

# Iterative Kramers-Kronig method for non-interferometric quantitative phase imaging: beyond the first-order Born and Rytov approximations

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Traditional non-interferometric QPI methods often face challenges in realizing rapid and accurate imaging of large-phase samples, mainly due to slow convergence and dependence on object approximation models. In this Letter, we propose a new non-interferometric QPI approach that leverages iterative Kramers-Kronig (KK) relations, named iKK-QPI, to achieve high-accuracy quantitative measurement of objects with large phase values. In the current KK relations reconstruction framework, we impose real-part constraints on the cepstrum, breaking the restriction of weak scattering condition. With only a few iterations, iKK-QPI extends the phase range that can be reliably retrieved by non-interferometric QPI, exceeding the first-order Born and Rytov approximations. The capability of iKK-QPI is demonstrated by imaging a microlens array and COS-7 cells. We accurately reconstruct objects with large phase ranges 6 rad (error <  $\pm 5\%$ ), three times that of the KK relations-based method, opening up the possibility for non-interferometric QPI to measure biological and industrial samples with large-phase features.

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Quantitative phase imaging (QPI) has emerged as an essential optical tool in biological research and medical diagnostics owing to its capability to quantify the optical thickness of living cells and tissues in a label-free manner. The phase distribution allows the determination of cellular structure and biophysical parameters, which is crucial for the investigation of their intrinsic properties. [1, 2] Conventional QPI techniques generally rely on the superposition of two highly coherent beams, demanding complex interferometric configurations and stable environments. [3] Moreover, the interferometric characteristics lead to limited lateral resolution and laser speckle noise, prohibiting their widespread use in biological and medical science.

Non-interferometric QPI techniques address several issues inherent in interferometric methods, offering simplified imaging system while enhancing reconstruction accuracy and quality. These techniques recover the phase directly from the intensity, viewing it as an inverse problem that requires a rigorous "intensity-phase" model, which varies across different imaging systems. A coherent imaging system, such as Fourier ptychographic microscopy (FPM) [4–6], is linear in complex amplitude. Despite this, FPM still suffers from two weaknesses: (1) substantial data redundancy is required to ensure stable convergence; (2) a reliable solution needs considerable iterations and is computationally intensive. These limitations complicate the optimal balance between reconstruction speed and measurement precision, especially for objects with high phase dynamic range (referred to as "large-phase" objects below for brevity). In contrast, the nonlinear image generation model of partially coherent imaging leads to the coupling of amplitude and phase, such as transport of intensity equation (TIE) [7, 8] and differential phase contrast (DPC) [9, 10]. Their solutions often linearize the forward model of the imaging process by introducing the Born/Rytov (weak/slowly varying object) approximation. Specifically, the first-order Born approximation assumes that the object exhibits weak scattering [11], while the first-order Rytov approximation presumes that the phase gradient introduced by the object is relatively smooth [12]. The deterministic nature of phase retrieval depends on these approximations, which are not always strictly valid in practical applications. Although some iterative methods can overcome these limitations, the solutions remain intricate and do not depart from the process of introducing approximate models [13]. Consequently, non-interferometric phase retrieval for samples with large phase values remains a challenge.

Recently, the Kramers-Kronig (KK) relations have garnered interest in QPI field [14–17] due to their distinctive ability to decouple the real and imaginary components of a complex function analytic in the upper half-plane. A method based on space-domain KK relations transforms the spatial intensity variations into spatial phase variations, allowing for phase images from a

single intensity measurement under oblique illumination. [18] Essentially, the KK relations establish a linear model that converts a multiplicative modulation relationship into an additive one via cepstrum, a nonlinear operation that does not involve any object approximation. However, the true phase range remains unrecoverable solely relying on the KK relations when the object scattering is strong. Nevertheless, its linear model gets rid of the approximation limitations that usually conflict with the optical properties of samples, providing the potential to estimate the morphology of large-phase objects more accurately.

In this Letter, we propose an iterative KK relations-based method for non-interferometric QPI (iKK-QPI) to achieve high-accuracy large-phase retrieval, exceeding the limitations of the first-order Born and Rytov approximations. We use the KK relations to model objects and combine it with a complex amplitude retrieval process. This model uses the cepstrum to allow direct acquisition of analytical expression for intensity and phase without any approximation process, which avoids the nonlinear errors arising from the neglect of higher-order terms in Born or Rytov approximation. Furthermore, we update the real part of the complex amplitude in the logarithmic domain by iteration. iKK-QPI imposes constraints based on the KK relations to dramatically speed up the iterative convergence, enabling high-precision reconstruction with only a few iterations. Thus, the proposed method overcomes the challenge of applying non-interferometric QPI techniques to large-phase samples.

Conventional non-interferometric QPI methods commonly simplify the imaging model to a mathematical analytical form by introducing object approximations. However, these approximation conditions ignore a series of higher-order phase terms, leading to nonlinear errors. More importantly, accurate phase retrieval cannot be achieved for samples that deviate from these conditions, such as large-phase objects. In our method, instead of the approximate models that introduce higher-order nonlinear errors, iKK-QPI describes the distribution of objects by a more accurate linear imaging model based on the KK relations. To satisfy the KK relations, we use annular matched illumination [19], i.e., the unscattered light must be located at the edge of the pupil in the Fourier plane. The complex amplitude of the object under each illumination angle is  $U_i(x, y)$ , the sub-spectrum of the corresponding aperture is  $S_i(u, v)$ , and the captured intensity image is  $I_i = |U_i(x, y)|^2$ . Define a complex function

$$\chi(\mathbf{r}) = \log[U_i(\mathbf{r})] - i\mathbf{k}_{inc} \cdot \mathbf{r} \quad (1)$$

where  $\mathbf{r} = x\hat{x} + y\hat{y}$ ,  $\mathbf{k}_{inc}$  is the transverse wave vector of the incident plane wave. The imaginary part of  $\chi(\mathbf{r})$  can be obtained from its real part  $\text{Re}[\chi(\mathbf{r})] = \log(I_i)/2$  by a directional Hilbert transform, and thus the complete complex amplitude of the object is reconstructed.

Assuming that the incident beam is a quasi-monochromatic plane wave  $U_{in}(\mathbf{r}) = |U_{in}|e^{i\mathbf{k}_{inc} \cdot \mathbf{r}}$ , the total field  $U(\mathbf{r})$  can be regarded as a superposition of the incident field  $U_{in}(\mathbf{r})$  and the scattered field  $U_s(\mathbf{r})$ , i.e.,  $U(\mathbf{r}) = U_{in}(\mathbf{r}) + U_s(\mathbf{r})$ . Then the Eq. (1) can be written as

$$\chi = \log\left[1 + \frac{U_s}{U_{in}}\right] + \log|U_{in}| \quad (2)$$

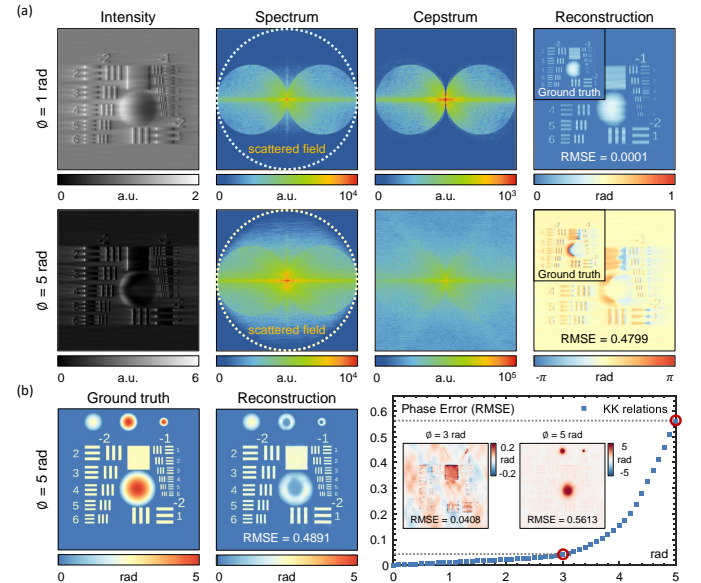
Without loss of generality, the incident beam can be considered to have a unit amplitude  $U_{in}(\mathbf{r}) = e^{i\mathbf{k}_{inc} \cdot \mathbf{r}}$ , then the intensity and scattered field can be transformed into an additive relationship by the cepstrum

$$\log I = \log(1 + U_s) + \log(1 + U_s)^* \quad (3)$$

Different from the Born/Rytov approximation, the equality sign of Eq. (3) always holds without any approximation. For  $|U_{in}| > |U_s|$ , the logarithmic term in Eq. (2) can be Taylor expanded as

$$\log\left[1 + \frac{U_s}{U_{in}}\right] = \sum_{n=0}^{\infty} \frac{(-1)^n}{n+1} \left(\frac{U_s}{U_{in}}\right)^{n+1} \quad (4)$$

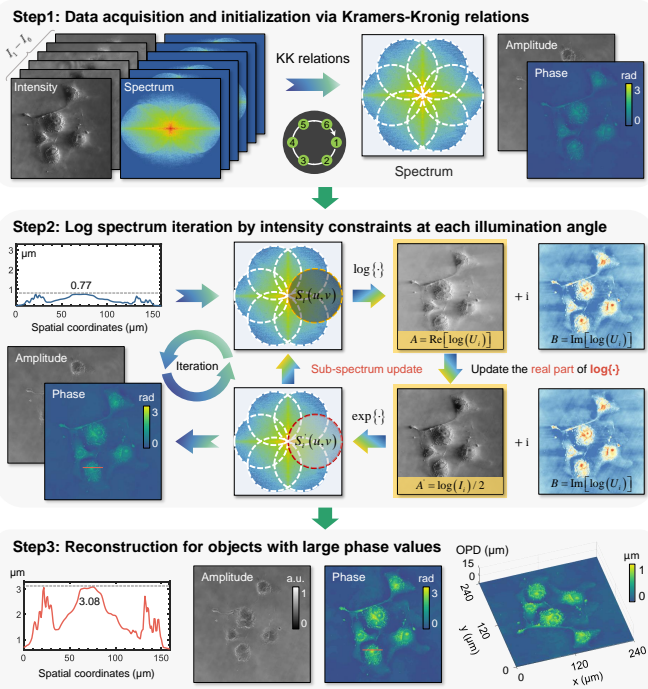
Since the analyticity means the existence of a convergent power series, the validity of the KK relations requires that the unscattered light is stronger than the scattered light. Due to the intrinsic correlation between the scattering intensity and the internal refractive index variations of the object, which manifest as phase changes in QPI, the fulfillment of this condition is closely related to the phase distribution of the measured object. For large-phase objects with strong scattering, the higher-order power series in Eq. (4) are severely divergent in the frequency domain, making reconstruction via the KK relations no longer valid [Fig. 1(a)]. In addition, the phase gradient is also one of the crucial factors in determining the reconstruction quality. For the same phase range, smaller phase gradient means higher reconstruction accuracy [Fig. 1(b)]. Inspired by the alternating projection in phase retrieval, an iterative algorithm based on the KK relations model enables high-accuracy reconstruction of objects with large phase values and phase gradients through nonlinear optimization.



**Fig. 1.** Simulation results of the KK relations-based method. (a) Comparison of intensity, spectrum and reconstruction results for objects of different phase ranges. (b) Reconstruction result of a 5 rad object and RMSE curve as phase increases.

Figure 2 illustrates the working flow of iKK-QPI with unstained COS-7 cells as an example. Multi-angle intensity images are acquired under the matched illumination condition and the complex amplitude of the object is reconstructed via the KK relations [see Step1]. In Step2, we take the reconstructed complex amplitude as the initial value to perform the iteration. Taking the logarithm of  $U_i(x, y)$  corresponding to the sub-spectrum  $S_i(u, v)$  of each illumination angle in turn, we obtain  $\log[U_i(x, y)]$ , whose complex amplitude can be written in the form of  $A + iB$ , with  $A$  and  $B$  denoting the real and imaginary parts. According to Eq. (3), calculate  $\log(I_i)/2$  and update the real part  $A$ . One iteration of the algorithm is completed after updating all the sub-spectrums. This process is repeated to minimize the  $L_2$ -distance between the real part of the logarithm of forward-generated complex amplitude and the logarithm of

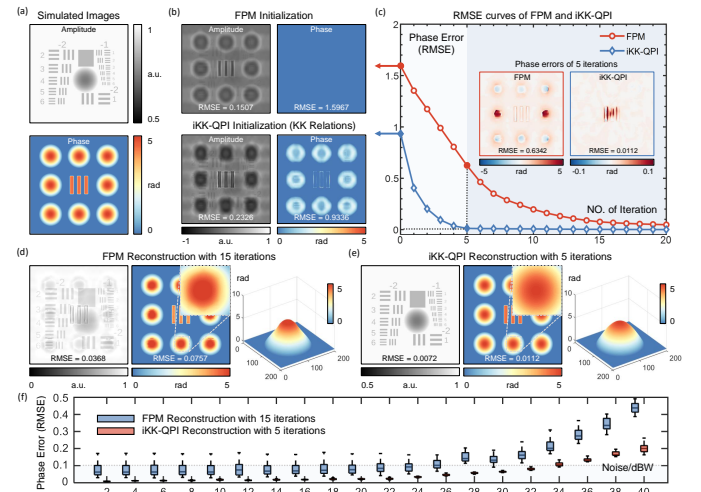
144 observations until convergence. The reconstructed phase range  
 145 is much larger than the initial value via the KK relations [see  
 146 Step 3]. It should be emphasized that the intensity constraint  
 147 of iKK-QPI is conducted in the logarithmic domain, which is a  
 148 fundamental difference from conventional FPM. The details of  
 149 high and low brightness regions in a logarithmic image can be  
 150 displayed simultaneously. In addition, the logarithmic opera-  
 151 tion combined with filtering can suppress the effects of noise,  
 152 particularly multiplicative noise, thereby improving the image  
 153 quality. [20] iKK-QPI achieves high-precision measurement of  
 154 large-phase objects with only a few iterations, enhancing the  
 155 imaging efficiency of large-phase objects.



**Fig. 2.** Flow chart of data processing in iKK-QPI for large-phase retrieval on the example of unstained COS-7 cells.

156 Simulations were carried out to verify the validity of iKK-QPI  
 157 for reconstructing large-phase objects. We simulated a sample  
 158 with a phase distribution of 0 – 5 rad [Fig. 3(a)], in which the  
 159 scattered light is stronger than the unscattered light, exceeding  
 160 the typical conditions required for accurate phase retrieval with  
 161 the KK relations. As a result, the phase reconstructed by the  
 162 KK relations-based method exhibits a much smaller range than  
 163 the true value, leading to errors in the amplitude at the same  
 164 positions [Fig. 3(b)]. We solved the phase using FPM and iKK-  
 165 QPI, respectively, where the conventional FPM algorithm takes  
 166 the average value of the intensity images as the initialization.  
 167 The root mean square error (RMSE) curves for the two iterative  
 168 methods are shown in Fig. 3(c). It is obvious from the blue curve  
 169 that as the number of iterations increases, the RMSE value of  
 170 iKK-QPI decreases rapidly and finally converges to 0 after just 5  
 171 iterations (RMSE 0.0112, total computation time 0.6 s with a 2.60  
 172 GHz laptop). In contrast, FPM requires 15 iterations to reduce  
 173 the RMSE evidently (red curve), three times as many as iKK-  
 174 QPI. Even after 15 iterations (RMSE 0.0757, total computation  
 175 time 1.9 s), the reconstruction results of FPM still suffered from  
 176 severe errors and thus could not be correctly phase unwrapped,  
 177 resulting in distortion of the object shape [Fig. 3(d)]. iKK-QPI  
 178 reconstructed large-phase objects with high accuracy in just 5  
 179 iterations, as shown by the amplitude and unwrapped phase

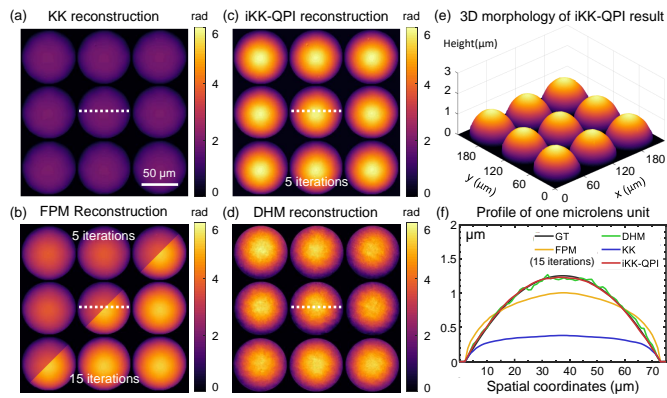
180 results in Fig. 3(e). In addition, we performed 20 experiments  
 181 under varying signal-to-noise ratios (SNRs) to evaluate the per-  
 182 formance of the two methods, confirming the noise suppression  
 183 capability of iKK-QPI [Fig. 3(f)].



**Fig. 3.** Simulation results of FPM and iKK-QPI for large-phase samples. (a) The simulated images. (b) Initialization. (c) RMSE curves versus the iteration number. (d), (e) Reconstruction results. (f) Phase error of reconstruction at different SNRs.

184 To verify the practicality of iKK-QPI, two experiments were  
 185 performed with the imaging system of AIFPM [19]. We used a  
 186 programmable LED array to implement the annular illumination  
 187 scheme. The height of the LED array is adjusted to position each  
 188 LED element precisely at the edge of the objective numerical  
 189 aperture (NA) in frequency space, ensuring that the KK relations  
 190 hold. The pixel size of the CMOS camera is 2.4  $\mu\text{m}$ , and the  
 191 central wavelength of the illumination is 550 nm.

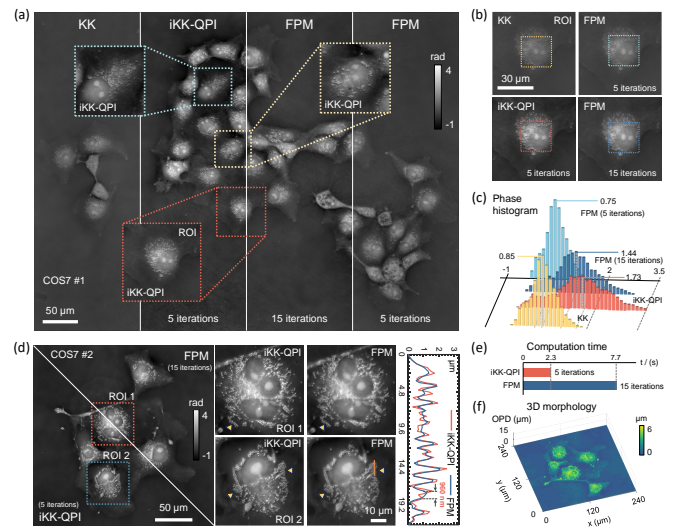
192 To quantitatively demonstrate the accuracy of iKK-QPI for  
 193 large-phase retrieval, we imaged a standard microlens array  
 194 with a curvature radius of 500  $\mu\text{m}$  and a pitch of 75  $\mu\text{m}$ . Its theo-  
 195 retical height is around 1.2  $\mu\text{m}$ , corresponding to a phase ampli-  
 196 tude of 6 rad. We used an objective lens with  $\times 4/0.16\text{NA}$  (Olym-  
 197 pus UPlanSApo) and acquired 8 images under annular matched  
 198 illumination. Since the background of the sample carries absorp-  
 199 tion, we processed the reconstructed phase with a mask. The  
 200 results of the KK relations-based method presented consider-  
 201 ably weaker phase contrast, indicating that the phase range was  
 202 much smaller than the theoretical value [Fig. 4(a)]. iKK-QPI  
 203 reconstructed a highly accurate phase distribution with only 5 it-  
 204 erations, while FPM failed to obtain the correct results even after  
 205 15 iterations [Fig. 4(b) and (c)]. From the three-dimensional (3D)  
 206 pseudo-color morphology in Fig. 4(e), iKK-QPI characterizes the  
 207 true morphology of the microlens. To quantitatively assess the  
 208 measurement precision, the same sample was measured using a  
 209 custom-built digital holographic microscope (DHM) equipped  
 210 with a  $\times 10/0.4$  NA objective lens (laser wavelength 550 nm)  
 211 [Fig. 4(d)]. After phase unwrapping and converting to physical  
 212 thickness, one microlens unit was selected and the phase values  
 213 along the white dashed line were plotted in Fig. 4(f). Although  
 214 the curvature radius of this line profile of DHM after arch fitting  
 215 reached an acceptable agreement with the nominal value, it suf-  
 216 fered severely from noise. The results obtained by iKK-QPI with  
 217 5 iterations are almost the same as the true value (error  $< \pm 5\%$ ).  
 218 It verifies that iKK-QPI realizes high-accuracy reconstruction  
 219 of large-phase objects and provides reliable quantitative phase  
 220 data for subsequent research and analysis.



**Fig. 4.** Comparative experiments on a standard microlens array sample. (a)–(d) Reconstructed phase distribution separately based on the KK relations, FPM, iKK-QPI, and DHM methods. (e) 3D pseudo-color morphological distribution. (f) Quantitative phase values along the white dashed.

Experiments on a COS-7 cell sample was conducted to demonstrate the capability of iKK-QPI for imaging complex samples such as unlabeled cells. We switched to a  $\times 10/0.4\text{NA}$  objective lens to better visualize cellular details. The phase results are shown in Fig. 5(a). It is evident that the reconstruction results of different methods are roughly the same for the relatively thin regions of the cells, but the phase values for the thicker regions around the nucleus differ considerably. The phase range reconstructed using the KK relations-based method is approximately 2.5 rad, much smaller than the theoretical thickness of COS-7 cells. In consistent with the simulation, iKK-QPI reconstructed 4 rad in only 5 iterations, while FPM was still not reached in 15 iterations. We selected a cell [Fig. 5(b)] and calculated the histograms of the dashed box regions, as shown in Fig. 5(c). The histograms provide a direct visualization of the phase distribution, further illustrating the effectiveness of the proposed method for large-phase retrieval. In addition, we compared the reconstructed image quality of iKK-QPI and FPM with two regions of interest (ROI) as shown in Fig. 5(d). Although both methods obtained similar phase ranges, iKK-QPI reconstructed COS-7 cells with much sharper edges of organelles such as nuclei and lipid droplets, even increasing the resolution. Moreover, the reconstruction process of iKK-QPI substantially reduced the number of iterations and shortened the time by more than three-fold compared with FPM [Fig. 5(e)]. This experiment demonstrated that iKK-QPI provides higher reconstruction accuracy and quality in shorter time for large-phase retrieval.

In conclusion, we have proposed the iKK-QPI method for high-accuracy imaging of large-phase objects. By integrating the KK relations with the real-part constraint of the cepstrum, iKK-QPI has overcome the limitations of conventional QPI technique for measuring large-phase objects, significantly broadening the application of QPI. This method belongs to the non-interferometric QPI technique, which does not require complex interferometric setups and coherent illumination, making it less susceptible to noise and artifacts. Experimental validation with a microlens array and live COS-7 cells has demonstrated the practical applicability of iKK-QPI, providing a promising tool for quantitative morphological measurements in both biological research and industrial inspection. In the future, iKK-QPI is expected to be combined with deep learning [21, 22], giving the potential to further enhance the imaging performance of non-interferometric QPI. iKK-QPI can also be extended to diffraction tomography for measuring 3D refractive index distribution of transparent samples [23–25], opening up new possibilities for



**Fig. 5.** Comparative experiments on COS-7 cells. (a) Reconstructed phase under the KK relations, iKK-QPI and FPM. (b) Enlarged images of the area in the red box in (a). (c) Phase histogram of the boxed regions in (b). (d) Reconstructed phase with iKK-QPI (5 iterations) and FPM (15 iterations), and phase values along the red line. (e) Computation time for the results in (d). (f) 3D display of reconstruction results.

studying a diverse range of specimens in various scientific fields.

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## REFERENCES

1. Y. Park, C. Depeursinge, and G. Popescu, *Nat. photonics* **12**, 578 (2018).
2. Z. Huang and L. Cao, *Light. Sci. & Appl.* **13**, 145 (2024).
3. E. Cuche, F. Bevilacqua, and C. Depeursinge, *Opt. letters* **24**, 291 (1999).
4. G. Zheng, R. Horstmeyer, and C. Yang, *Nat. photonics* **7**, 739 (2013).
5. X. Ou, G. Zheng, and C. Yang, *Opt. express* **22**, 4960 (2014).
6. C. Zuo, J. Sun, and Q. Chen, *Opt. express* **24**, 20724 (2016).
7. M. R. Teague, *JOSA* **73**, 1434 (1983).
8. C. Zuo, J. Li, J. Sun, *et al.*, *Opt. Lasers Eng.* **135**, 106187 (2020).
9. S. B. Mehta and C. J. Sheppard, *Opt. letters* **34**, 1924 (2009).
10. L. Tian and L. Waller, *Opt. express* **23**, 11394 (2015).
11. J. M. Cowley, *Diffraction physics* (Elsevier, 1995).
12. M. H. Jenkins and T. K. Gaylord, *Appl. optics* **54**, 8566 (2015).
13. Y. Fan, J. Sun, Y. Shu, *et al.*, *Photonics Res.* **11**, 442 (2023).
14. C. Shen, M. Liang, A. Pan, and C. Yang, *Photonics Res.* **9**, 1003 (2021).
15. Z. Huang and L. Cao, *Adv. Photonics Res.* **3**, 2100273 (2022).
16. R. Cao, C. Shen, and C. Yang, *Nat. Commun.* **15**, 4713 (2024).
17. S. Zhao, H. Zhou, S. Lin, *et al.*, *Biomed. Opt. Express* **15**, 5739 (2024).
18. Y. Baek and Y. Park, *Nat. Photonics* **15**, 354 (2021).
19. J. Sun, C. Zuo, J. Zhang, *et al.*, *Sci. reports* **8**, 7669 (2018).
20. R. C. Gonzales and P. Wintz, *Digital image processing* (Addison-Wesley Longman Publishing Co., Inc., 1987).
21. A. Saba, C. Gigli, A. B. Ayoub, and D. Psaltis, *Adv. Photonics* **4**, 066001 (2022).
22. Z. Wu, I. Kang, Y. Yao, *et al.*, *eLight* **3**, 7 (2023).
23. C. Zuo, J. Sun, J. Li, *et al.*, *Opt. Lasers Eng.* **128**, 106003 (2020).
24. J. Li, N. Zhou, J. Sun, *et al.*, *Light. Sci. & Appl.* **11**, 154 (2022).
25. Z. Huang and L. Cao, *APL Photonics* **9** (2024).

## FULL REFERENCES

- 305 1. Y. Park, C. Depeursinge, and G. Popescu, "Quantitative phase imaging  
306 in biomedicine," *Nat. photonics* **12**, 578–589 (2018).
- 307 2. Z. Huang and L. Cao, "Quantitative phase imaging based on hologra-  
308 phy: trends and new perspectives," *Light. Sci. & Appl.* **13**, 145 (2024).
- 309 3. E. Cuche, F. Bevilacqua, and C. Depeursinge, "Digital holography for  
310 quantitative phase-contrast imaging," *Opt. letters* **24**, 291–293 (1999).
- 311 4. G. Zheng, R. Horstmeyer, and C. Yang, "Wide-field, high-resolution  
312 fourier ptychographic microscopy," *Nat. photonics* **7**, 739–745 (2013).
- 313 5. X. Ou, G. Zheng, and C. Yang, "Embedded pupil function recovery for  
314 fourier ptychographic microscopy," *Opt. express* **22**, 4960–4972 (2014).
- 315 6. C. Zuo, J. Sun, and Q. Chen, "Adaptive step-size strategy for noise-  
316 robust fourier ptychographic microscopy," *Opt. express* **24**, 20724–  
317 20744 (2016).
- 318 7. M. R. Teague, "Deterministic phase retrieval: a green's function solu-  
319 tion," *JOSA* **73**, 1434–1441 (1983).
- 320 8. C. Zuo, J. Li, J. Sun, *et al.*, "Transport of intensity equation: a tutorial,"  
321 *Opt. Lasers Eng.* **135**, 106187 (2020).
- 322 9. S. B. Mehta and C. J. Sheppard, "Quantitative phase-gradient imaging  
323 at high resolution with asymmetric illumination-based differential phase  
324 contrast," *Opt. letters* **34**, 1924–1926 (2009).
- 325 10. L. Tian and L. Waller, "Quantitative differential phase contrast imaging  
326 in an led array microscope," *Opt. express* **23**, 11394–11403 (2015).
- 327 11. J. M. Cowley, *Diffraction physics* (Elsevier, 1995).
- 328 12. M. H. Jenkins and T. K. Gaylord, "Quantitative phase microscopy via  
329 optimized inversion of the phase optical transfer function," *Appl. optics*  
330 **54**, 8566–8579 (2015).
- 331 13. Y. Fan, J. Sun, Y. Shu, *et al.*, "Accurate quantitative phase imaging by  
332 differential phase contrast with partially coherent illumination: beyond  
333 weak object approximation," *Photonics Res.* **11**, 442–455 (2023).
- 334 14. C. Shen, M. Liang, A. Pan, and C. Yang, "Non-iterative complex wave-  
335 field reconstruction based on kramers–kronig relations," *Photonics Res.*  
336 **9**, 1003–1012 (2021).
- 337 15. Z. Huang and L. Cao, "High bandwidth-utilization digital holographic  
338 multiplexing: an approach using kramers–kronig relations," *Adv. Pho-  
339 tonics Res.* **3**, 2100273 (2022).
- 340 16. R. Cao, C. Shen, and C. Yang, "High-resolution, large field-of-view  
341 label-free imaging via aberration-corrected, closed-form complex field  
342 reconstruction," *Nat. Commun.* **15**, 4713 (2024).
- 343 17. S. Zhao, H. Zhou, S. Lin, *et al.*, "Efficient, gigapixel-scale, aberration-  
344 free whole slide scanner using angular ptychographic imaging with  
345 closed-form solution," *Biomed. Opt. Express* **15**, 5739–5755 (2024).
- 346 18. Y. Baek and Y. Park, "Intensity-based holographic imaging via space-  
347 domain kramers–kronig relations," *Nat. Photonics* **15**, 354–360 (2021).
- 348 19. J. Sun, C. Zuo, J. Zhang, *et al.*, "High-speed fourier ptychographic  
349 microscopy based on programmable annular illuminations," *Sci. reports*  
350 **8**, 7669 (2018).
- 351 20. R. C. Gonzales and P. Wintz, *Digital image processing* (Addison-  
352 Wesley Longman Publishing Co., Inc., 1987).
- 353 21. A. Saba, C. Gigli, A. B. Ayoub, and D. Psaltis, "Physics-informed neural  
354 networks for diffraction tomography," *Adv. Photonics* **4**, 066001–066001  
355 (2022).
- 356 22. Z. Wu, I. Kang, Y. Yao, *et al.*, "Three-dimensional nanoscale reduced-  
357 angle ptycho-tomographic imaging with deep learning (rapid)," *eLight*  
358 **3**, 7 (2023).
- 359 23. C. Zuo, J. Sun, J. Li, *et al.*, "Wide-field high-resolution 3d microscopy  
360 with fourier ptychographic diffraction tomography," *Opt. Lasers Eng.*  
361 **128**, 106003 (2020).
- 362 24. J. Li, N. Zhou, J. Sun, *et al.*, "Transport of intensity diffraction tomogra-  
363 phy with non-interferometric synthetic aperture for three-dimensional  
364 label-free microscopy," *Light. Sci. & Appl.* **11**, 154 (2022).
- 365 25. Z. Huang and L. Cao, "k-space holographic multiplexing for synthetic  
366 aperture diffraction tomography," *APL Photonics* **9** (2024).
- 367