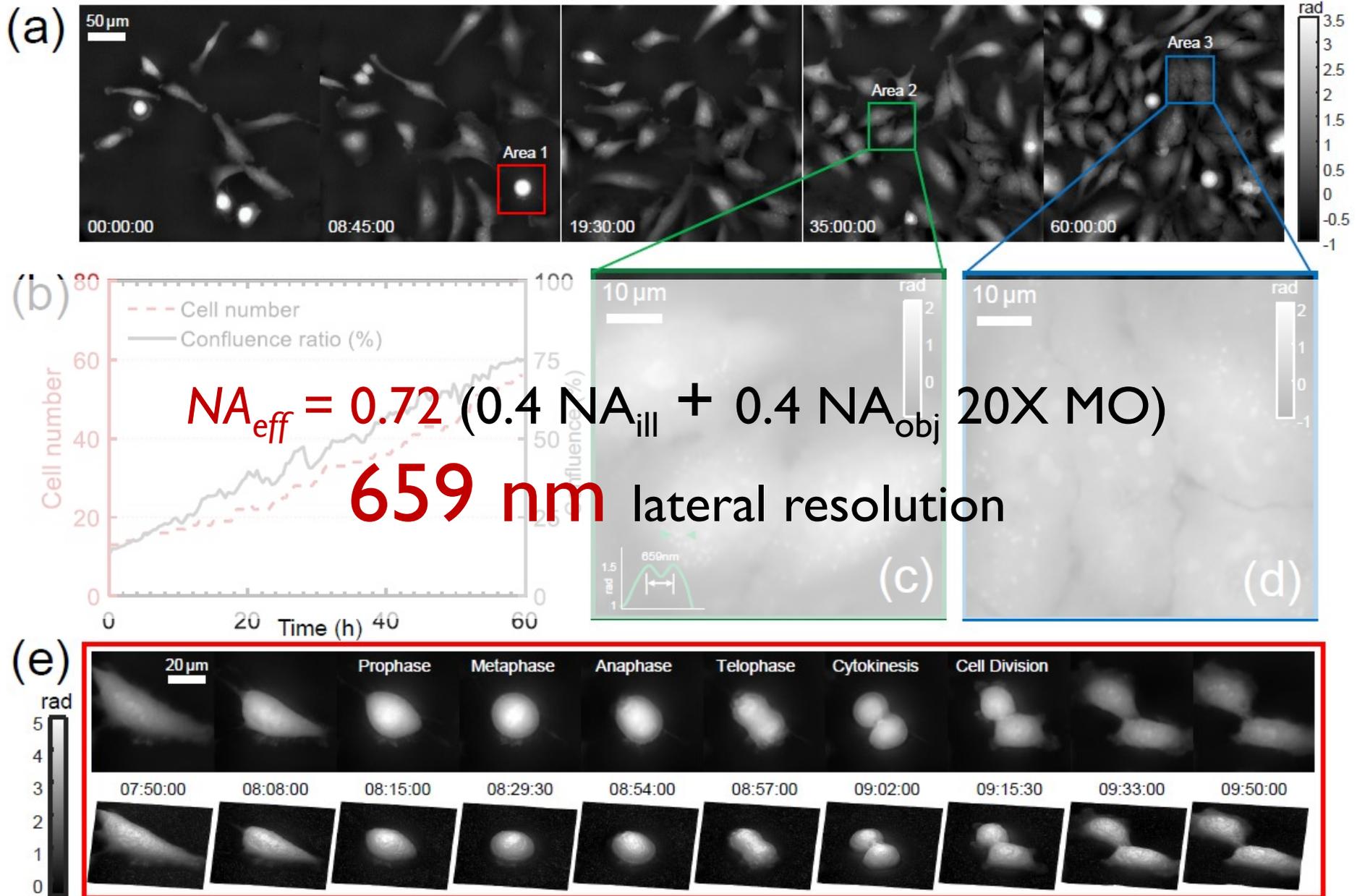


50 μm

Cell No.:13

Confluence:13.8%

Annular-illumination TIE



Multi-modal computational imaging of HeLa cell apoptosis

00:00:00

ROI 1

ROI 2

50 μm

rad

4
2
0



Fast Motion Factor: 150X

10 μm

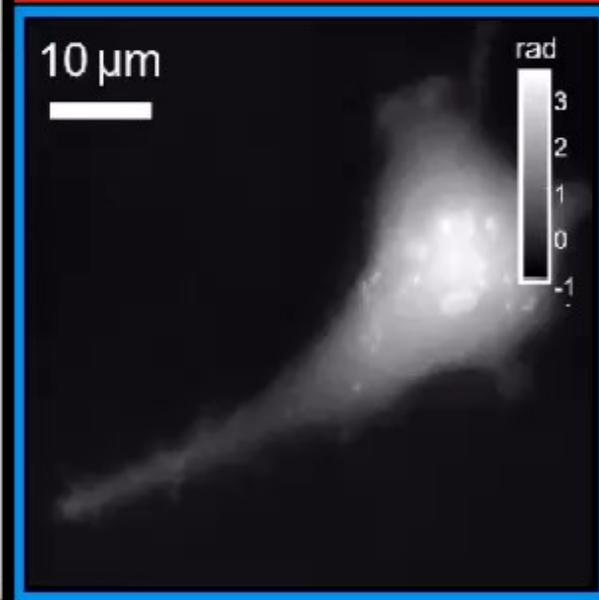
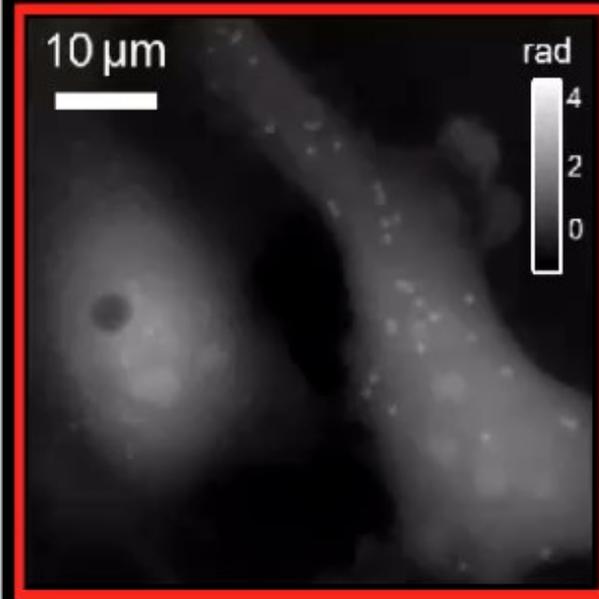
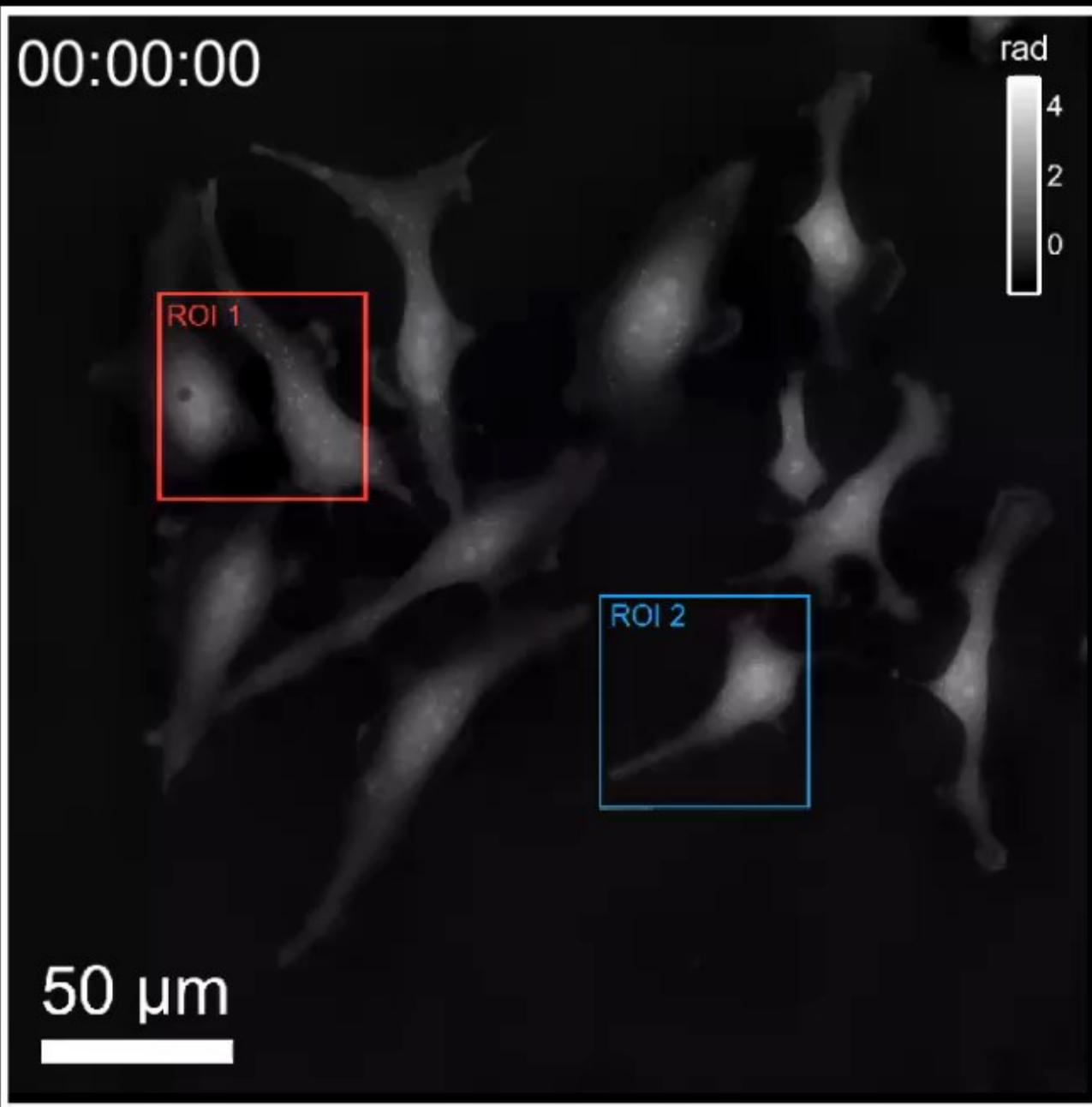
rad

4
2
0

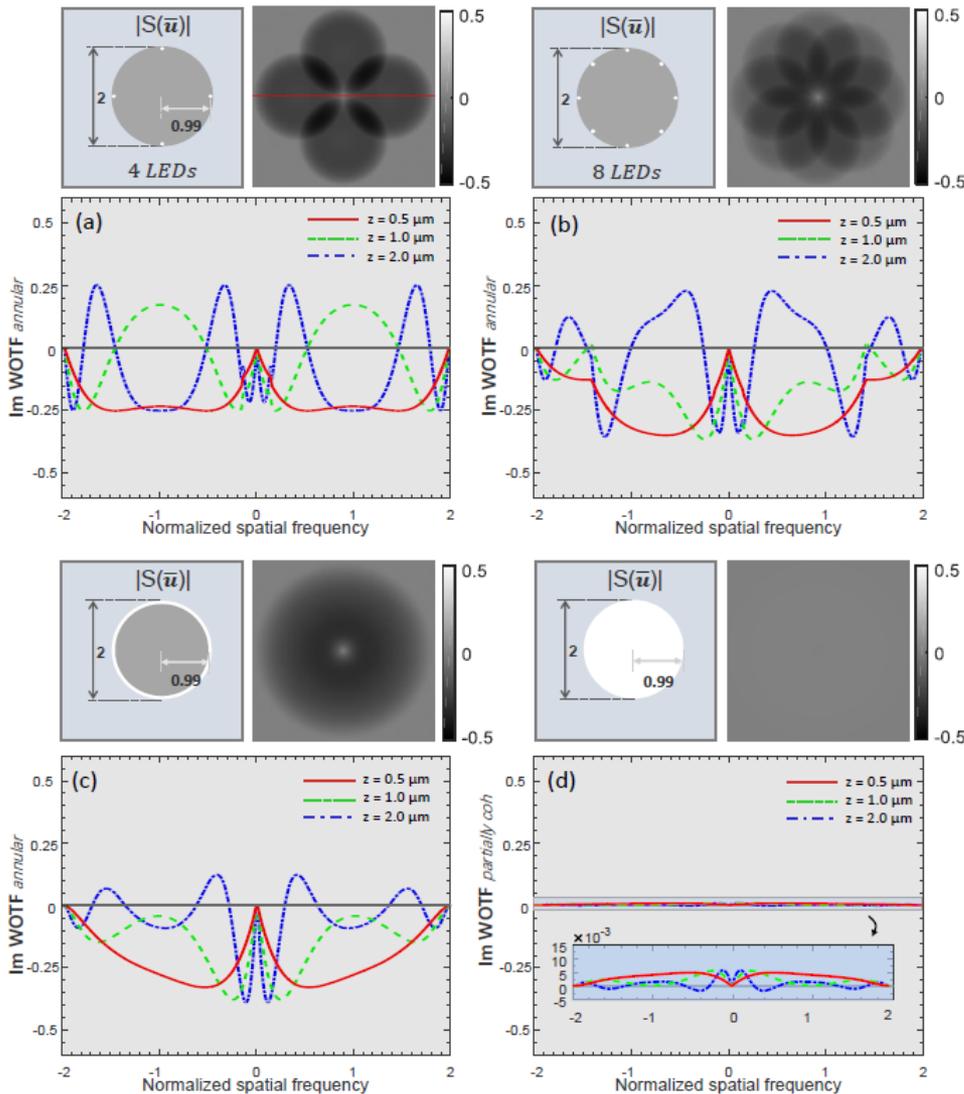
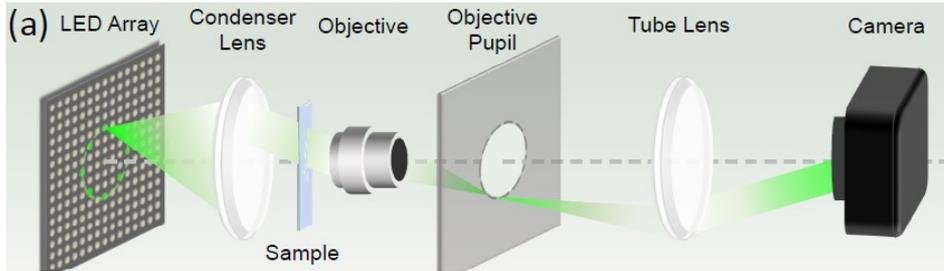
10 μm

rad

3
2
1
0
-1



Multi-modal Imaging



Efficient quantitative phase microscopy using programmable annular LED illumination

JIAJI LI,^{1,2,3,4} QIAN CHEN,^{1,2} JIALIN ZHANG,^{1,2,3} YAN ZHANG,^{1,2,3} LINPENG LU,^{1,2,3} AND CHAO ZUO^{1,2,3,*}

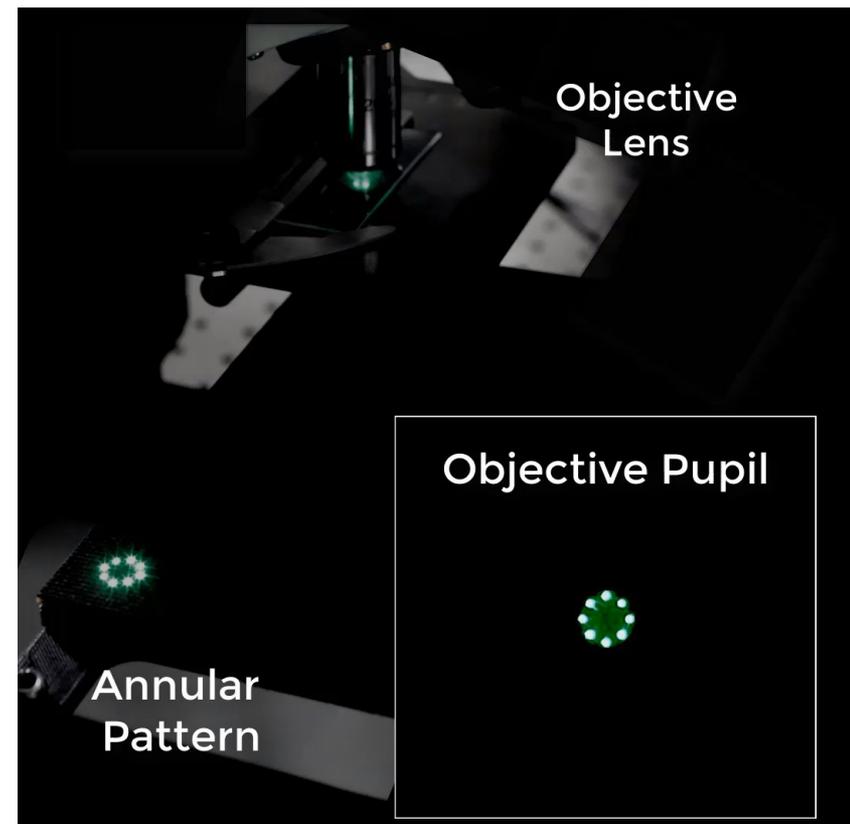
¹School of Electronic and Optical Engineering, Nanjing University of Science and Technology, No. 200 Xiaolingwei Street, Nanjing, Jiangsu Province 210094, China

²Jiangsu Key Laboratory of Spectral Imaging & Intelligent Sense, Nanjing University of Science and Technology, Nanjing, Jiangsu Province 210094, China

³Smart Computational Imaging (SCI) Laboratory, Nanjing University of Science and Technology, Nanjing, Jiangsu Province 210094, China

⁴jjajili@njust.edu.cn

*zuocho@njust.edu.cn



Best?



Yes!

Optimal illumination pattern for transport-of-intensity quantitative phase microscopy

JIAJI LI,^{1,2,3} QIAN CHEN,^{1,2,4} JIASONG SUN,^{1,2,3} JIALIN ZHANG,^{1,2,3} XIANGPENG PAN,^{1,2,3} AND CHAO ZUO^{1,2,3,*}

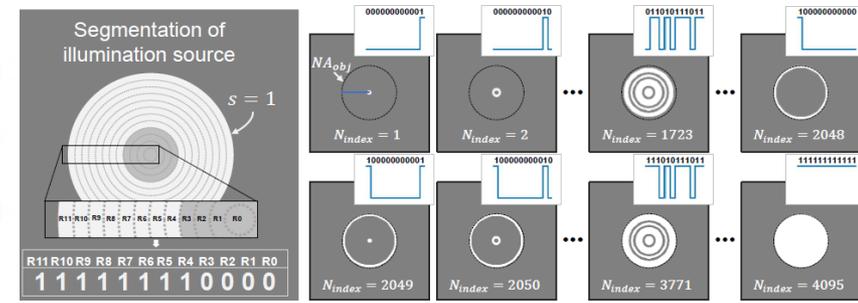
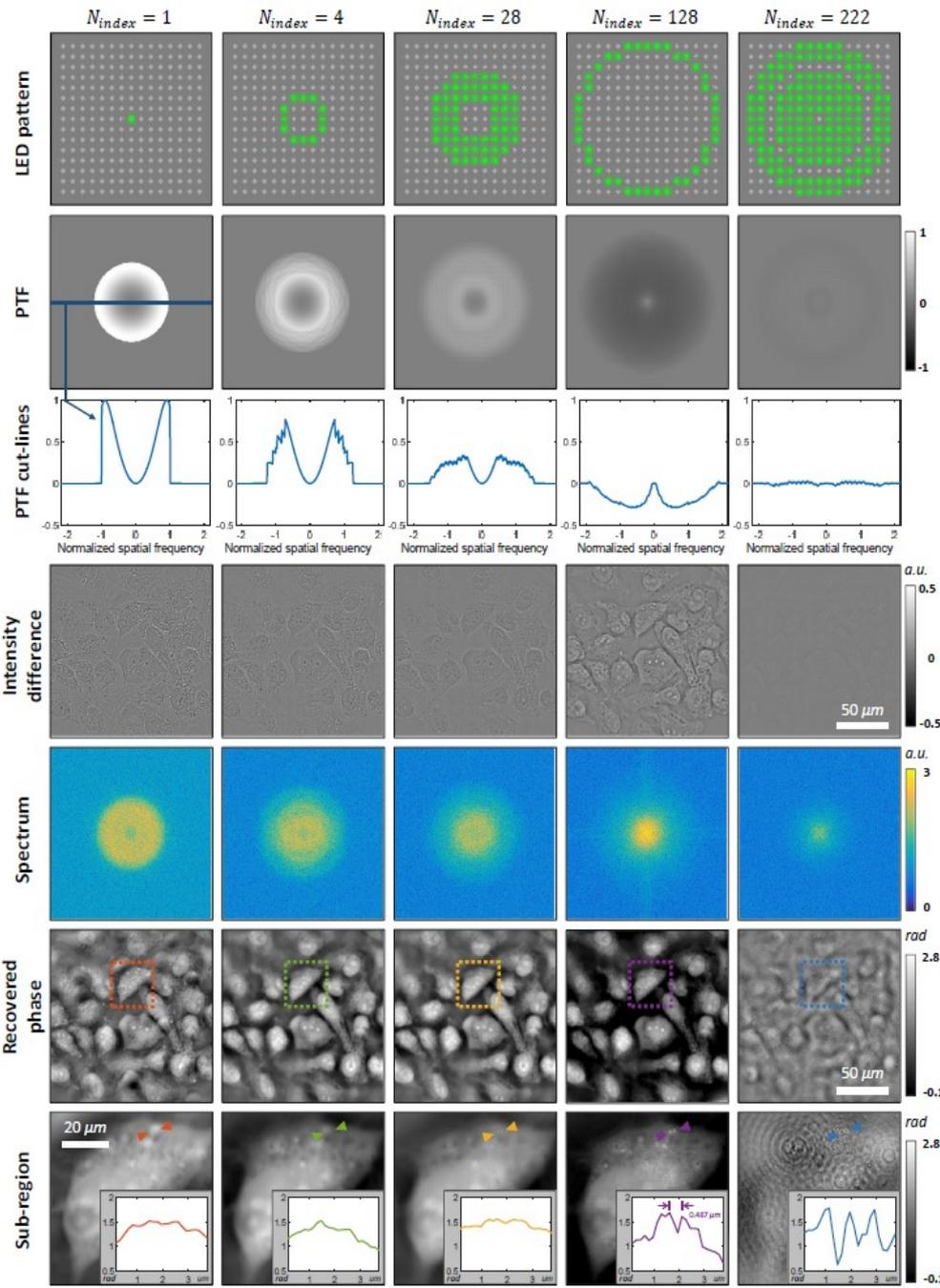
¹School of Electronic and Optical Engineering, Nanjing University of Science and Technology, No. 200 Xiaolingwei Street, Nanjing, Jiangsu Province 210094, China

²Jiangsu Key Laboratory of Spectral Imaging & Intelligent Sense, Nanjing University of Science and Technology, Nanjing, Jiangsu Province 210094, China

³Smart Computational Imaging Laboratory (SCILab), Nanjing University of Science and Technology, Nanjing, Jiangsu Province 210094, China

⁴chenqian@njust.edu.cn

*zuo@njust.edu.cn



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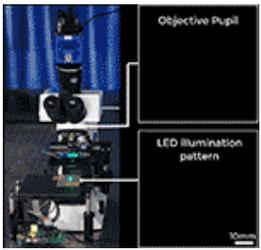


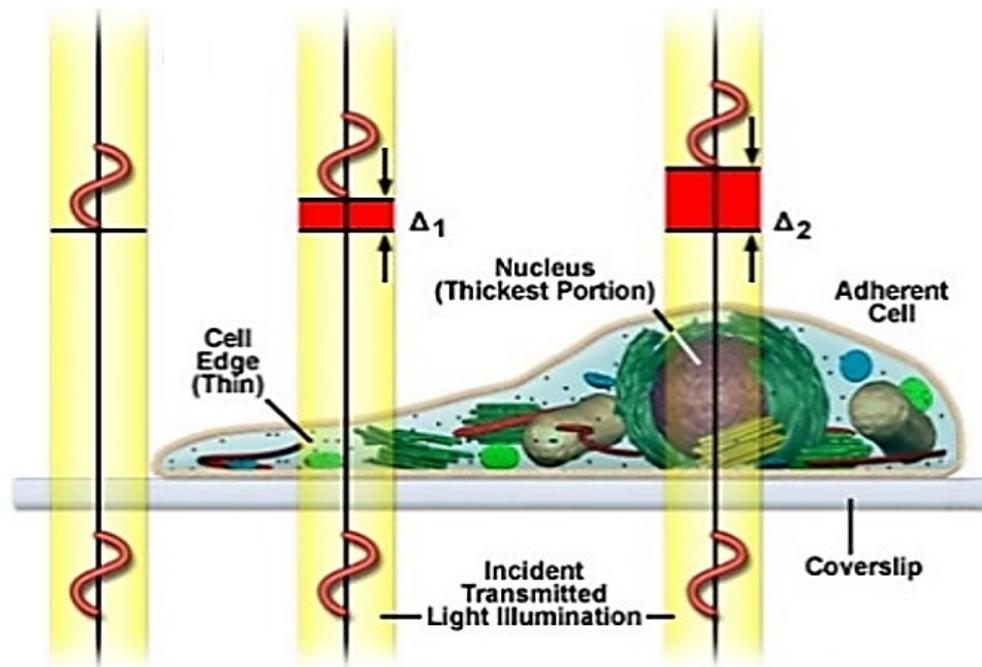
Image of the Week - 12 November 2018

Optimal illumination pattern for transport-of-intensity quantitative phase microscopy

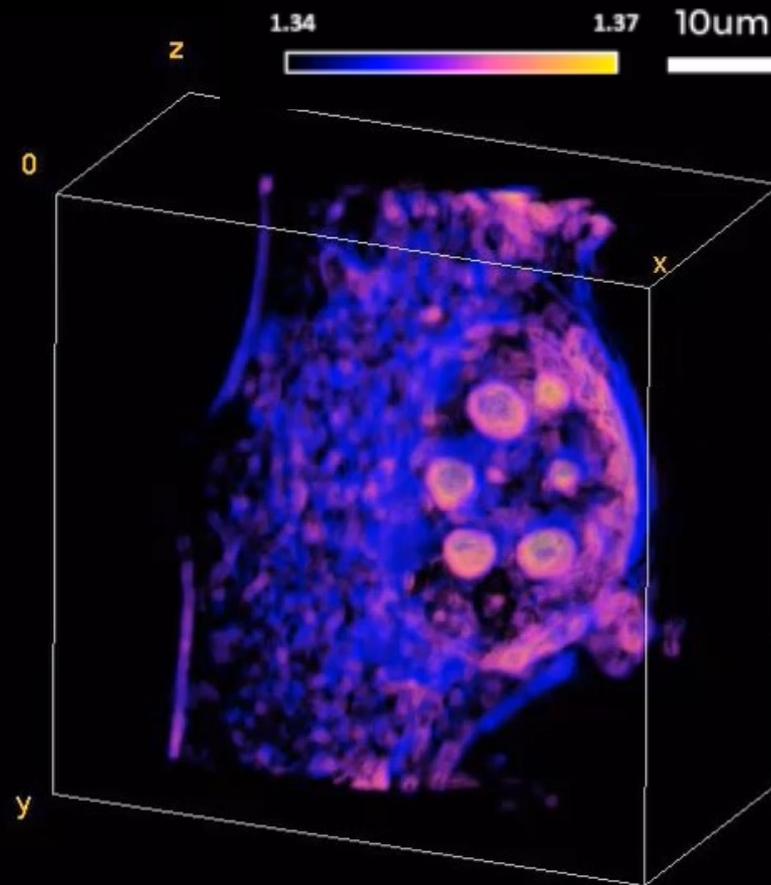
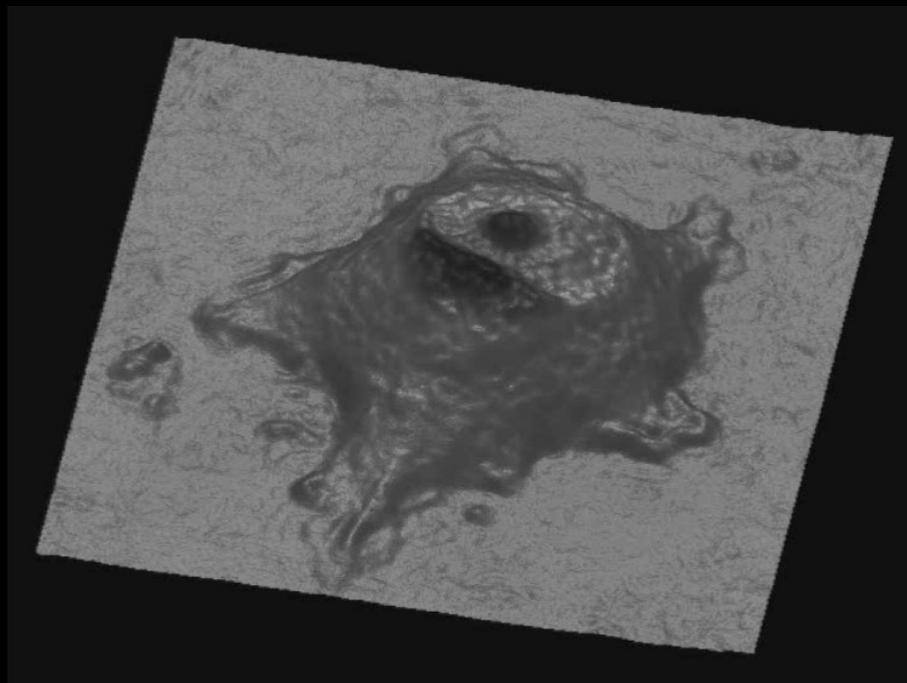
See Visualization 1 in Opt. Express 26(21), 27599-27614 (2018).

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3D phase imaging ?



QPI vs ODT (optical diffraction tomography)

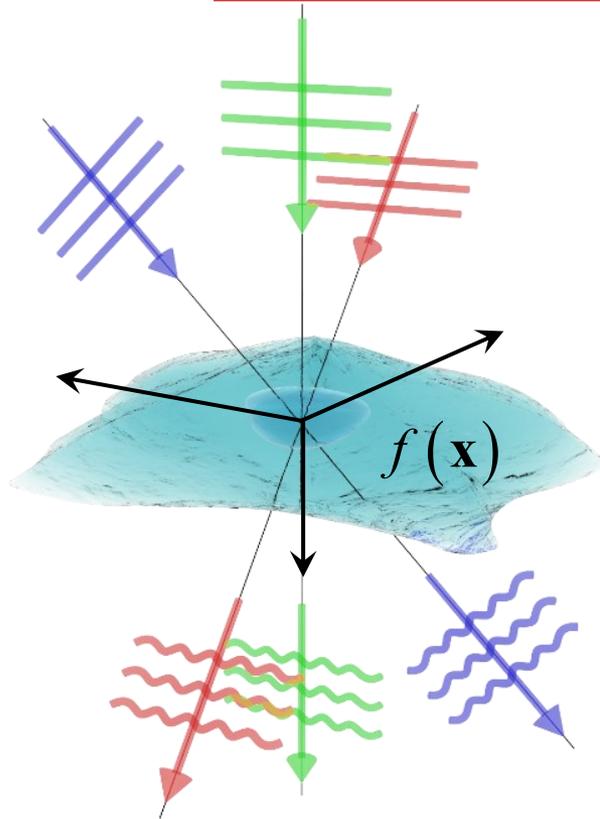


QPI: **2.5D** optical path length
Profile

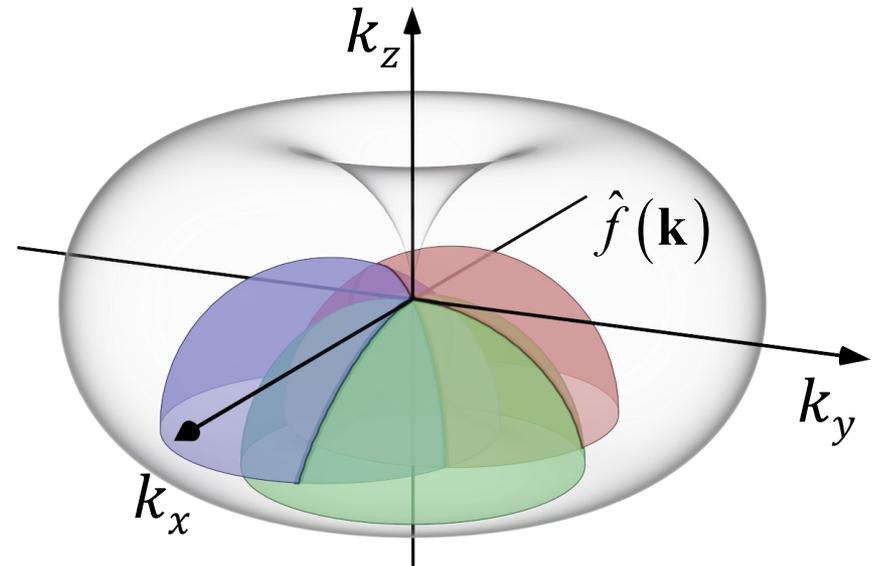
ODT: true **3D** refractive index
Volume

Transport-of-intensity diffraction tomography (TIDT)

Fourier diffraction theorem



3D real space

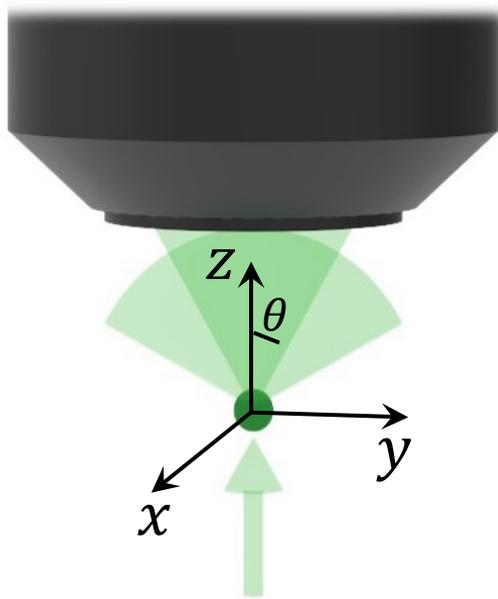


3D Fourier space

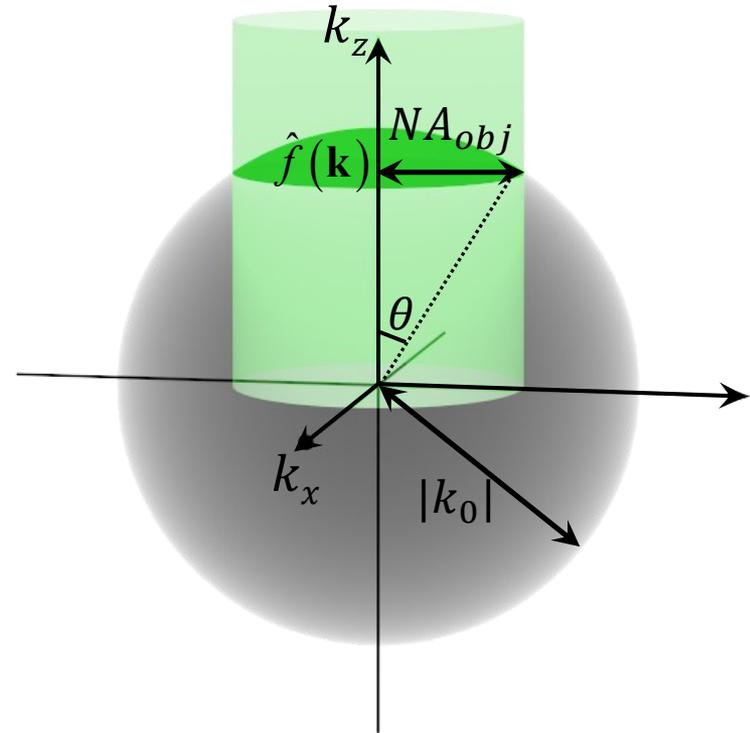
Free-space: **semi-sphere** in 3D Fourier space

Transport-of-intensity diffraction tomography (TIDT)

Fourier diffraction theorem for a limit-aperture system



3D real space



3D Fourier space

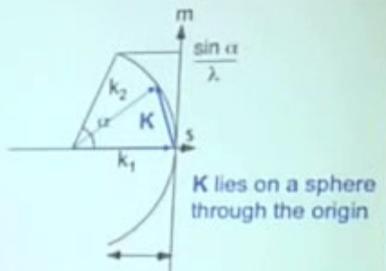
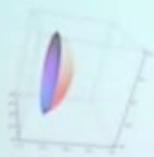
Microscopic imaging: **partial spherical cap** bounded by the lens aperture

3D phase imaging ?

Coherent imaging (including holography)

transmission $k = 2\pi / \lambda$
 $|k_1| = |k_2|$

Coherent transfer function (CTF)



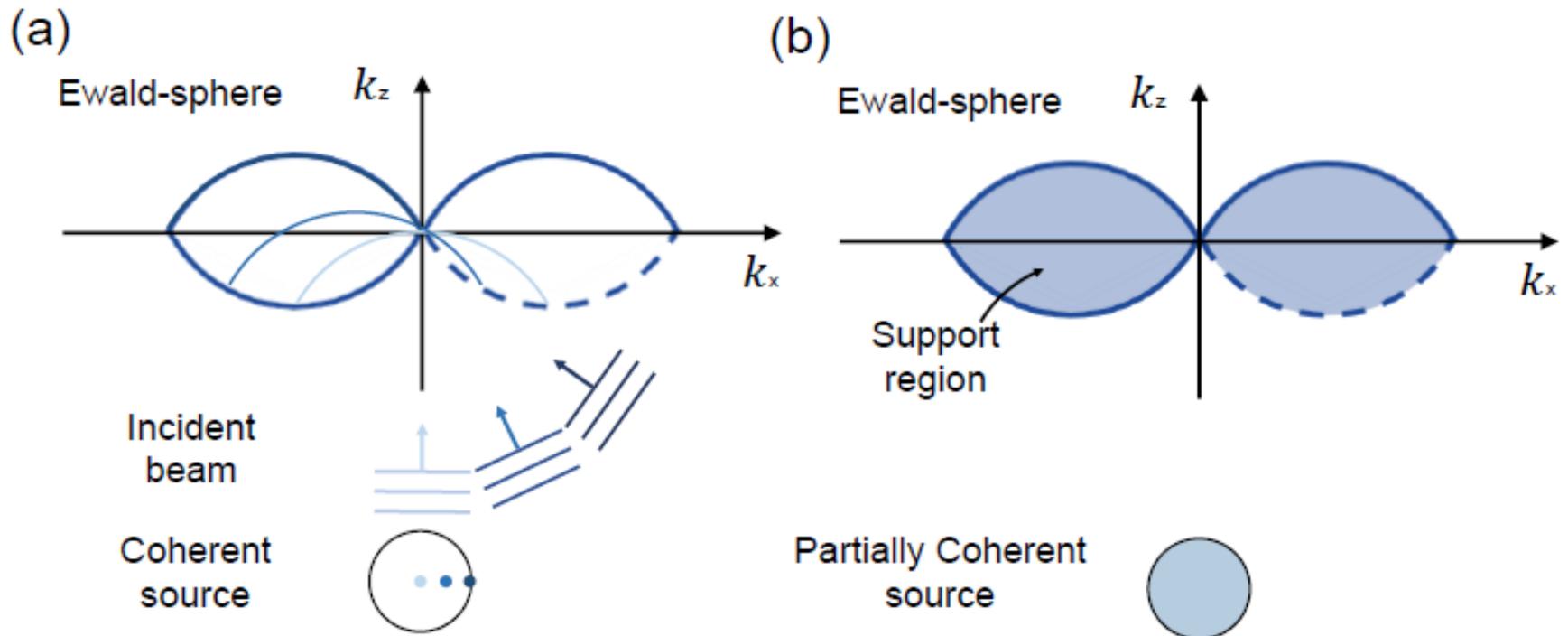
$\frac{1 - \cos \alpha}{\lambda} = \frac{2}{\lambda} \sin^2 \frac{\alpha}{2}$

Wolf, *Opt. Commun.* **1**, 153-156 (1969)
only image frequencies on cap of sphere

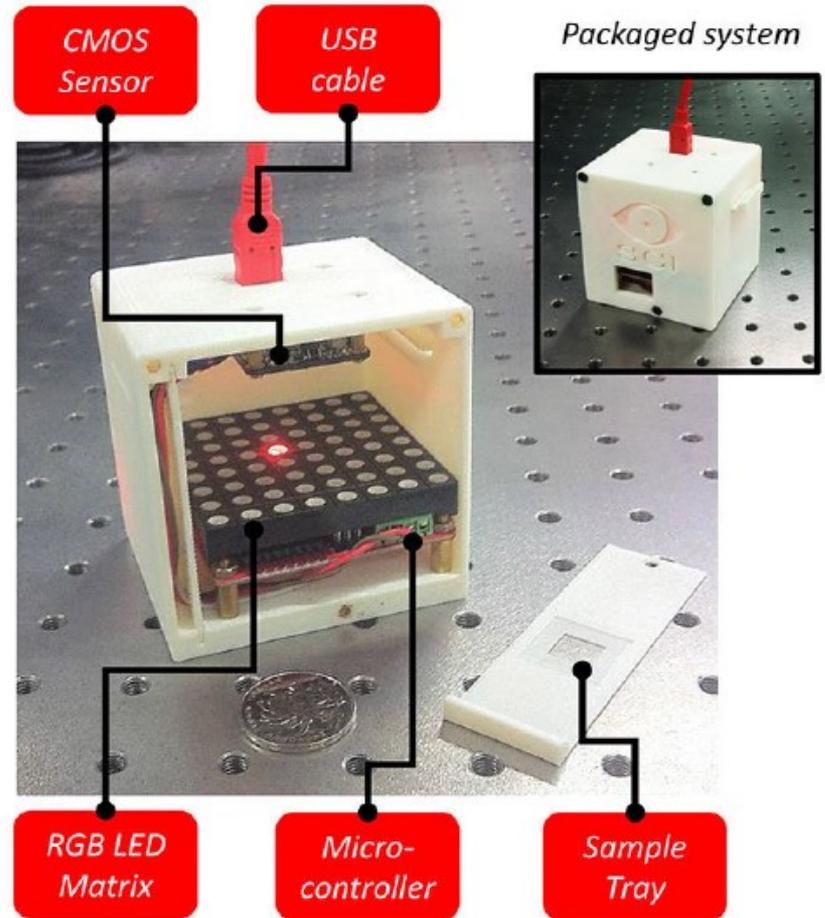
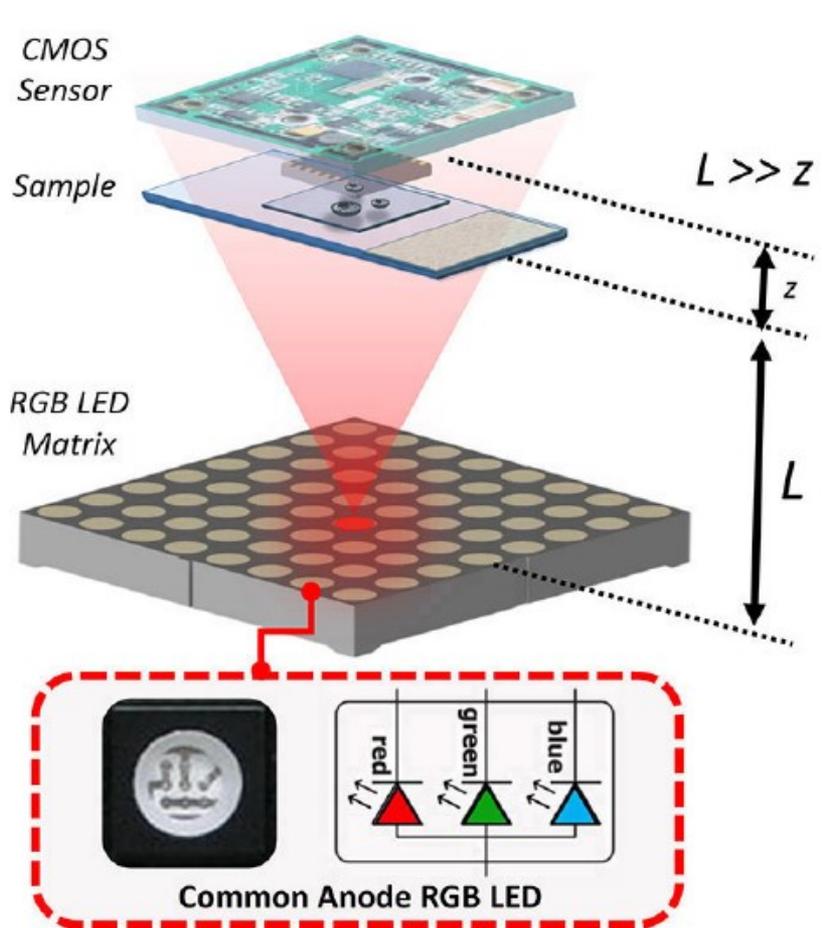
S. S. Kou and C. J. R. Sheppard, "Image formation in holographic tomography,"
Opt. Lett. **33**, 2362-2364 (2008).

S. S. Kou and C. J. R. Sheppard, "Image formation in transmission holographic
tomography: High aperture imaging conditions," *Appl. Opt.* **34**, H168-H175 (2009)

Coherent / partially coherent ODT

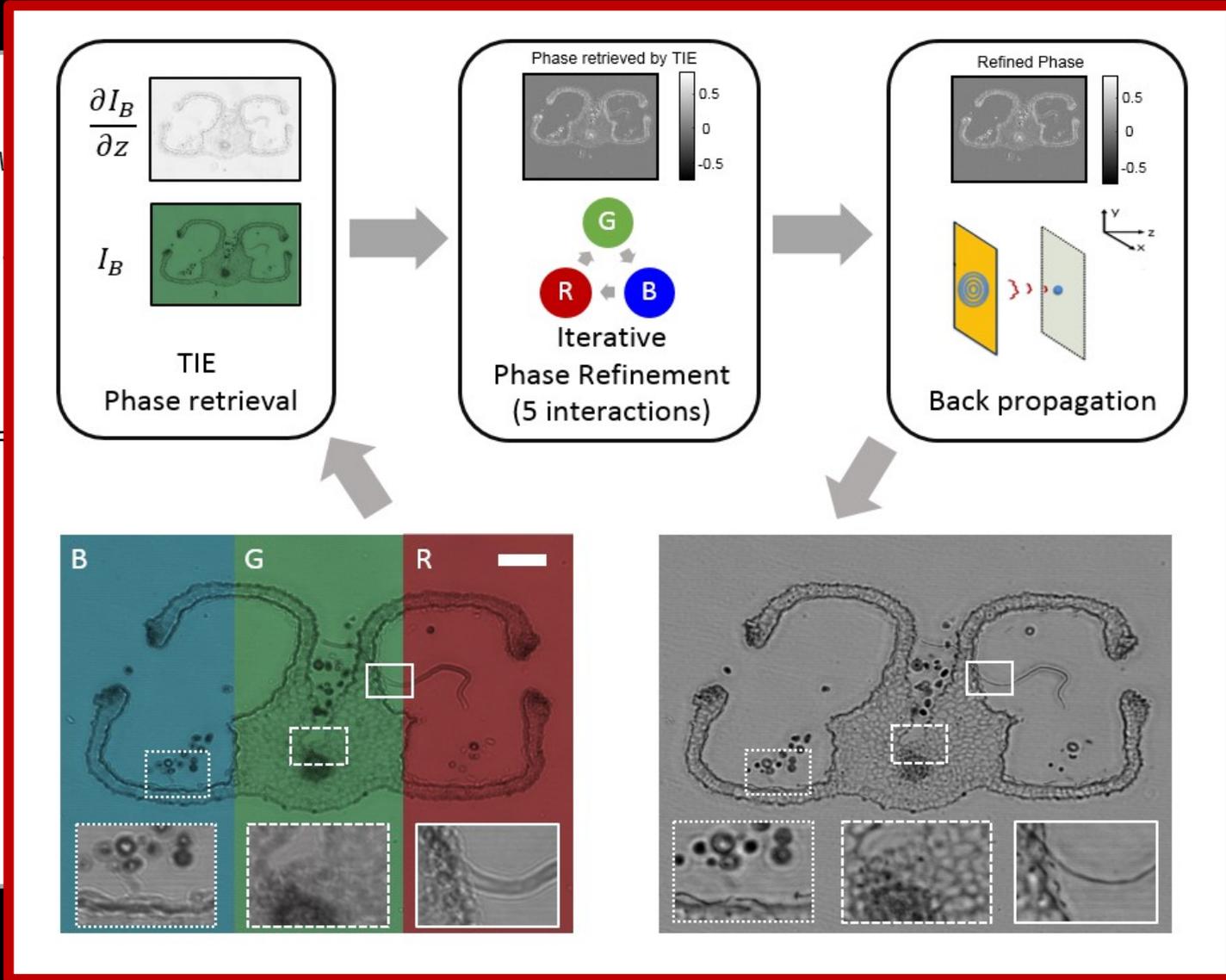


Lensless TIE microscopy

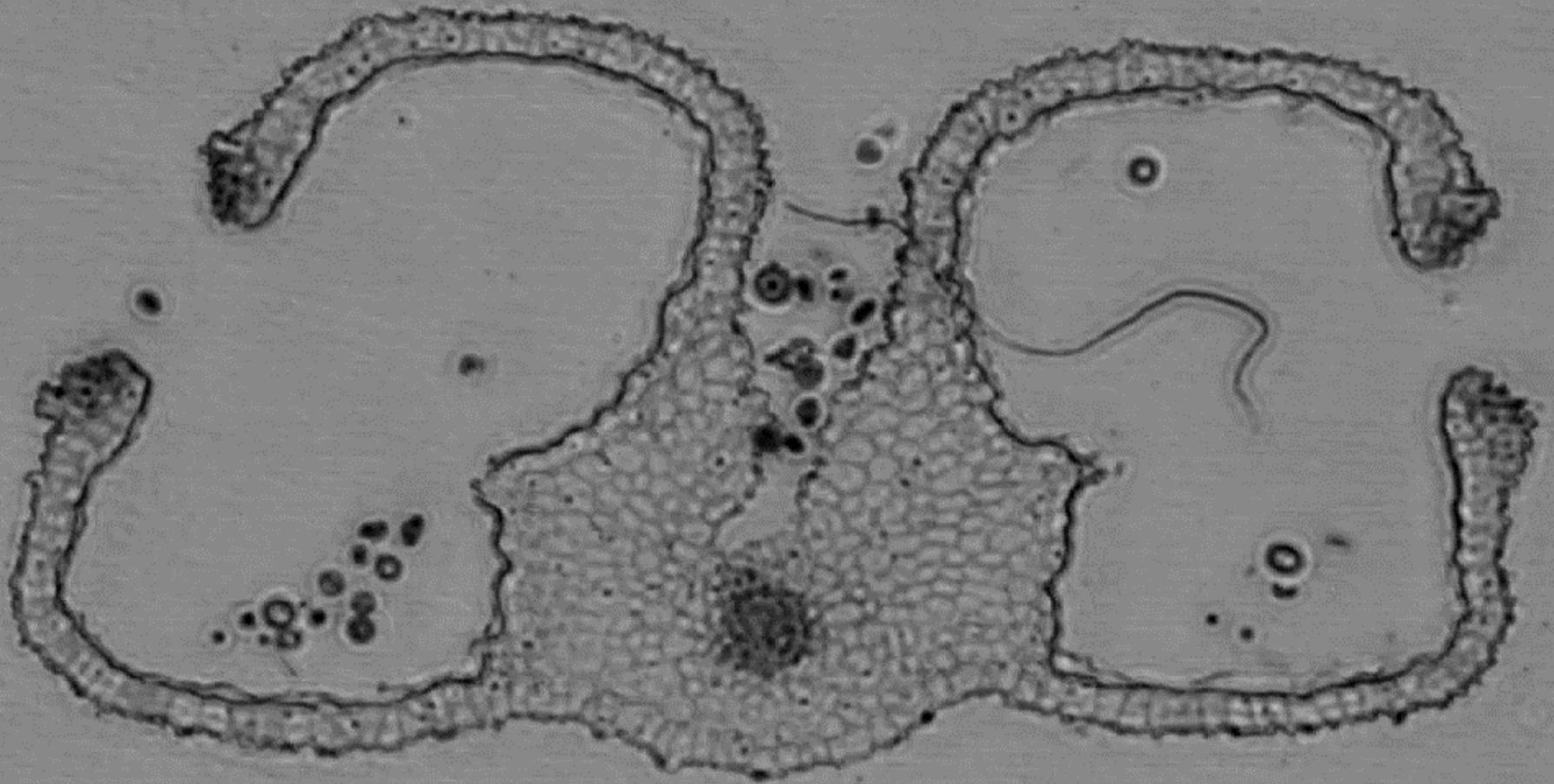


Lensless TIE microscope

Lensless TIE microscopy

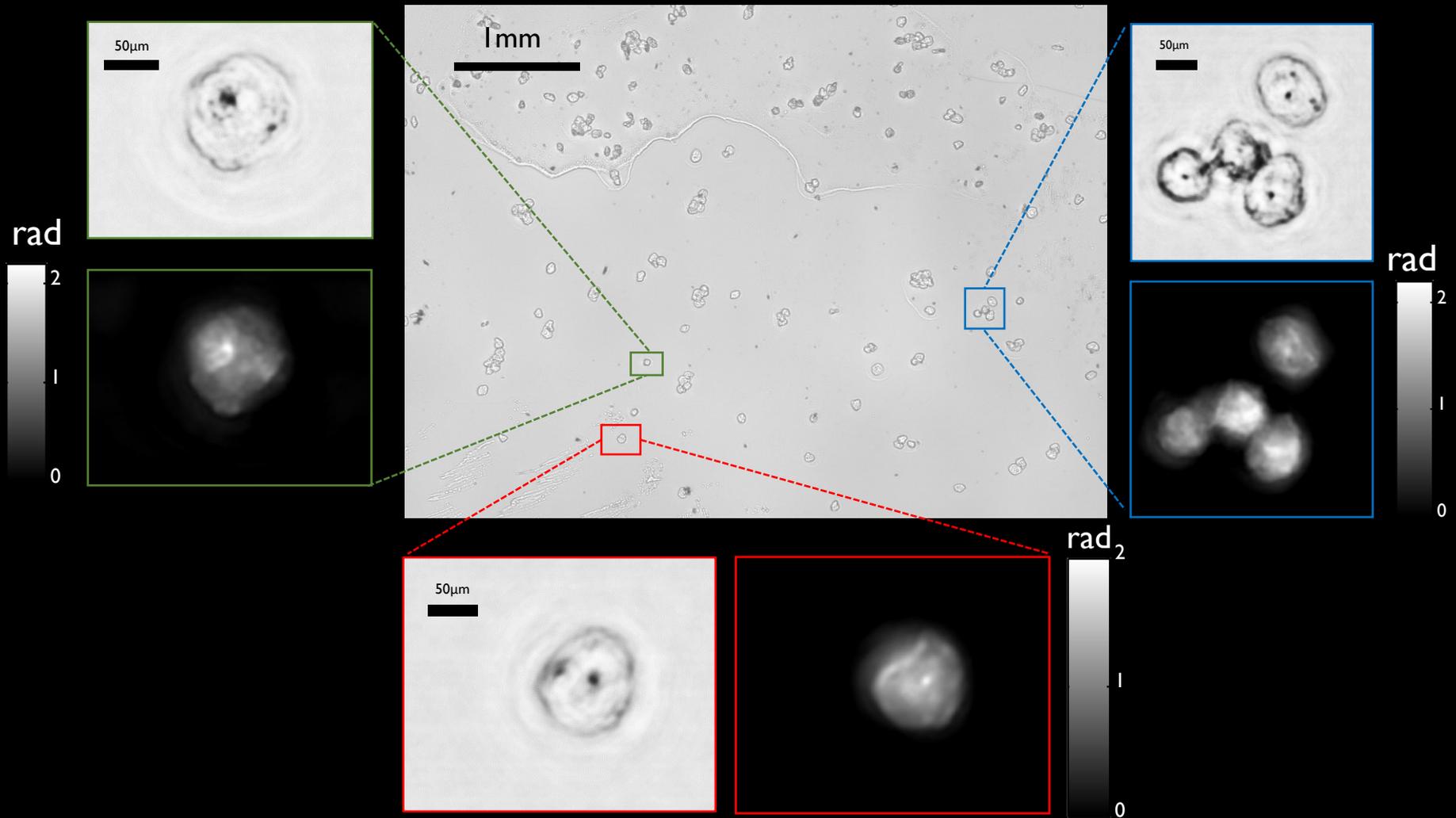


Lensless TIE microscopy



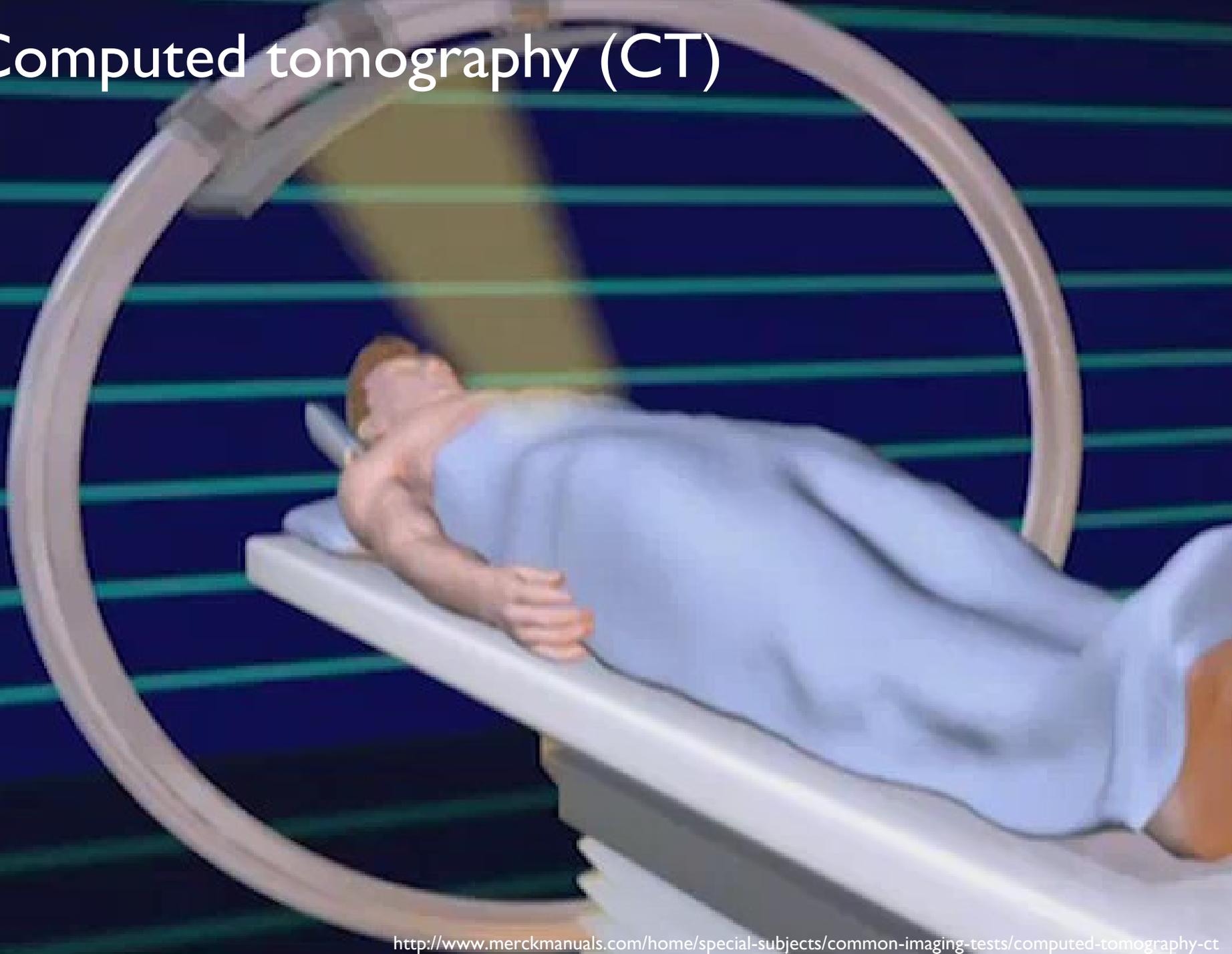
Digital refocusing

Lensless TIE microscopy

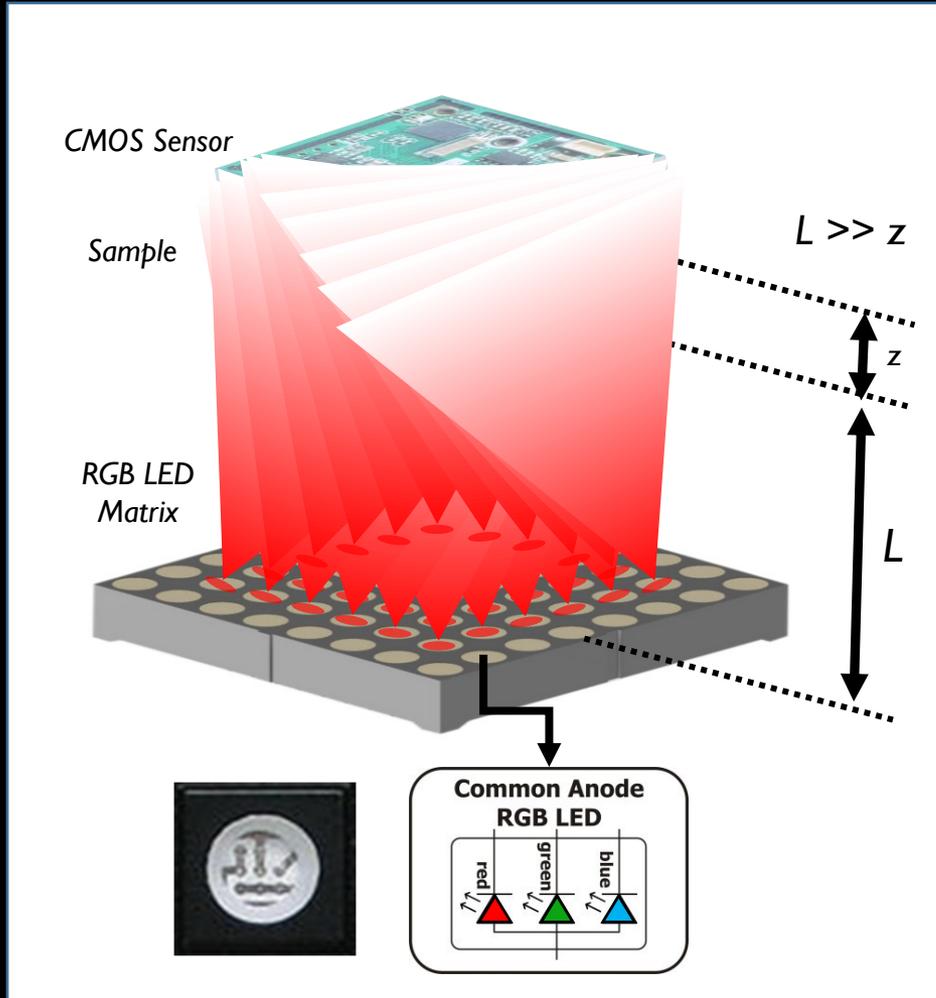


Quantitative phase of cheek cells (entire FOV 24mm²)

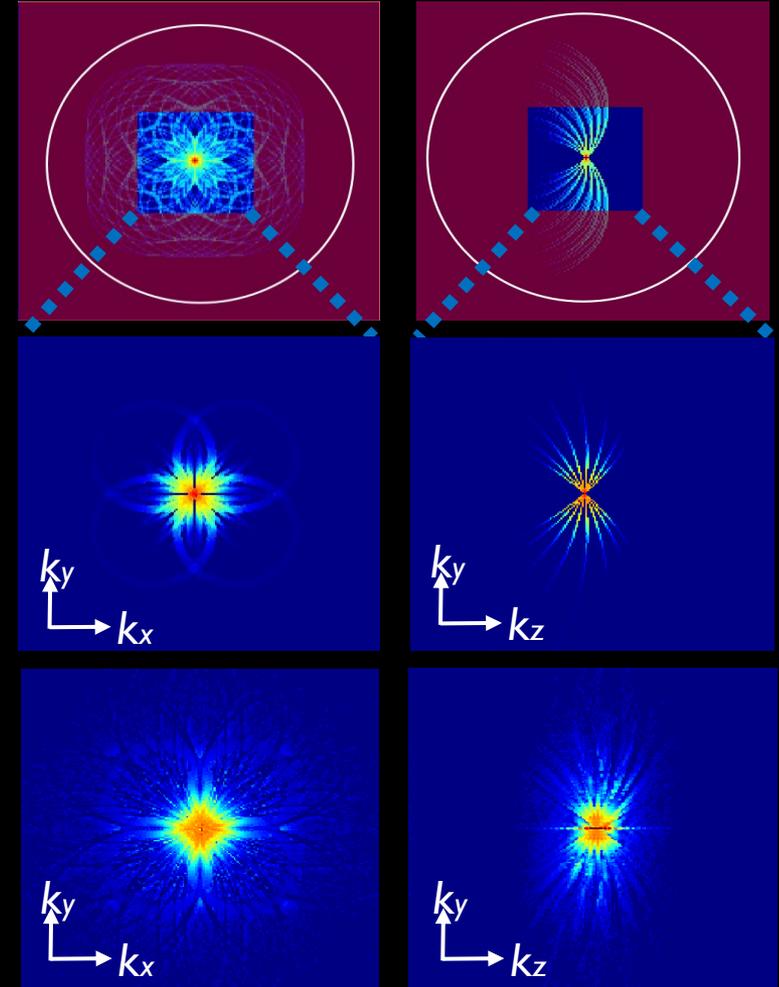
Computed tomography (CT)



Lensless TIE tomography



Change Illumination angle ($\approx \pm 45^\circ$)

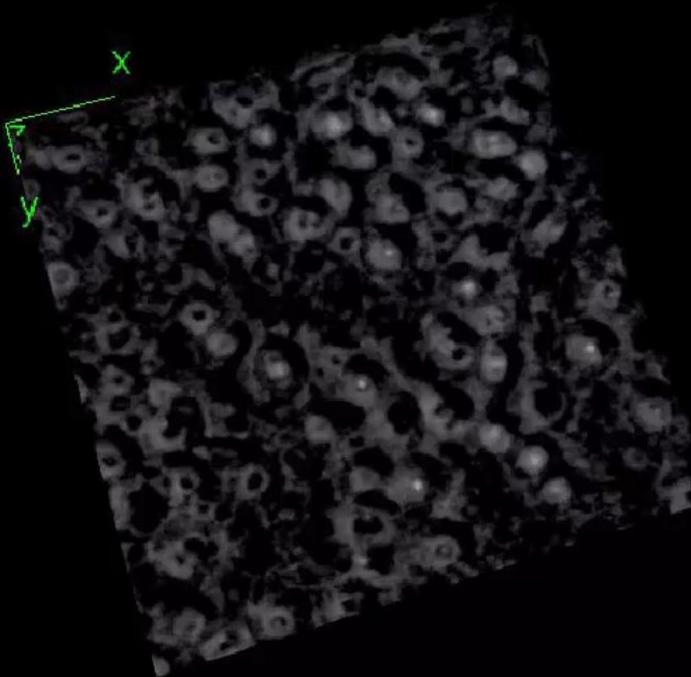


Fill the 3D Fourier Space of the object

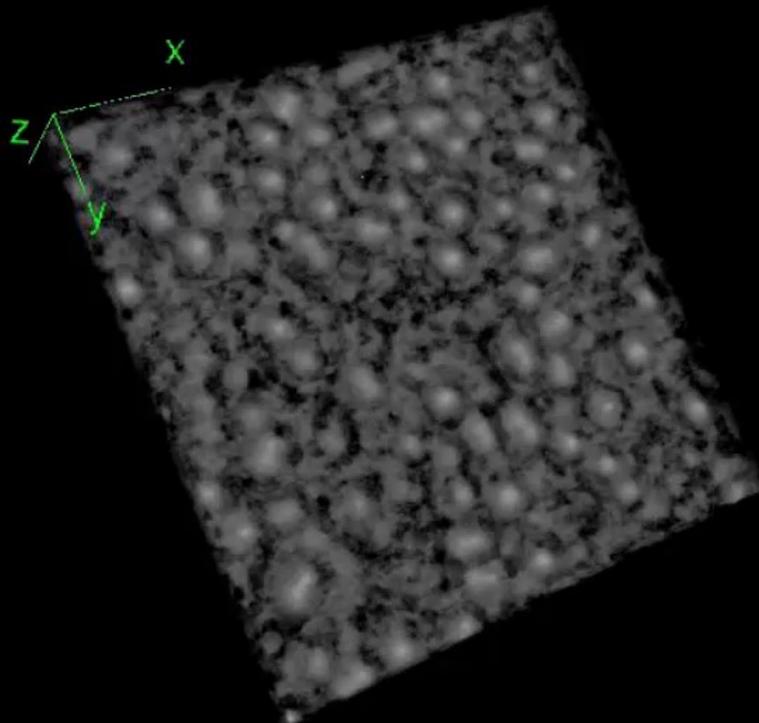
Lensless TIE tomography

The uterus of *Parascaris equorum*

Phase tomography



Absorption tomography



OSA Publishing

Cover feature of Optics Express

OSA Image of the Week

The screenshot shows the journal's homepage with a featured article on the cover and a section for the 'Image of the Week'. The featured article is titled 'Coherence and Statistical Optics' and includes a small thumbnail image of a textured surface, similar to the tomography images shown above. The 'Image of the Week' section also features a small thumbnail image of a textured surface.

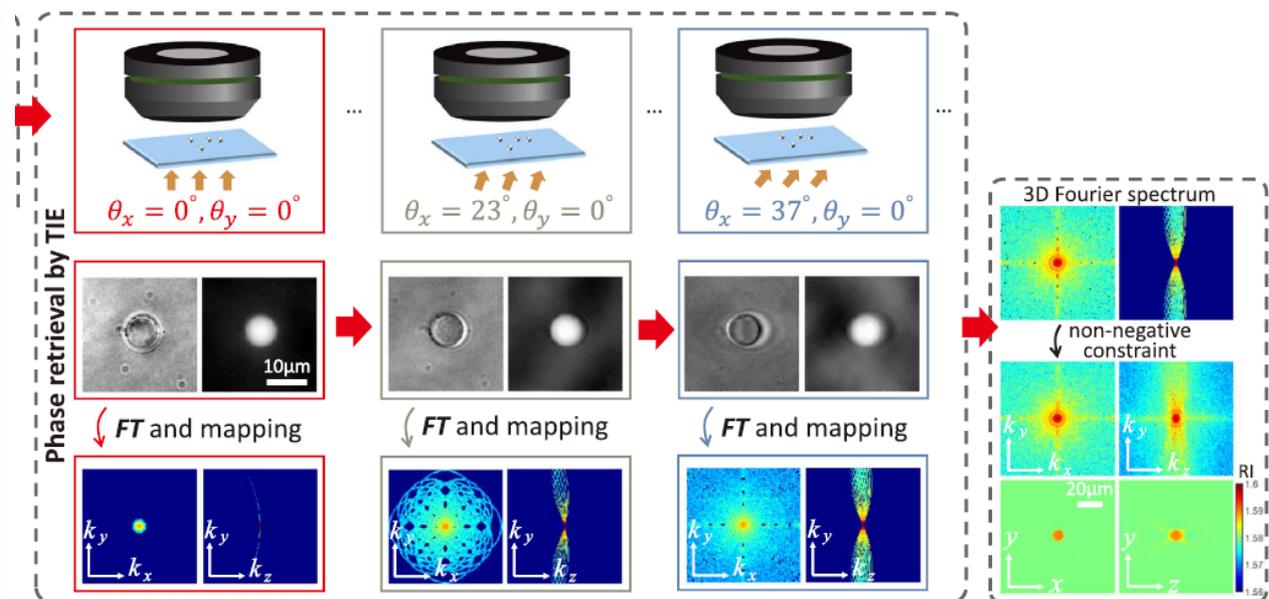
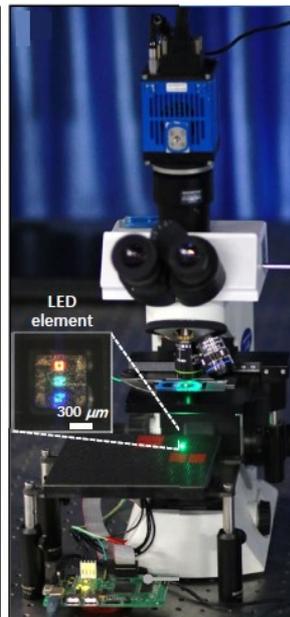
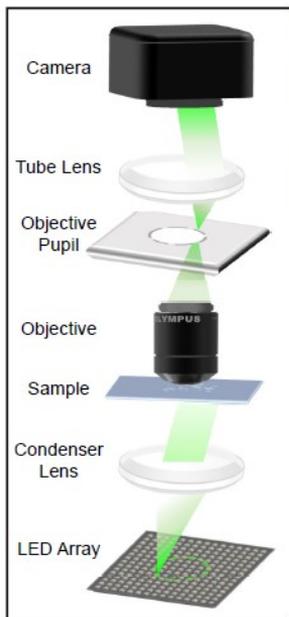
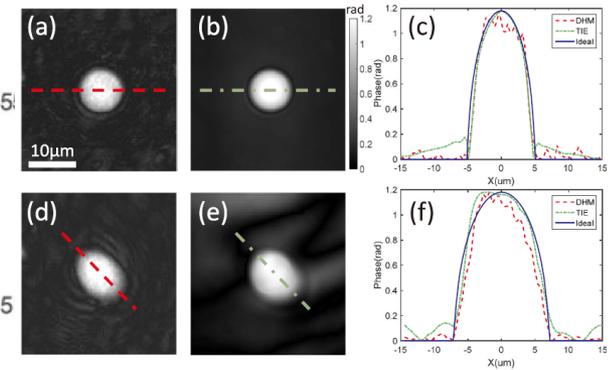
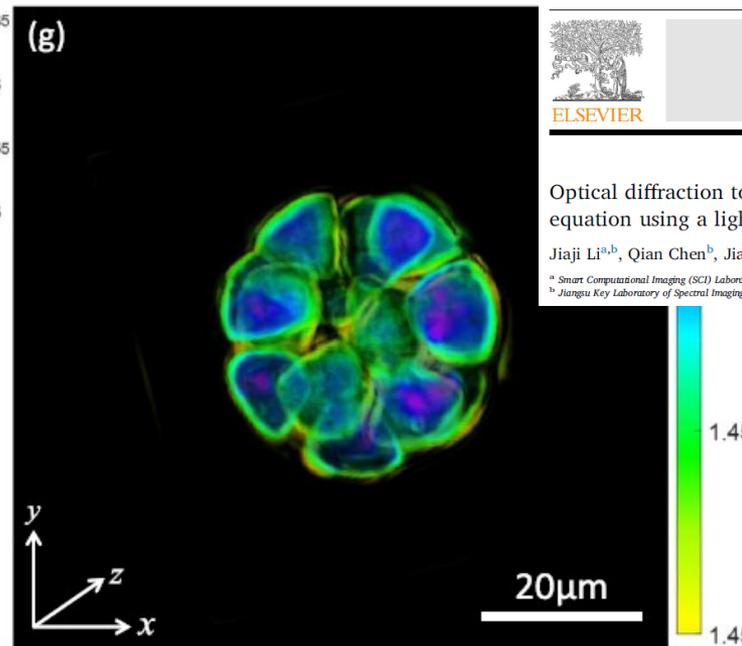
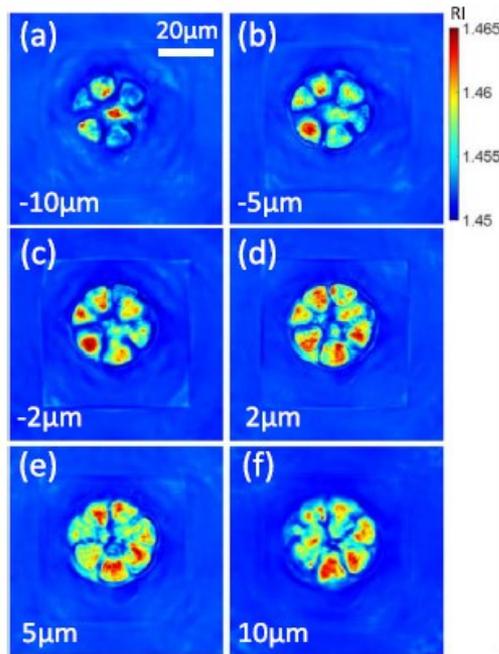


Optical diffraction tomography microscopy with transport of intensity equation using a light-emitting diode array

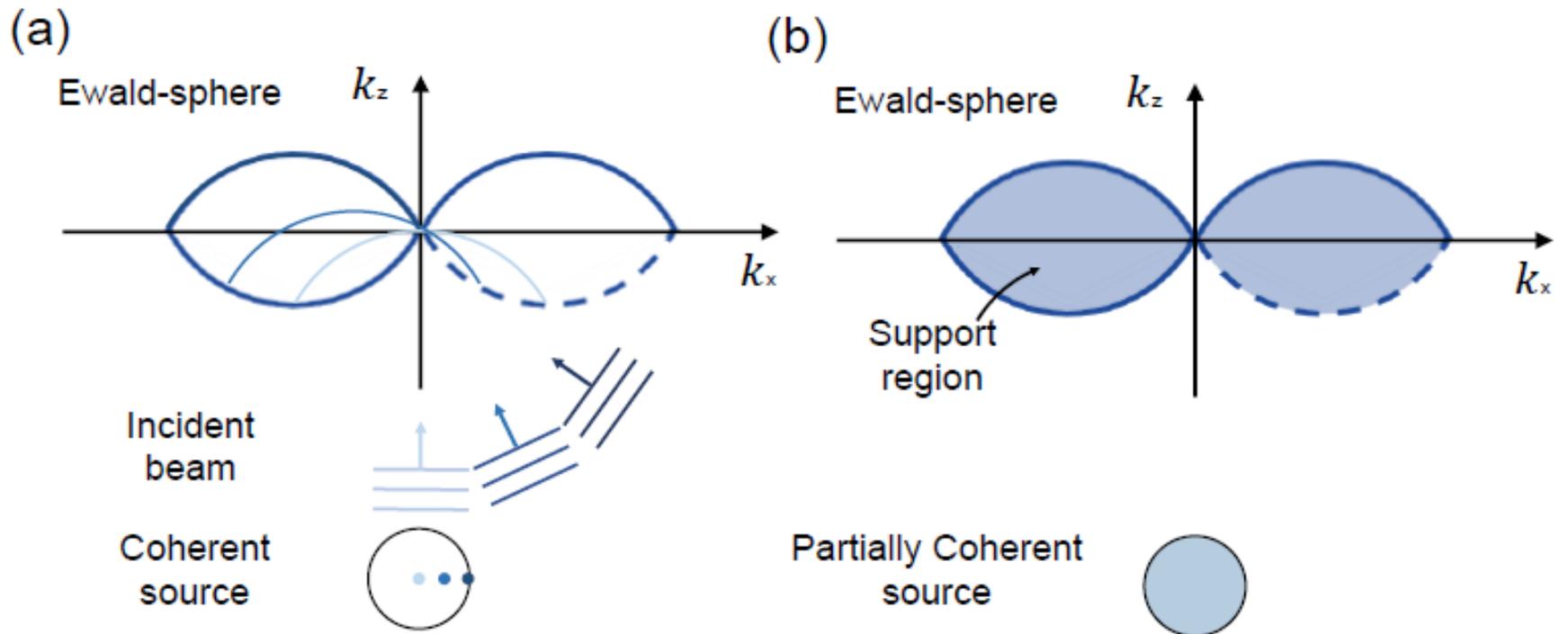
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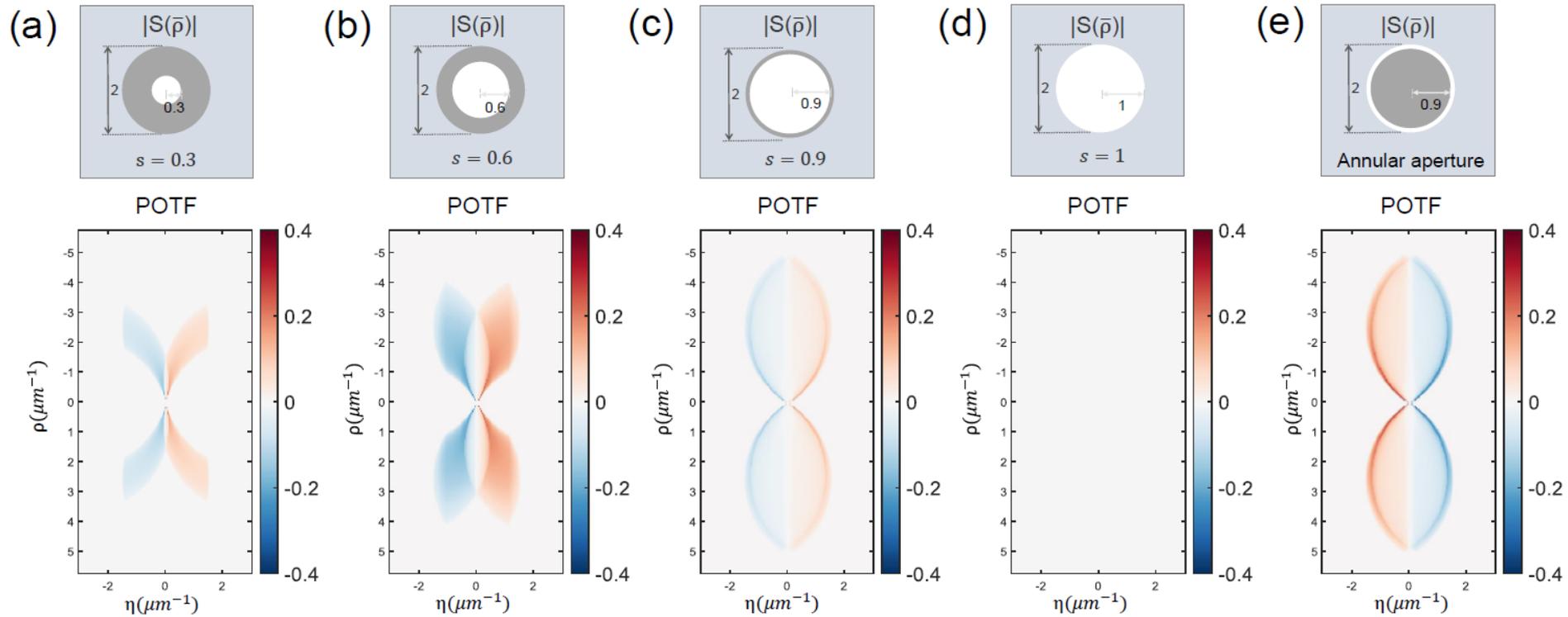
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Partially coherent ODT



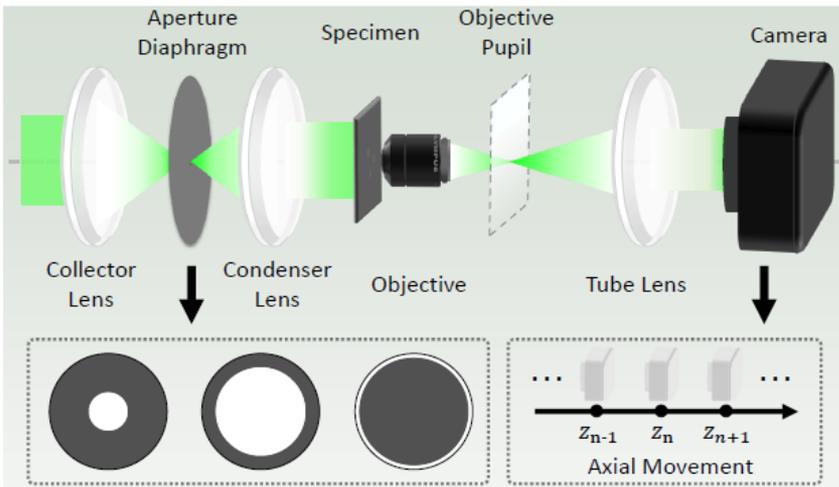
Partially coherent 3D imaging



Partially coherent 3D imaging

$$\begin{aligned} WOTF(\mathbf{u}) &\equiv TCC(\mathbf{u}, \mathbf{0}) \\ &= \iint S(\mathbf{u}') H(\mathbf{u}' + \mathbf{u}) H^*(\mathbf{u}') d\mathbf{u}' \end{aligned}$$

$$\begin{aligned} H(\rho, l) &= \int P(\rho) e^{jkz\sqrt{1-\lambda^2\rho^2}} e^{-j2\pi zl} dz \\ &= P(\rho) \delta\left(l - \sqrt{\left(\frac{1}{\lambda}\right)^2 - \rho^2}\right) \end{aligned}$$



Three-dimensional tomographic microscopy technique with multi-frequency combination with partially coherent illuminations

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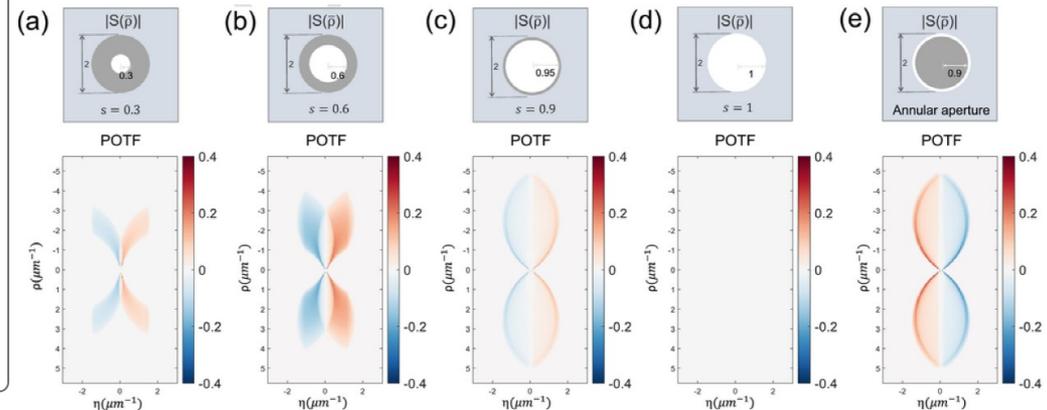
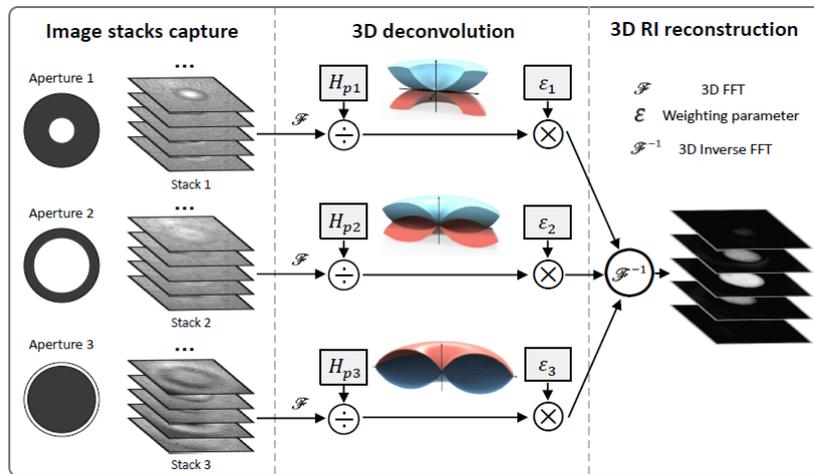
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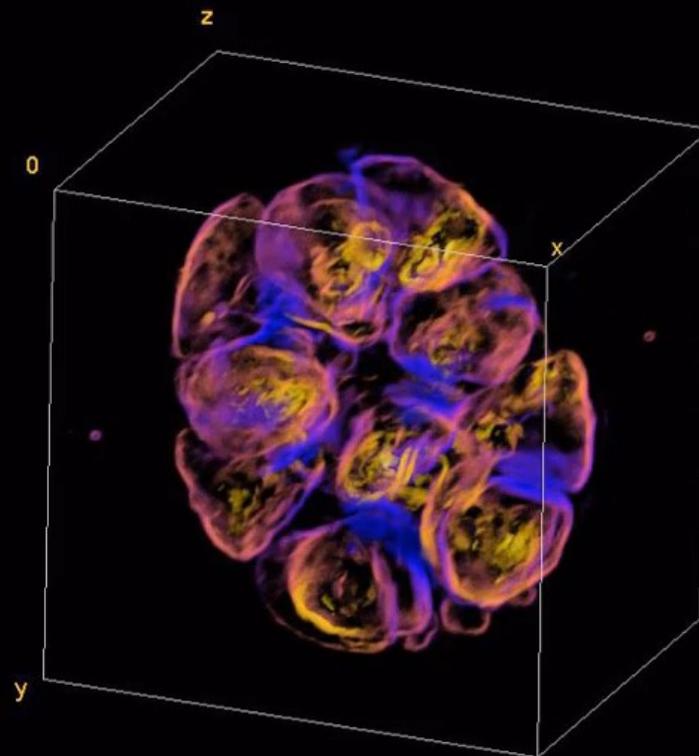
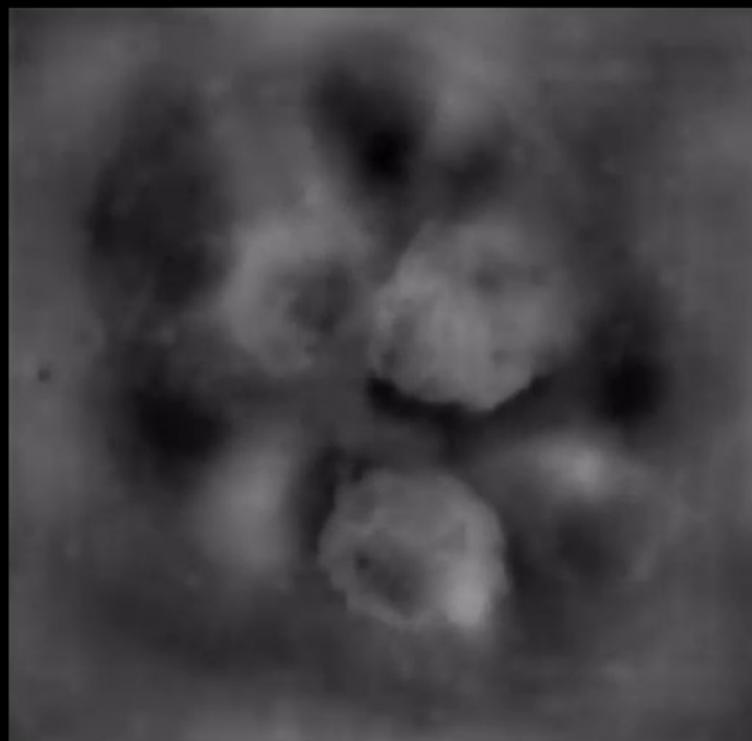
3D intensity spectrum

$$\tilde{I}(\zeta) = B\delta(\zeta) + \tilde{\Phi}(\zeta)T_P(\zeta) + \tilde{A}(\zeta)T_A(\zeta)$$

3D phase / amplitude transfer function

Transport-of-intensity diffraction tomography (TIDT)

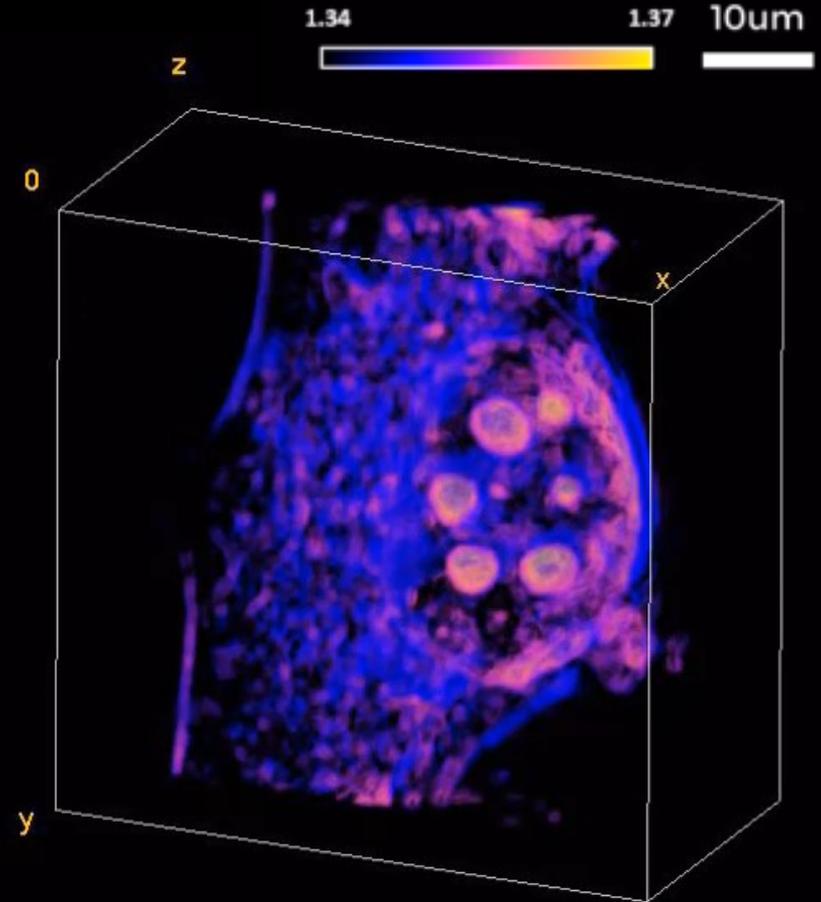
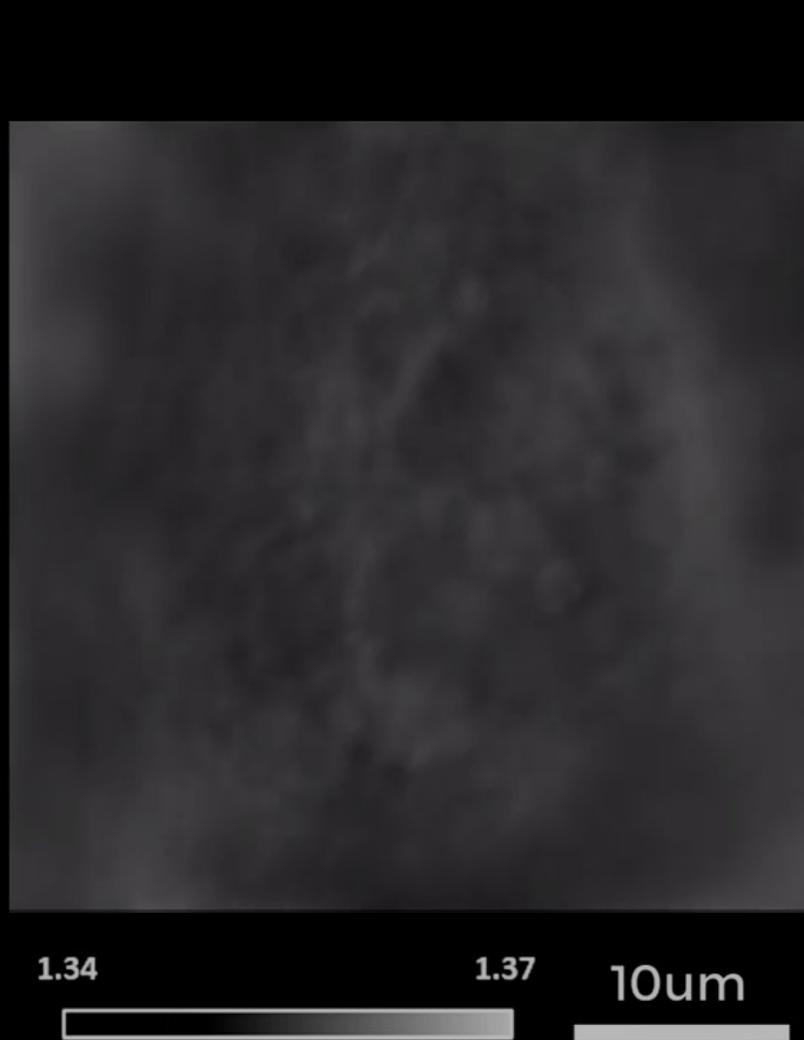
Annular-illumination ODT



3D rendering of Pandorina

1.4 NA_{ill} + 1.4 NA_{obj} 100X MO; Lateral resolution 200nm; axial resolution 650 nm.

Annular-illumination ODT



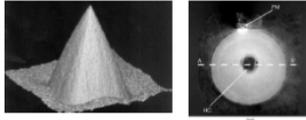
3D rendering of HeLa cell

1.4 NA_{ill} + 1.4 NA_{obj} 100X MO; Lateral resolution 200nm; axial resolution 650 nm.

Transport of intensity equation

2000-2008

Applications to TEM and neutron, and atom imaging [163-173]



2010-2015

High-order finite difference and OSF for Multi-plane TIE [188, 194-199, 204, 205, 273-275, 366, 367]

2014-2015

DCT-based solutions under inhomogeneous boundary conditions [200-202]

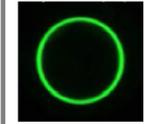
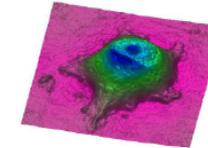
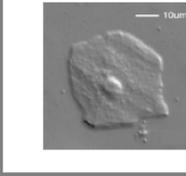
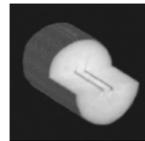
2014-2015

Generalized TIE in phase space [206, 207]

$$\frac{\partial I(\mathbf{x})}{\partial z} = -\nabla_{\mathbf{x}} \cdot \iint \lambda \mathbf{u} W_{\omega}(\mathbf{x}, \mathbf{u}) d\mathbf{u} d\omega$$

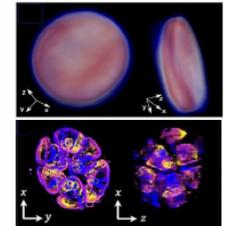
1999-2000

Frist demonstration of Quantitative phase tomography [162, 175]



2017-2019

Resolution enhancement by illumination engineering [208-210, 355, 369-371]

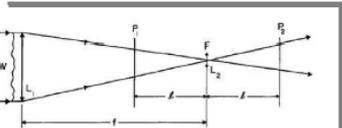


2015-2019

Transport of intensity diffraction tomography [211-213, 389, 395, 395, 407]

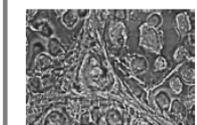
1988-1990

Frist application to adaptive optics (curvature sensing) [144-146]



1984

Frist exploration of partially coherence and optical microscopy [142]



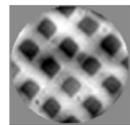
1982-1983

TIE derived [140, 141]

$$-k \frac{\partial I(\mathbf{x}, z)}{\partial z} = \nabla \cdot [I(\mathbf{x}, z) \nabla \phi(\mathbf{x})]$$

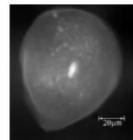
1995-1996

Frist applications to X-ray imaging [159, 160]



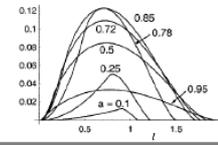
1998

Poynting vector Interpretation [158]



2010

Compatibility to DIC microscope [187]



2002

Transfer function analysis [176, 178]

1995

Proof of uniqueness [13]

1995-1998

Zernike and FFT-based solutions [156-158]

1998

Frist demonstration of quantitative optical phase microscopy [174]



For further details, please refer to:

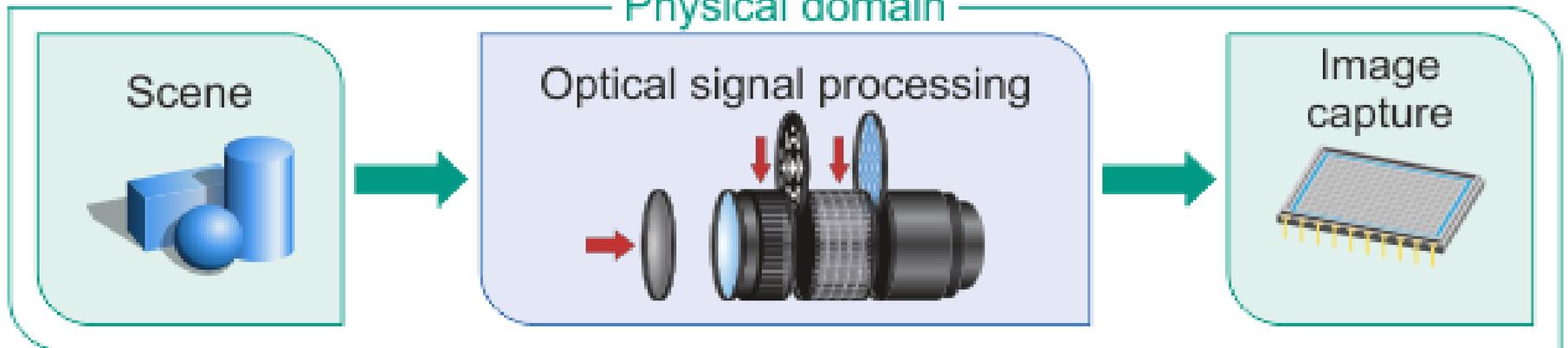
The screenshot shows the ScienceDirect website interface. At the top left is the ScienceDirect logo. The main header area includes 'Journals & Books', a search icon, and 'Register' and 'Sign in' buttons. Below the header, the journal title 'Optics and Lasers in Engineering' is displayed, along with the Elsevier logo and the journal homepage URL 'www.elsevier.com'. The article title 'Transport of intensity equation: a tutorial' is prominently featured, followed by the authors' names: Chao Zuo, Jiayi Li, Jiasong Sun, Yao Fan, Jialin Zhang, Linpeng Lu, Runnan Zhang, Bowen Wang, Lei Huang, and Qian Chen. The article information section includes keywords like 'Transport of Intensity Equation (TIE)', 'Quantitative Phase Imaging (QPI)', 'Phase Retrieval', 'Partial Coherence', and 'Optical Diffraction Tomography (ODT)'. The abstract section begins with 'When it comes to "phase measurement" or "quantitative phase imaging", many people will automatically connect them with "laser" and "interferometry". Indeed, conventional quantitative phase imaging and phase measurement techniques generally rely on the superposition of two beams with a high degree of coherence: complex interferometric configurations, stringent requirements on the environmental stabilities, and associated laser speckle noise severely limit their applications in optical imaging and microscopy. On a different note, as one of the most well-known phase retrieval approaches, the transport of intensity equation (TIE) provides a new non-interferometric way to access quantitative phase information through intensity only measurement. Despite the insufficiency for interferometry, TIE is applicable under partially coherent illuminations (like the Köhler's illumination in a conventional microscope), permitting optimum spatial resolution, higher signal-to-noise ratio, and better image quality. In this tutorial, we give an overview of the basic principle, research fields, and representative applications of TIE, focus particularly on optical imaging, metrology, and microscopy. The purpose of this tutorial is twofold. It should serve as a self-contained introduction to TIE for readers with little or no knowledge of TIE. On the other hand, it attempts to give an overview of recent developments in this field. These results highlight a new era in which strict coherence and interferometry are no longer prerequisites for quantitative phase imaging and diffraction tomography, paving the way toward new generation label-free three-dimensional microscopy, with applications in all branches of biomedicine.'

On the left side of the page, there is an 'Outline' section with a list of 10 items, including 'Introduction', 'Basic concept of TIE', 'Solutions to TIE', 'Image formation of coherent imaging an...', 'Axial intensity derivative estimation', 'Image formation under partially coheren...', 'Generalized TIE under partially coherent', '3D phase imaging under partially cohere...', 'Applications of TIE in optical imaging an...', 'Conclusions and future directions', 'CRedit authorship contribution statement', 'Declaration of Competing Interest', 'Acknowledgments', and 'Appendix A. Supplementary materials'. Below the outline, a box indicates 'Processing math: 26%'. On the right side, there are sections for 'if special issue:', 'Download special issue', and 'Recommended articles', which lists several related articles with 'View details' and 'PDF' links. At the bottom of the page, there is a navigation bar with page numbers '1 2' and a 'Next' button.

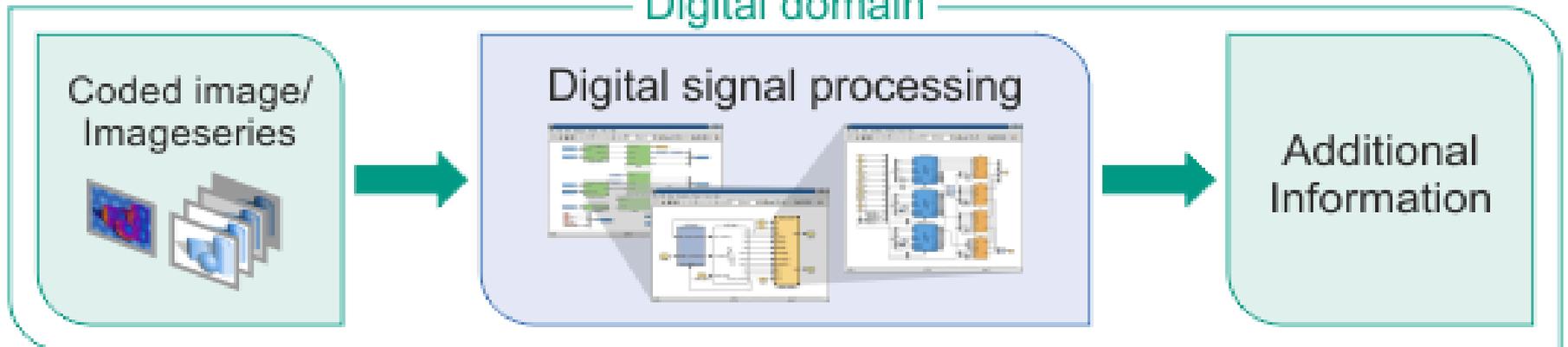
Transport of intensity equation: a tutorial
C Zuo, J Li, J Sun, Y Fan, J Zhang, L Lu, R Zhang, B Wang, L Huang, Q Chen
Optics and Lasers in Engineering, 106187, 2020

Computational imaging

Physical domain



Digital domain



· 特邀综述 ·

深度学习下的计算成像:现状、挑战与未来

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摘要 近年来,光学成像技术已经由传统的强度、彩色成像发展进入计算光学成像时代。计算光学成像基于几何光学、波动光学等理论对场景目标经光学系统成像再到探测器采样这一完整图像生成过程建立精确的正向数学模型,再求解该正向成像模型所对应的“逆问题”,以计算重构的方式来获得场景目标的高质量图像或者传统技术无法直接获得的相位、光谱、偏振、光场、相干度、折射率、三维形貌等高维度物理信息。然而,计算成像系统的实际成像性能也同样极大程度地受限于“正向数学模型的准确性”以及“逆向重构算法的可靠性”,实际成像物理过程的不可预见性与高维病态逆问题求解的复杂性已成为这一领域进一步发展的瓶颈问题。近年来,人工智能与深度学习技术的飞跃式发展为计算光学成像技术开启了一扇全新的大门。不同于传统计算成像方法所依赖的物理驱动,深度学习下的计算成像是一类由数据驱动的方法,它不但解决了许多过去计算成像领域难以解决的难题,还在信息获取能力、成像的功能、核心性能指标(如成像空间分辨率、时间分辨率、灵敏度等)上都获得了显著提升。基于此,首先概括性介绍深度学习技术在计算光学成像领域的研究进展与最新成果,然后分析了当前深度学习技术在计算光学成像领域面临的主要问题与挑战,最后展望了该领域未来的发展方向与可能的研究方向。

关键词 成像系统; 计算成像; 深度学习; 光学成像; 光信息处理

中图分类号 O436

文献标志码 A

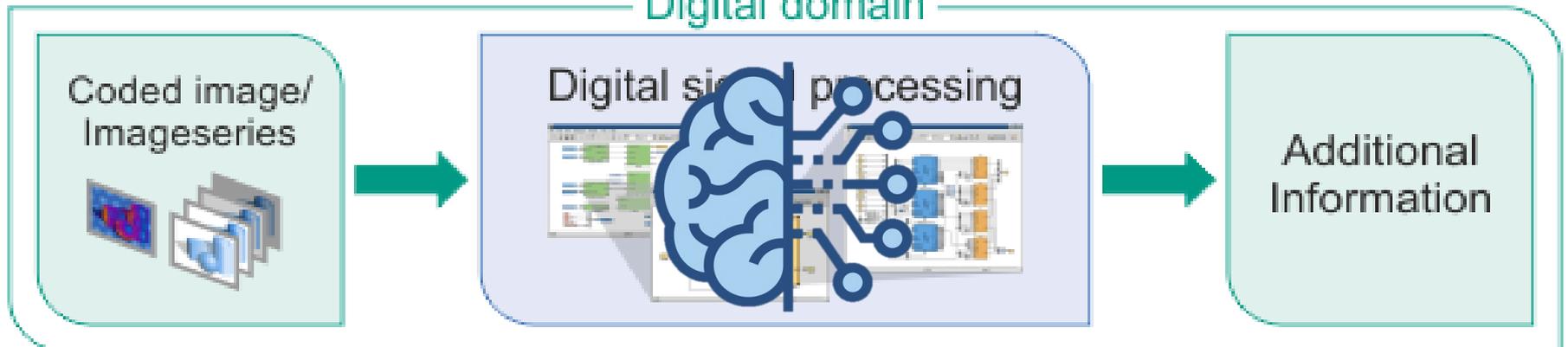
doi: 10.3788/AOS202040.0111003

Computational imaging

Physical domain



Digital domain





Thank you

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